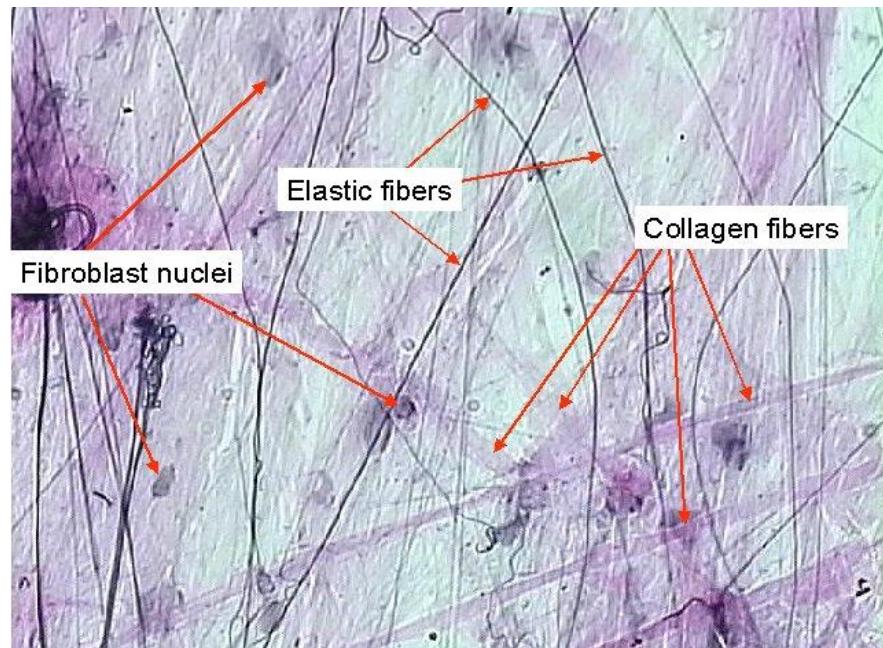


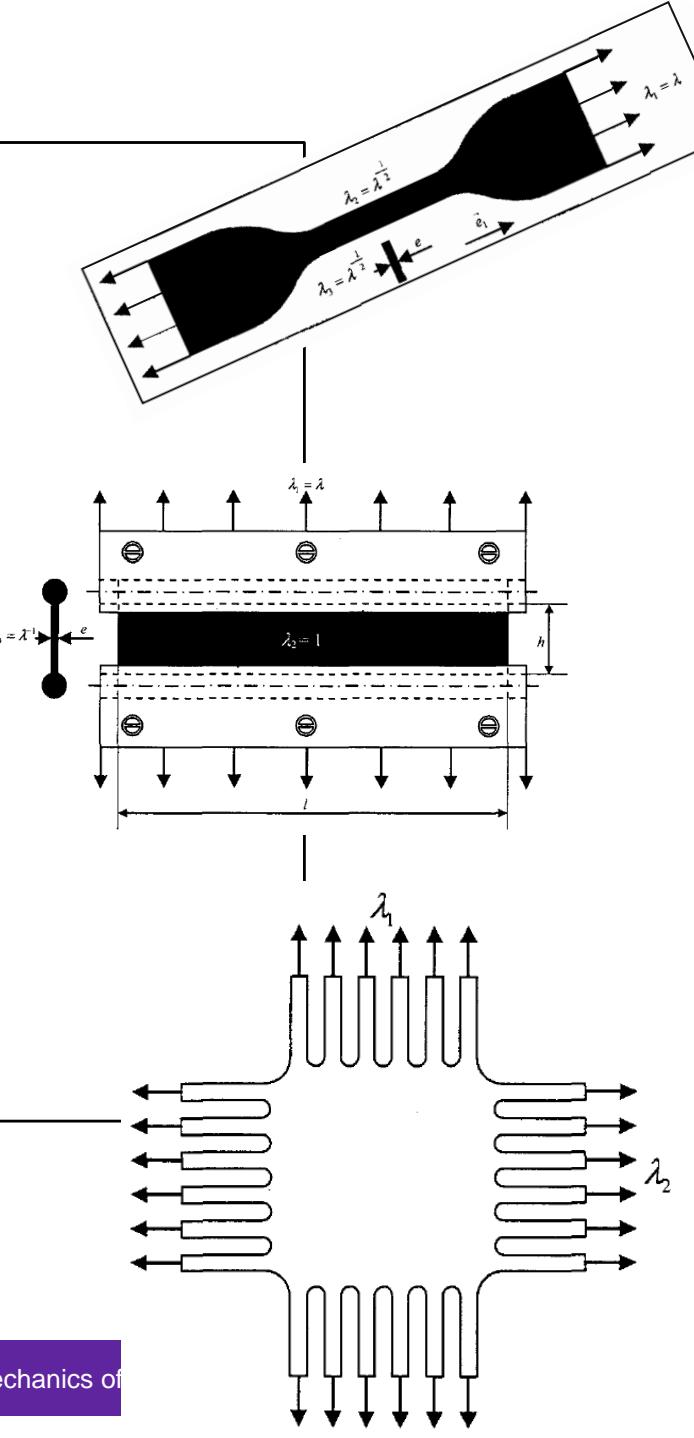
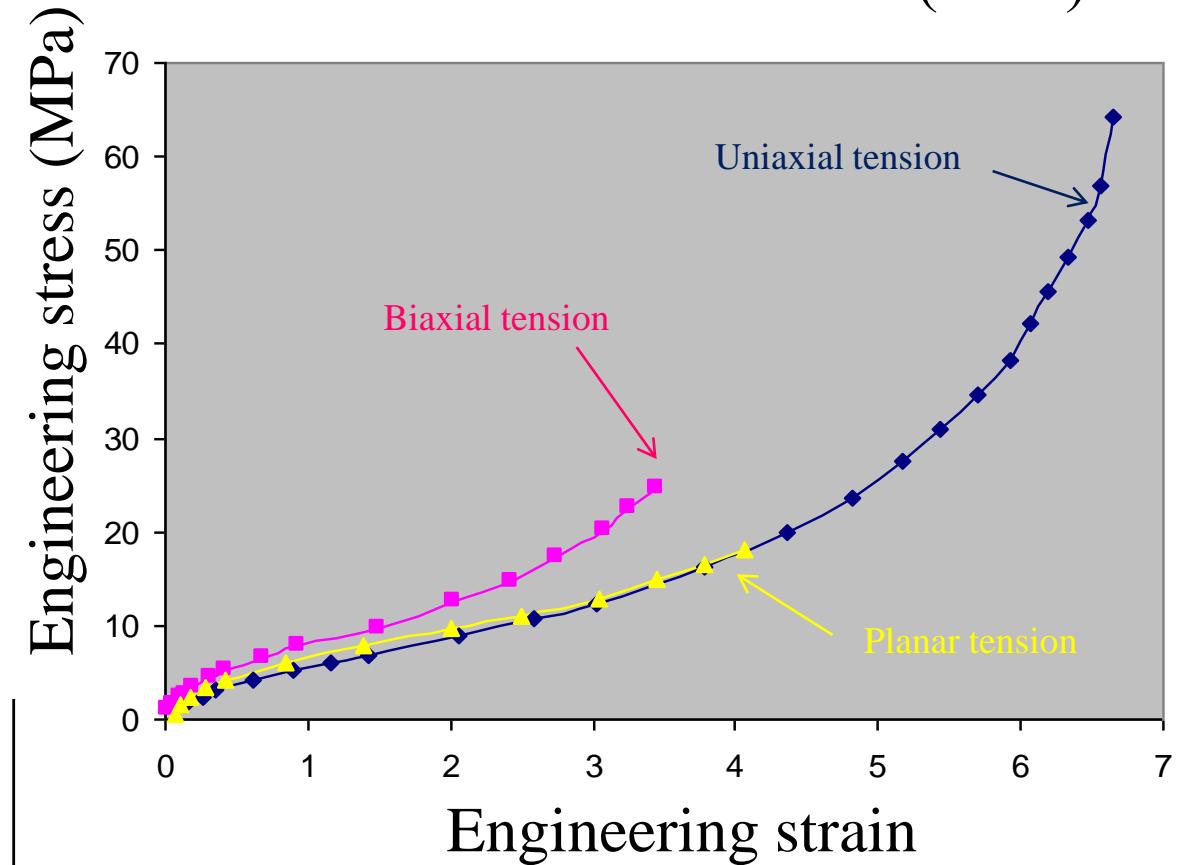
# Mechanics of soft biological tissues

Prof Stéphane AVRIL

# Soft biological tissues: many challenges for continuum mechanics



# Treolar's tests on rubber (1944)



# Identification approach

We choose a constitutive model and we determine the parameters so as to minimize the following cost function:

$$E = \sum_{i=1}^n \left( \frac{F_i^{mes} - F_i^{th}}{\bar{F}_i^{mes}} \right)^2$$

$F_i^{mes}$  are the experimentally measured forces

$\bar{F}_i^{mes}$  is their average

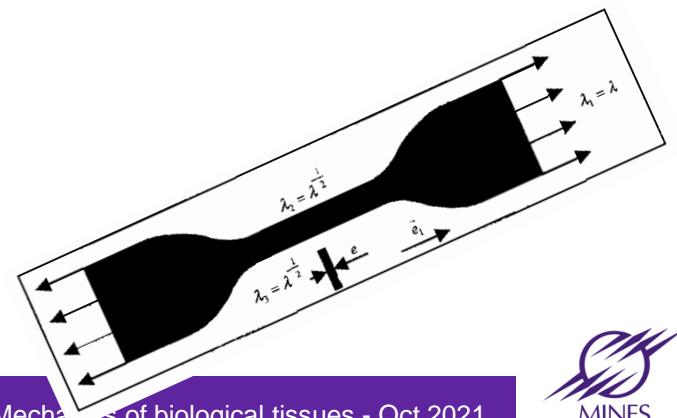
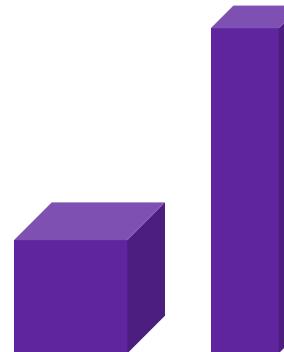
$F_i^{th}$  are the model predictions of the forces

# Identification procedure

Uniaxial tension

Equibiaxial tension

Planar tension

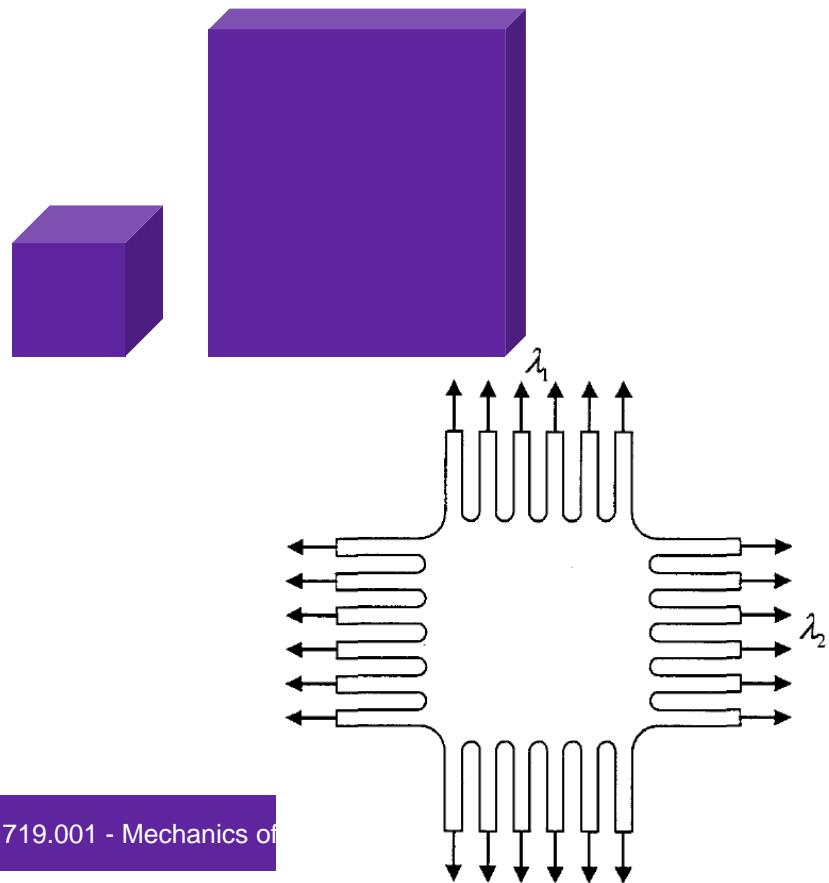


# Identification procedure

Uniaxial tension

Equibiaxial tension

Planar tension

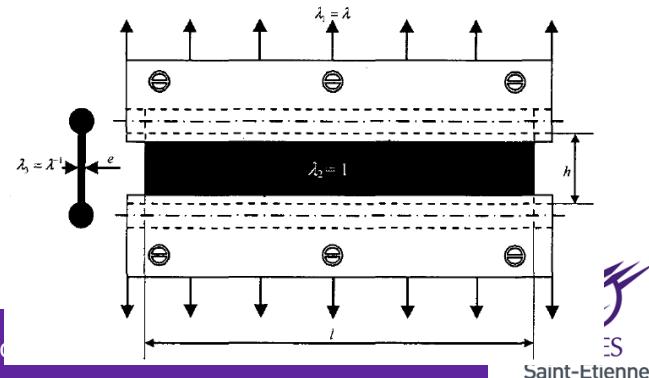
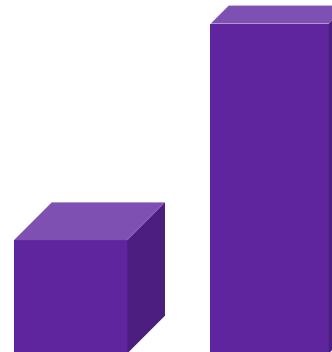


# Identification procedure

Uniaxial tension

Equibiaxial tension

Planar tension



# Identification procedure

## Uniaxial tension

$$\underline{\underline{F}} = \begin{bmatrix} \lambda & 0 & 0 \\ 0 & \lambda^{-\frac{1}{2}} & 0 \\ 0 & 0 & \lambda^{-\frac{1}{2}} \end{bmatrix}$$

$$\underline{\underline{\sigma}} = \begin{bmatrix} \frac{\lambda F}{S_0} & 0 & 0 \\ 0 & 0 & 0 \\ 0 & 0 & 0 \end{bmatrix}$$

$$I_1 = \lambda^2 + 2\lambda^{-1} \quad I_2 = \lambda^{-2} + 2\lambda$$

$$\underline{\underline{\sigma}} = \left[ \left( 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}_1} + 2 \underline{\underline{I}}_1 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \right) \underline{\underline{F}}^t \underline{\underline{F}} - 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \underline{\underline{F}}^t \underline{\underline{F}} \underline{\underline{F}}^t \underline{\underline{F}} \right] + c \underline{\underline{I}}$$

# Identification procedure

## Uniaxial tension

$$\frac{\lambda F}{S_0} = \left[ \left( 2 \frac{\partial \Psi}{\partial I_1} + 2 \left( \lambda^2 + \frac{2}{\lambda} \right) \frac{\partial \Psi}{\partial I_2} \right) \left( \lambda^2 - \lambda^{-1} \right) - 2 \frac{\partial \Psi}{\partial I_2} \left( \lambda^4 - \lambda^{-2} \right) \right]$$



$$\frac{F}{S_0} = 2 \left( 1 - \lambda^{-3} \right) \left( \lambda \frac{\partial \Psi}{\partial I_1} + \frac{\partial \Psi}{\partial I_2} \right)$$

Remark:

$$I_1 = \lambda^2 + 2\lambda^{-1} \quad I_2 = \lambda^{-2} + 2\lambda$$

$$\frac{dI_1}{d\lambda} = 2\lambda \left( 1 - \lambda^{-3} \right) \quad \frac{dI_2}{d\lambda} = 2 \left( 1 - \lambda^{-3} \right)$$

$$\frac{F}{S_0} = \frac{\partial \Psi}{\partial \lambda}$$

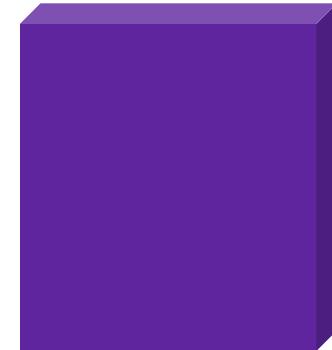
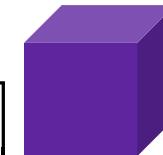
# Identification procedure

## Equibiaxial tension

$$\underline{\underline{F}} = \begin{bmatrix} \lambda & 0 & 0 \\ 0 & \lambda & 0 \\ 0 & 0 & \lambda^{-2} \end{bmatrix}$$

$$I_1 = 2\lambda^2 + \lambda^{-4} \quad I_2 = 2\lambda^{-2} + \lambda^4$$

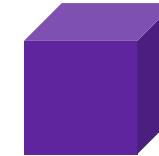
$$\underline{\underline{\sigma}} = \begin{bmatrix} \frac{\lambda F}{S_0} & 0 & 0 \\ 0 & \frac{\lambda F}{S_0} & 0 \\ 0 & 0 & 0 \end{bmatrix}$$



$$\underline{\underline{\sigma}} = \left[ \left( 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}} + 2 \underline{\underline{I}}_1 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \right) \underline{\underline{F}}^t \underline{\underline{F}} - 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \underline{\underline{F}}^t \underline{\underline{F}} \underline{\underline{F}}^t \underline{\underline{F}} \right] + c \underline{\underline{I}}$$

# Identification procedure

## Equibiaxial tension



$$\frac{\lambda F}{S_0} = \left[ \left( 2 \frac{\partial \Psi}{\partial I_1} + 2(2\lambda^2 + \lambda^{-4}) \frac{\partial \Psi}{\partial I_2} \right) (\lambda^2 - \lambda^{-4}) - 2 \frac{\partial \Psi}{\partial I_2} (\lambda^4 - \lambda^{-8}) \right]$$

$$\frac{F}{S_0} = 2(\lambda - \lambda^{-5}) \left( \frac{\partial \Psi}{\partial I_1} + \lambda^2 \frac{\partial \Psi}{\partial I_2} \right)$$

Remark:

$$I_1 = 2\lambda^2 + \lambda^{-4} \quad I_2 = 2\lambda^{-2} + \lambda^4$$

$$\frac{dI_1}{d\lambda} = 4(\lambda - \lambda^{-5}) \quad \frac{dI_2}{d\lambda} = 4\lambda^2(\lambda - \lambda^{-5})$$

$$\frac{F}{S_0} = \frac{1}{2} \frac{\partial \Psi}{\partial \lambda}$$

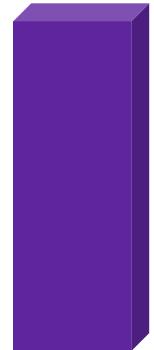
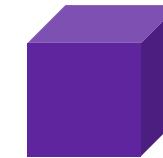
# Identification procedure

## Planar tension

$$\underline{\underline{F}} = \begin{bmatrix} \lambda & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & \lambda^{-1} \end{bmatrix}$$

$$\underline{\underline{\sigma}} = \begin{bmatrix} \frac{\lambda F}{S_0} & 0 & 0 \\ 0 & ? & 0 \\ 0 & 0 & 0 \end{bmatrix}$$

$$I_1 = \lambda^2 + \lambda^{-2} + 1 \quad I_2 = \lambda^2 + \lambda^{-2} + 1$$

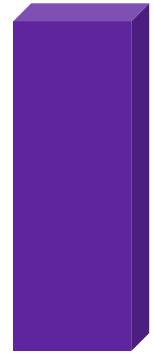


$$\underline{\underline{\sigma}} = \left[ \left( 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}_1} + 2 \underline{\underline{I}}_1 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \right) \underline{\underline{F}}^t \underline{\underline{F}} - 2 \frac{\partial \Psi}{\partial \underline{\underline{I}}_2} \underline{\underline{F}}^t \underline{\underline{\underline{F}}} \underline{\underline{F}}^t \underline{\underline{F}} \right] + c \underline{\underline{I}}$$

# Identification procedure

## Planar tension

$$\frac{\lambda F}{S_0} = \left[ \left( 2 \frac{\partial \Psi}{\partial I_1} + 2(\lambda^2 + \lambda^{-2} + 1) \frac{\partial \Psi}{\partial I_2} \right) (\lambda^2 - \lambda^{-2}) - 2 \frac{\partial \Psi}{\partial I_2} (\lambda^4 - \lambda^{-4}) \right]$$



$$\frac{F}{S_0} = 2(\lambda - \lambda^{-3}) \left( \frac{\partial \Psi}{\partial I_1} + \frac{\partial \Psi}{\partial I_2} \right)$$

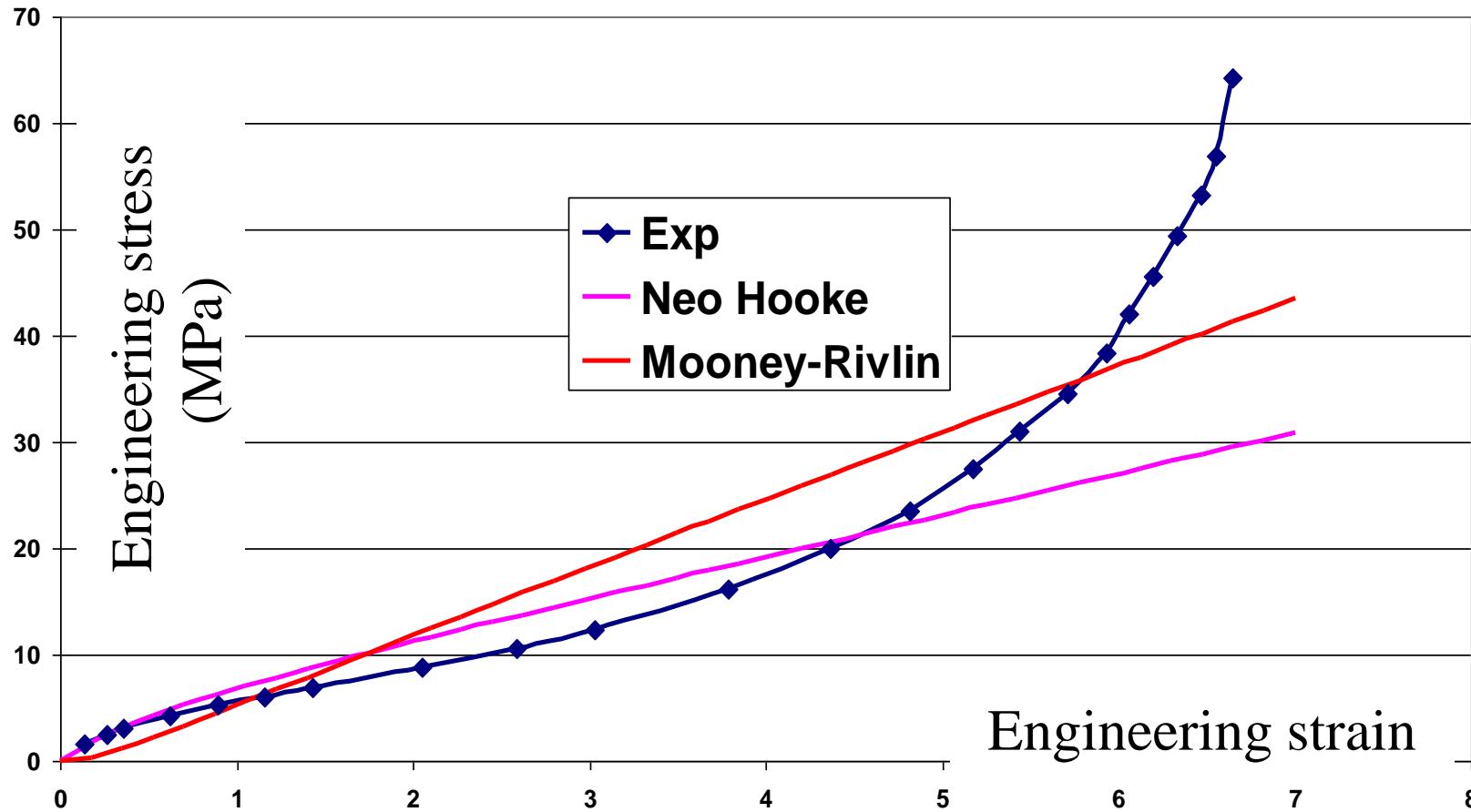
Remark:

$$I_1 = \lambda^2 + \lambda^{-2} + 1 \quad I_2 = \lambda^2 + \lambda^{-2} + 1$$

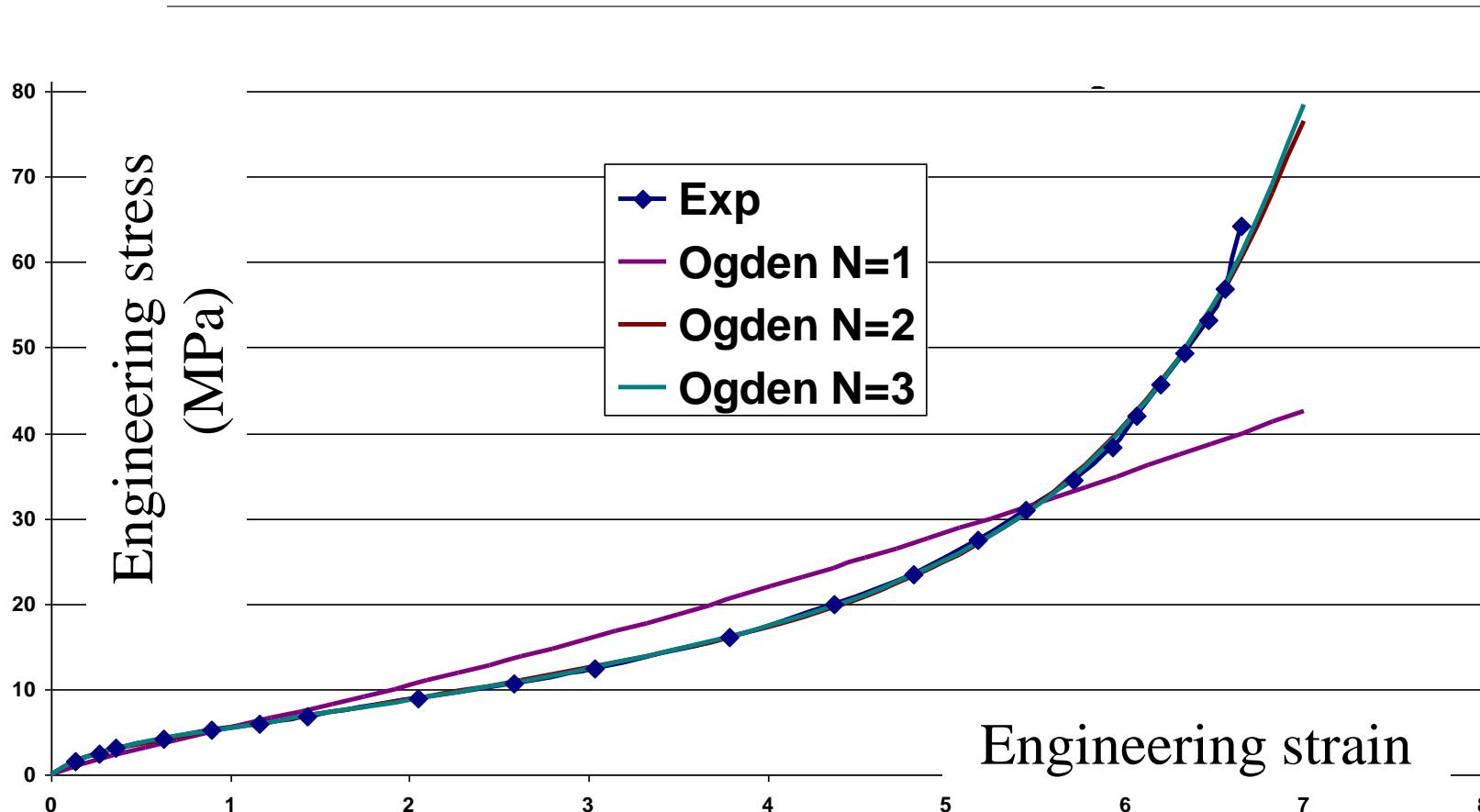
$$\frac{dI_1}{d\lambda} = 2(\lambda - \lambda^{-3}) \quad \frac{dI_2}{d\lambda} = 2(\lambda - \lambda^{-3})$$

$$\frac{F}{S_0} = \frac{\partial \Psi}{\partial \lambda}$$

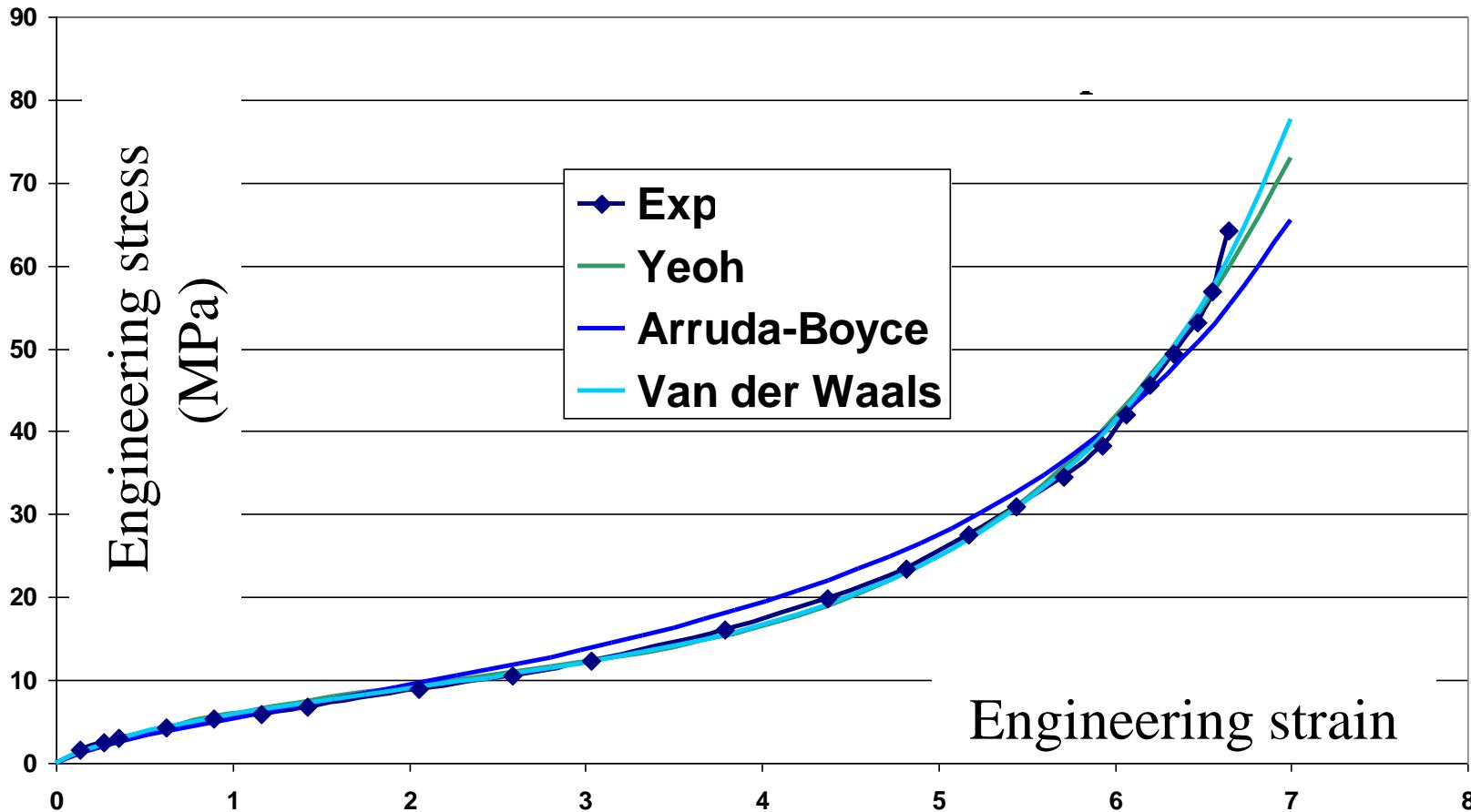
# Identification of parameters from the data of the uniaxial tensile test only



# Identification of parameters from the data of the uniaxial tensile test only

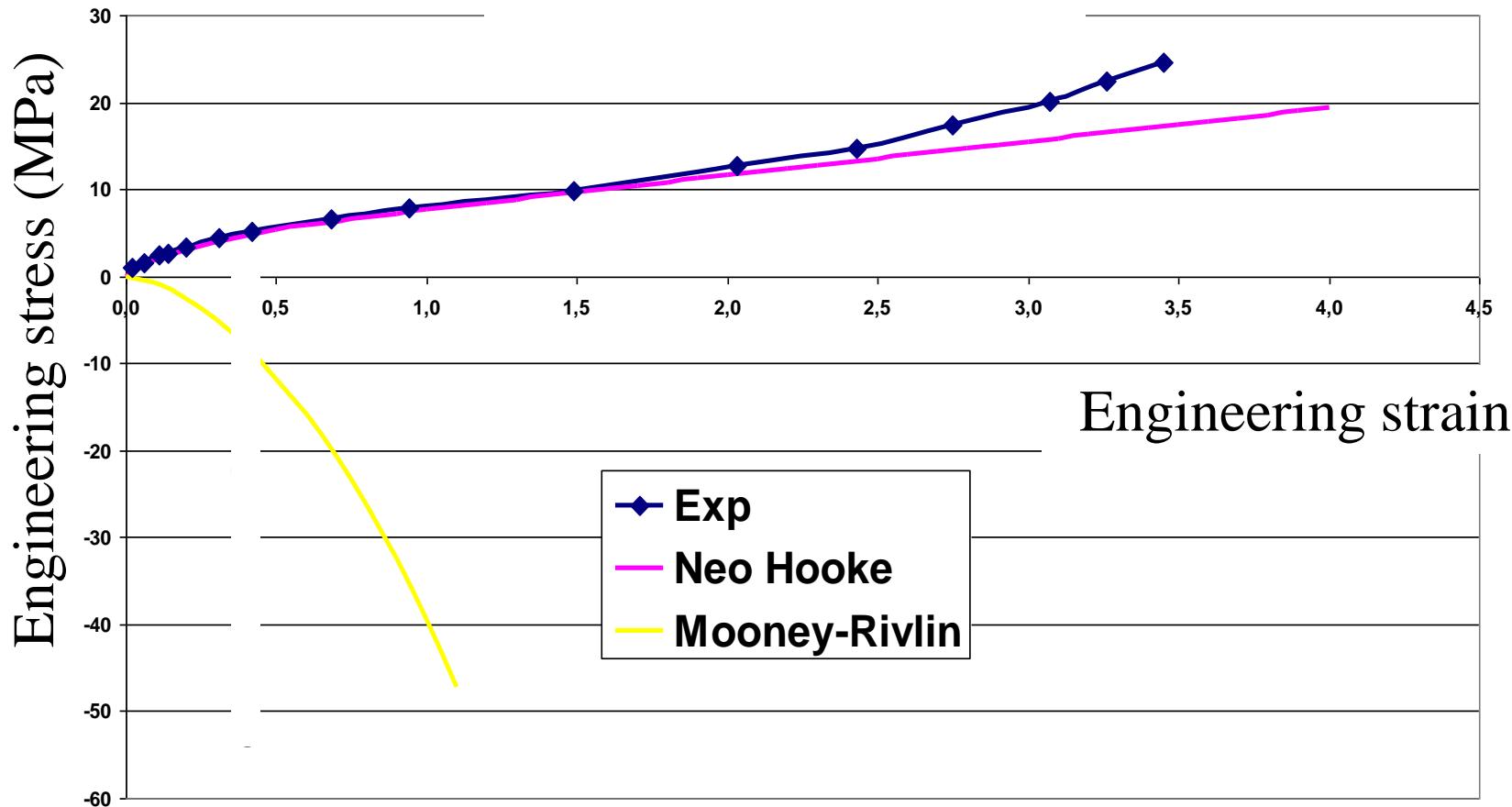


# Identification of parameters from the data of the uniaxial tensile test only



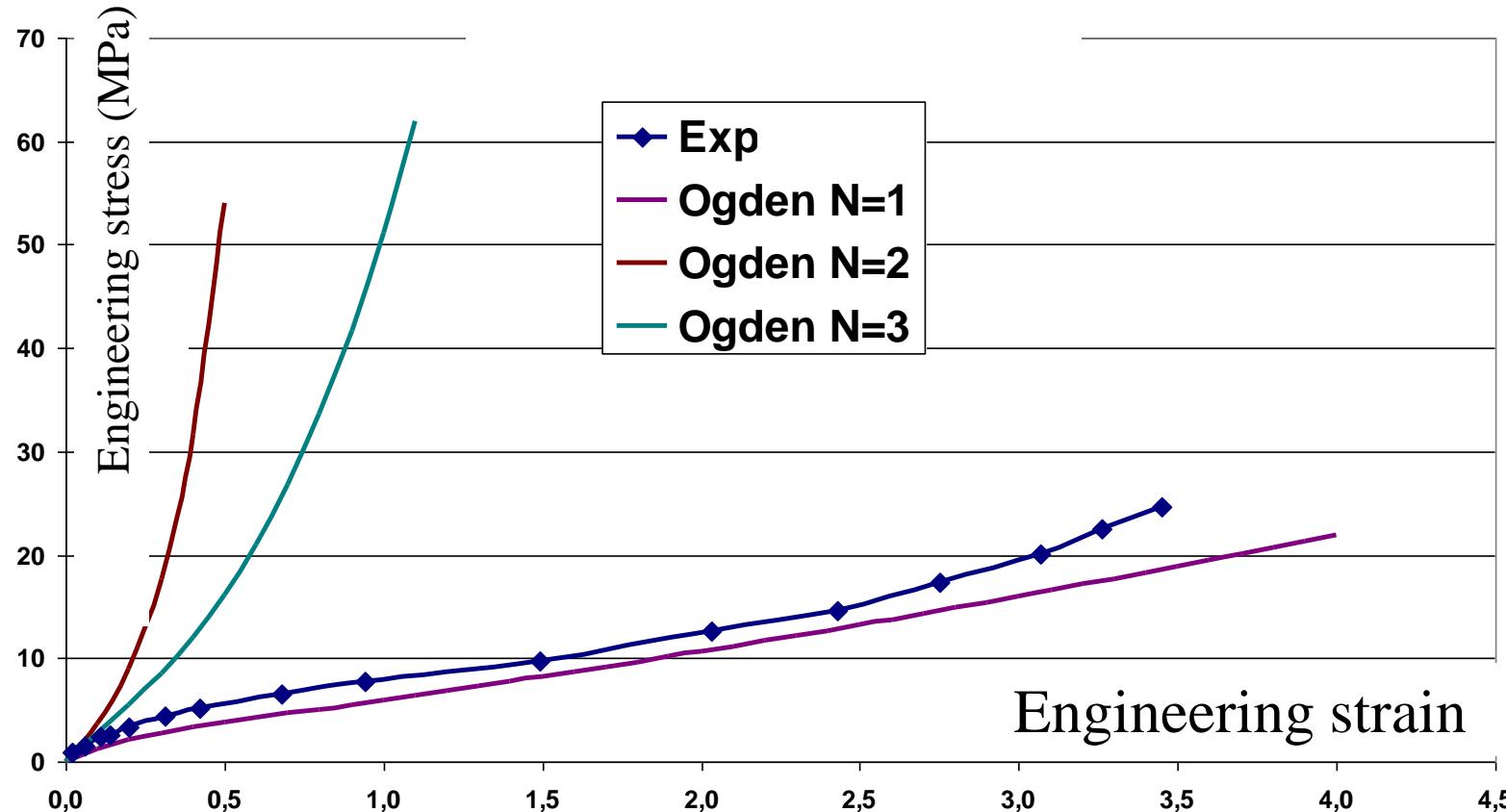
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the planar tension data



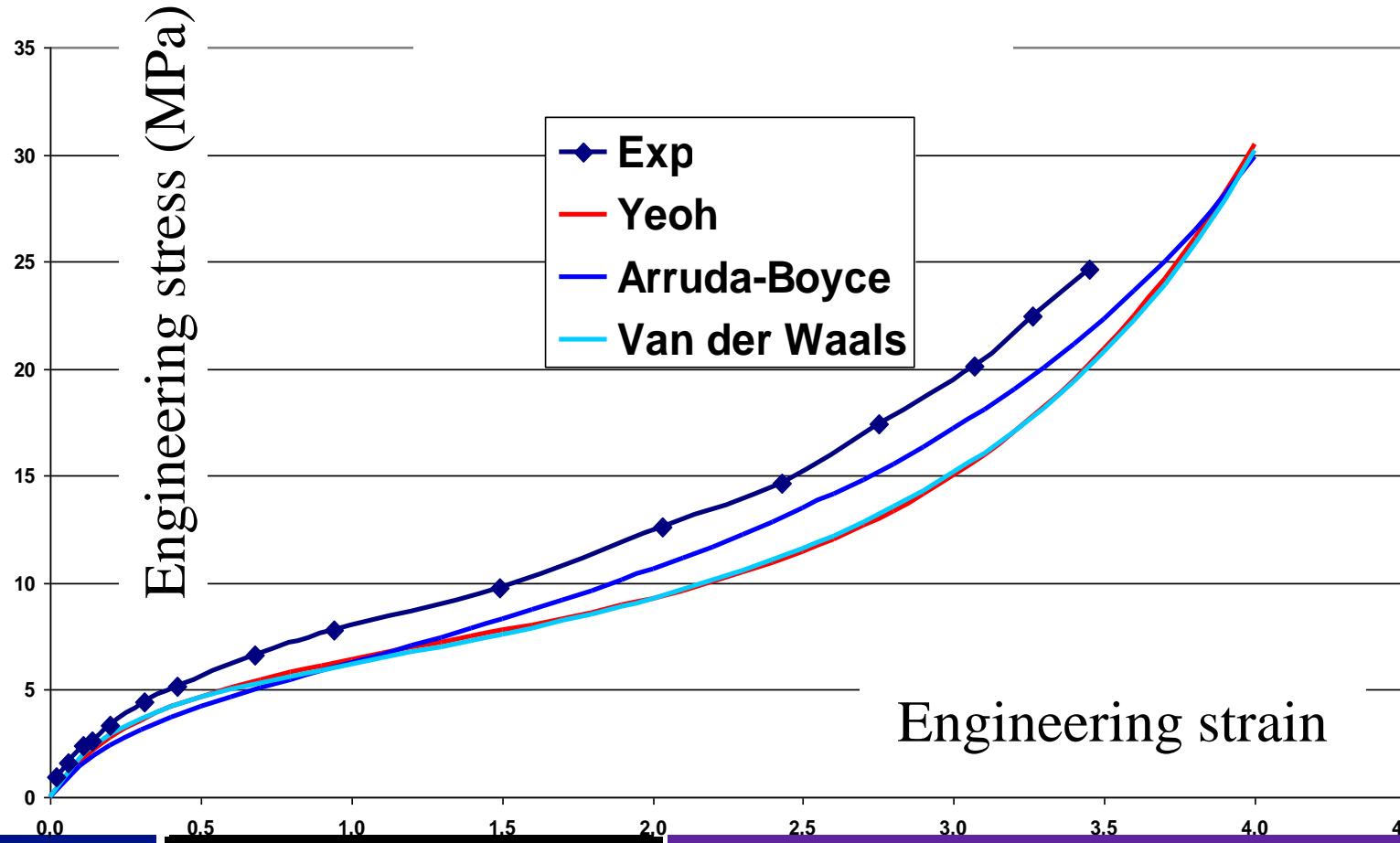
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the planar tension data



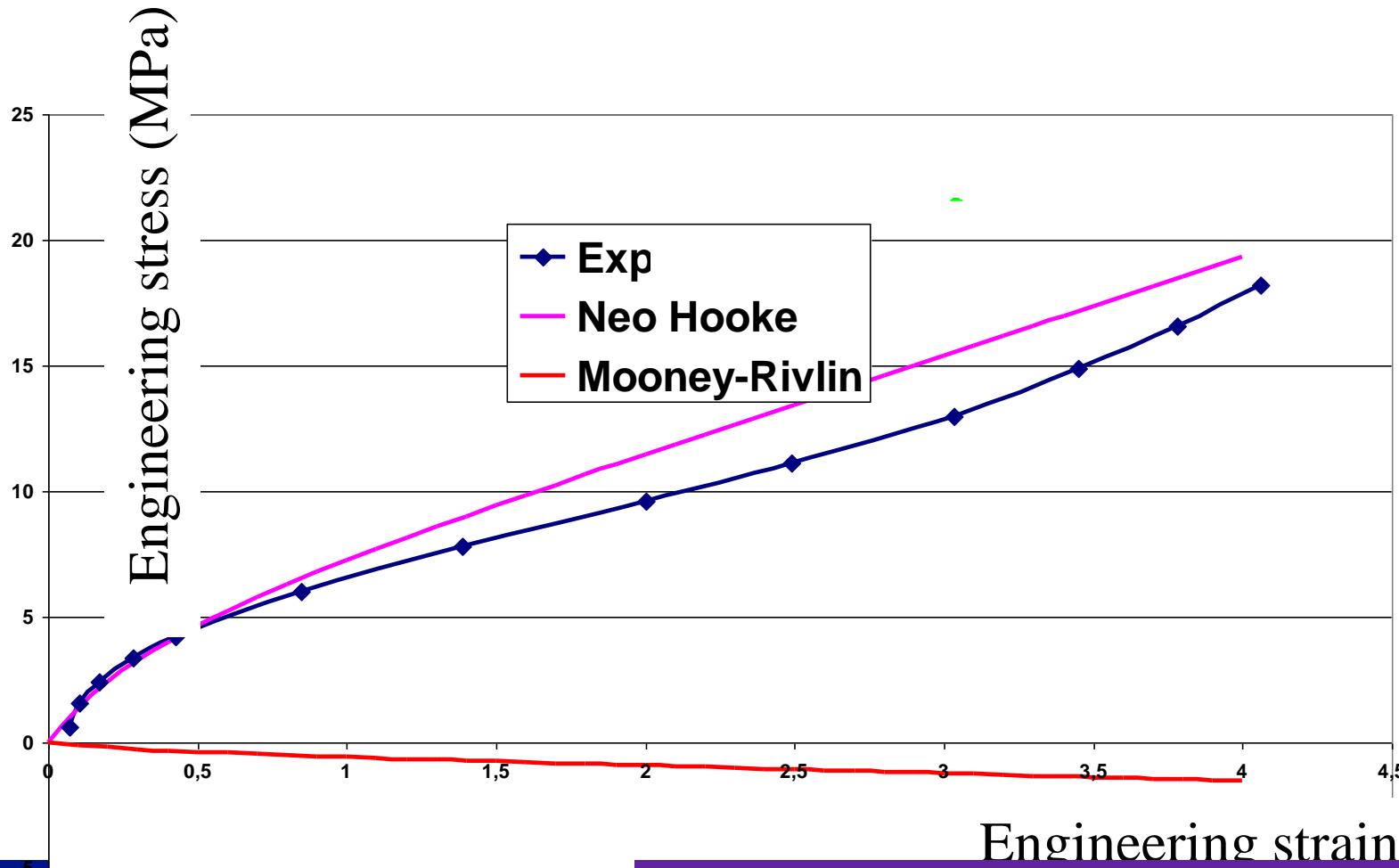
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the planar tension data



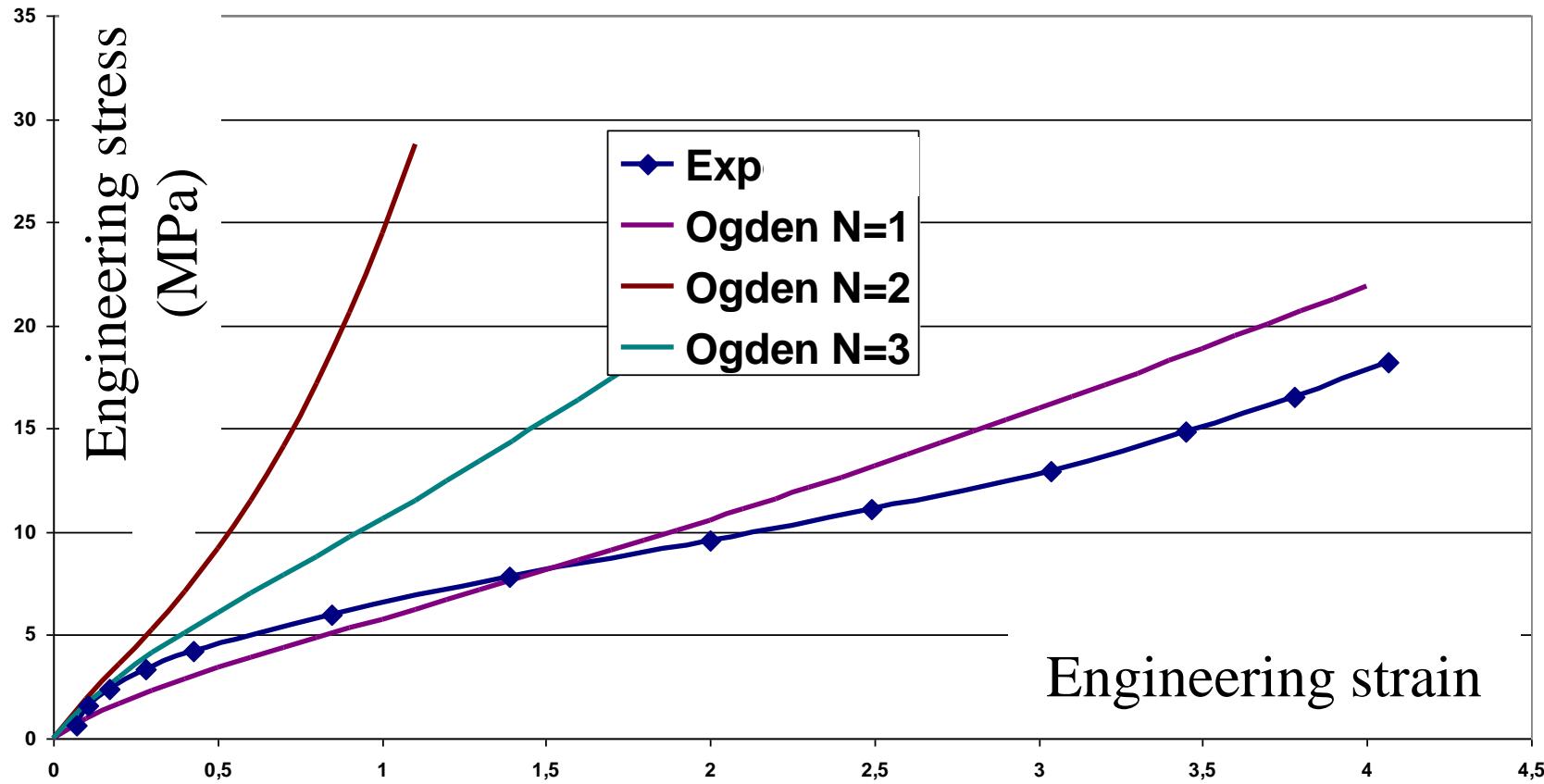
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the biaxial tension data



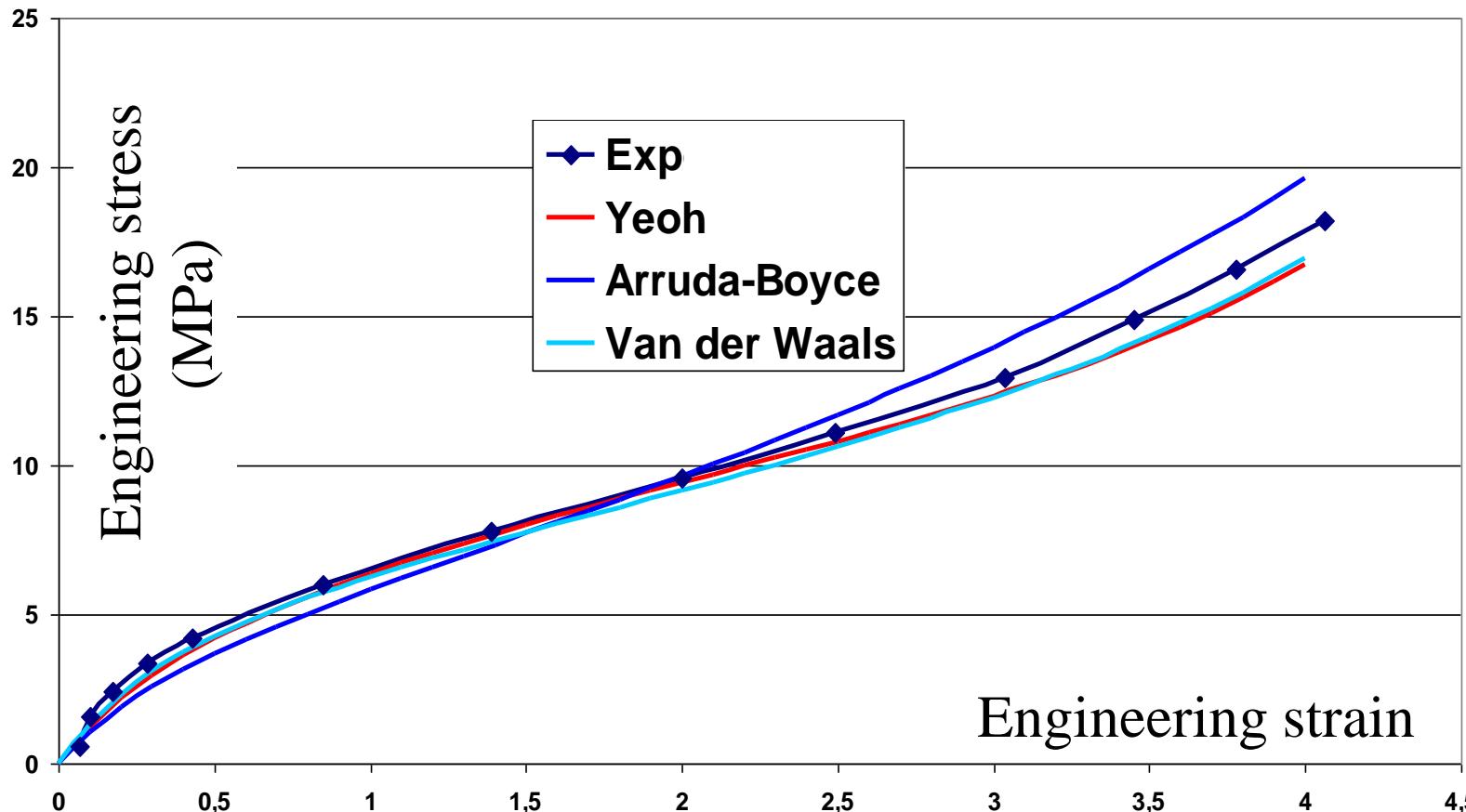
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the biaxial tension data



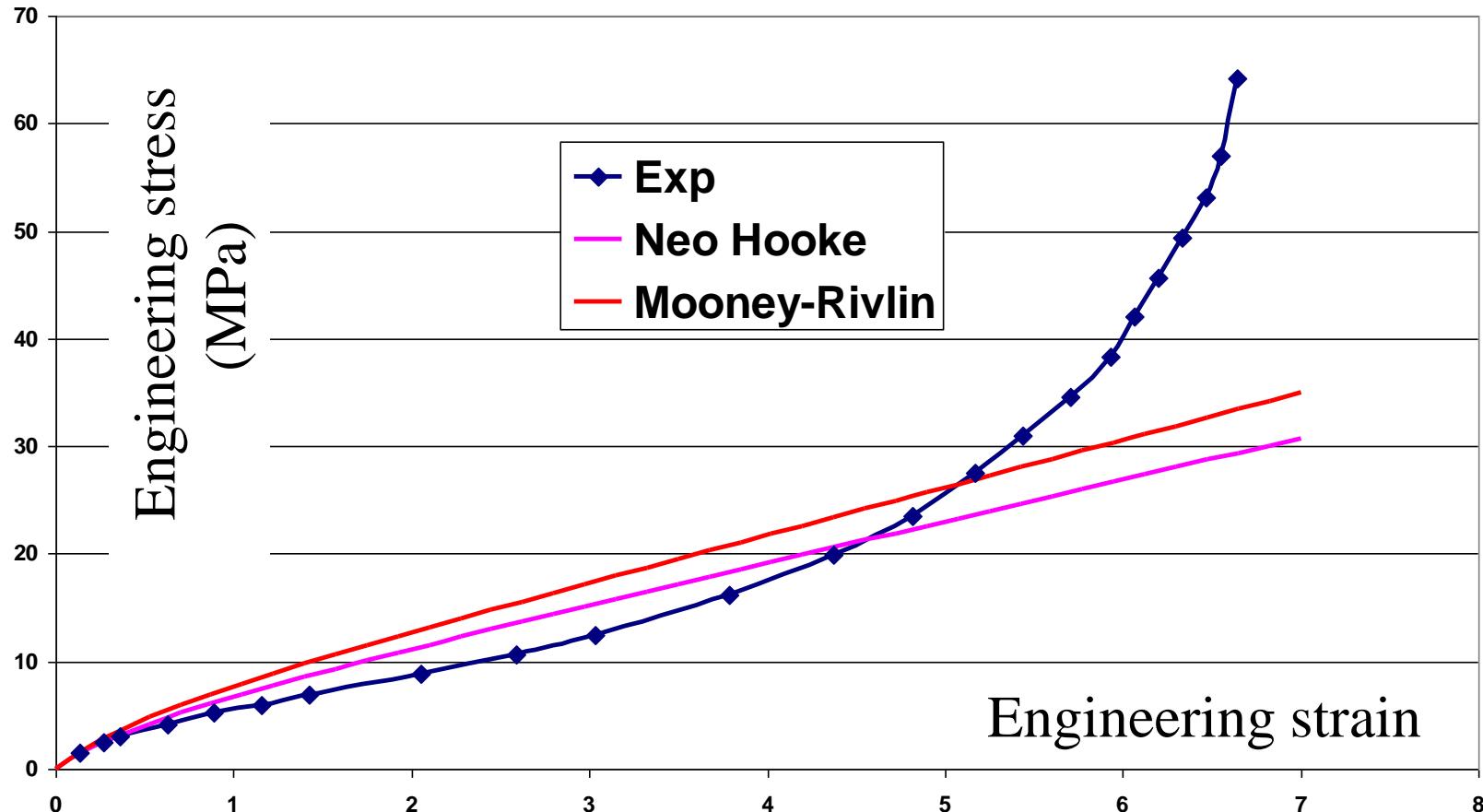
# Identification of parameters from the data of the uniaxial tensile test only

## Prediction of the planar tension data



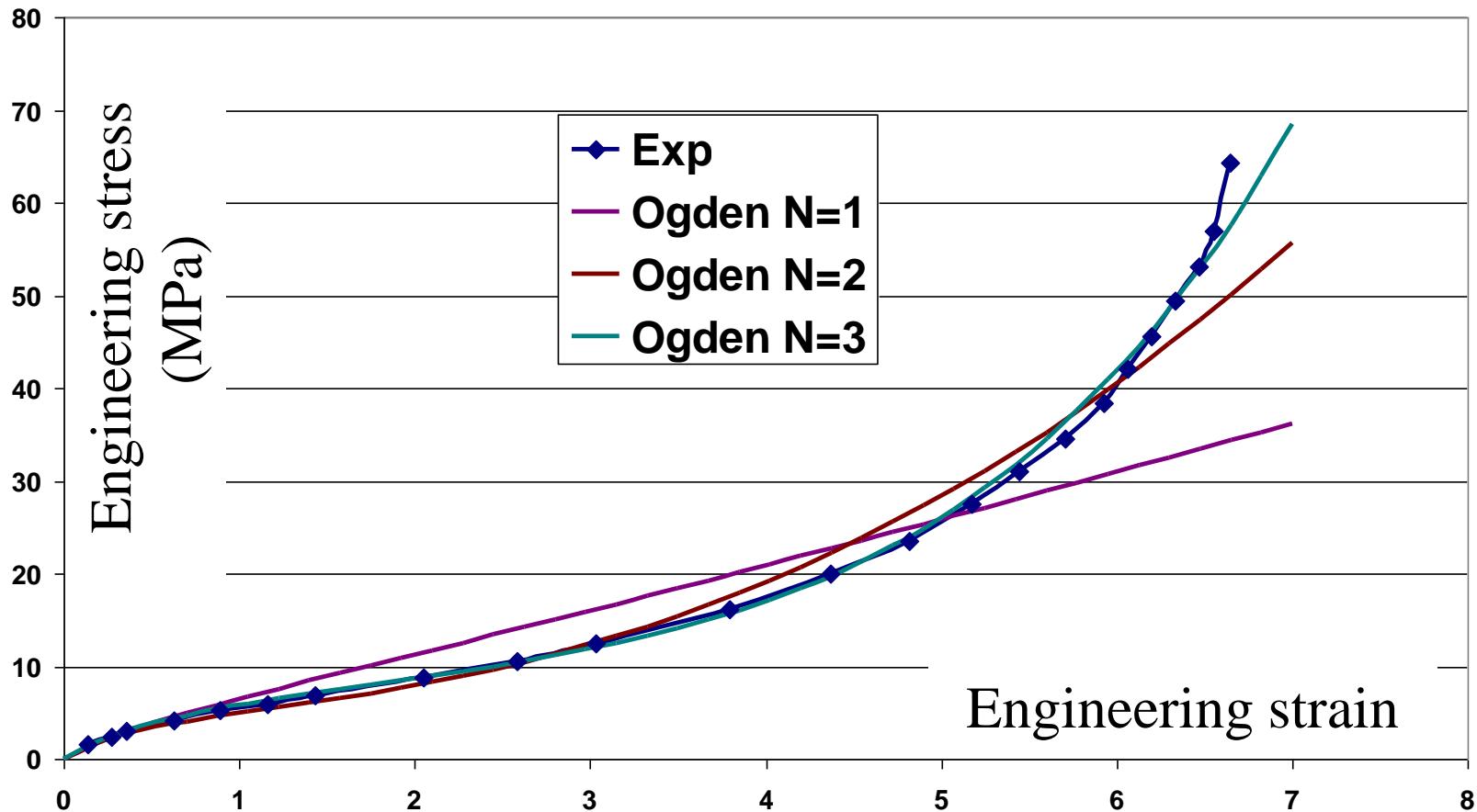
# Identification of parameters from all the data

## Prediction of the uniaxial tensile test



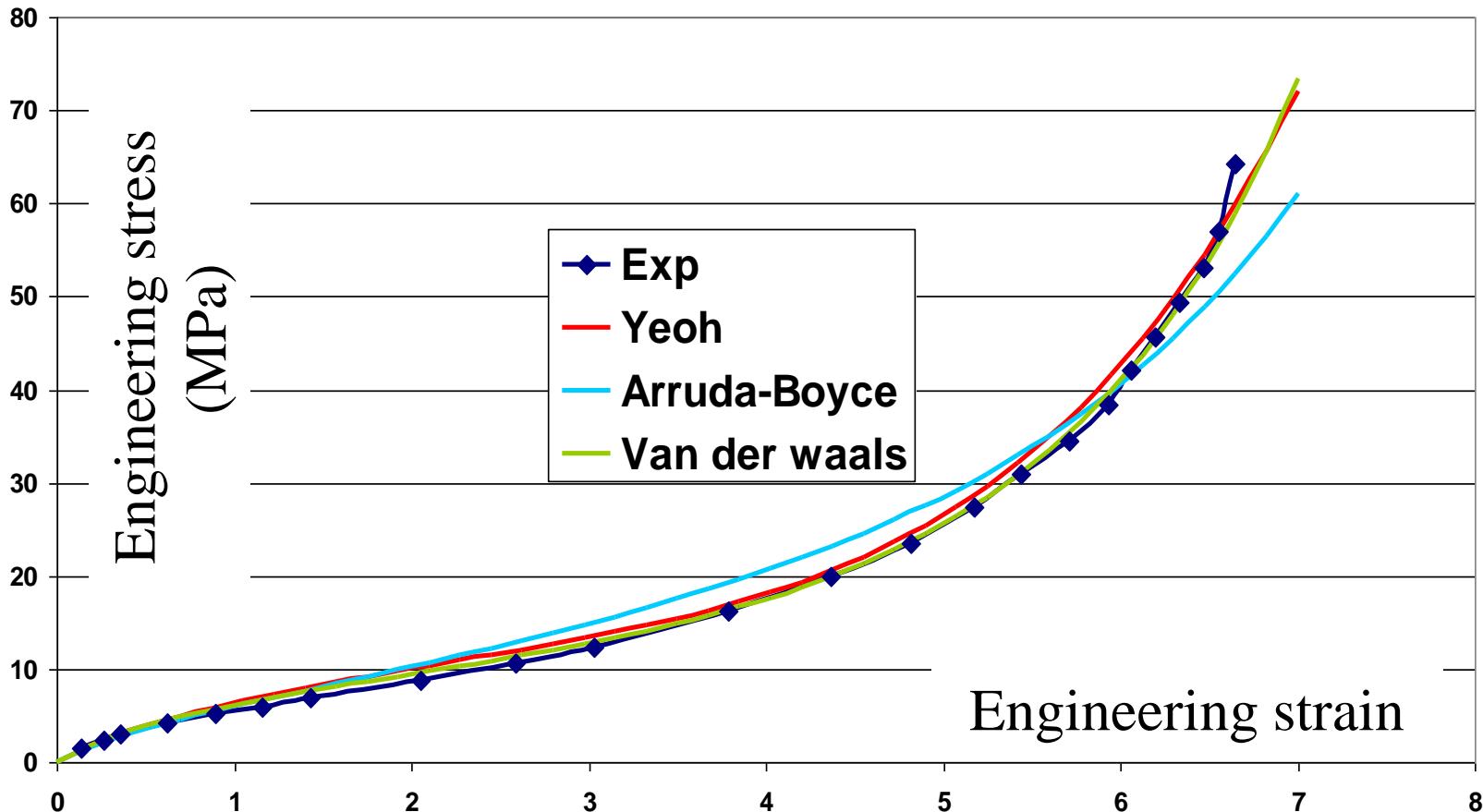
# Identification of parameters from all the data

## Prediction of the uniaxial tensile test



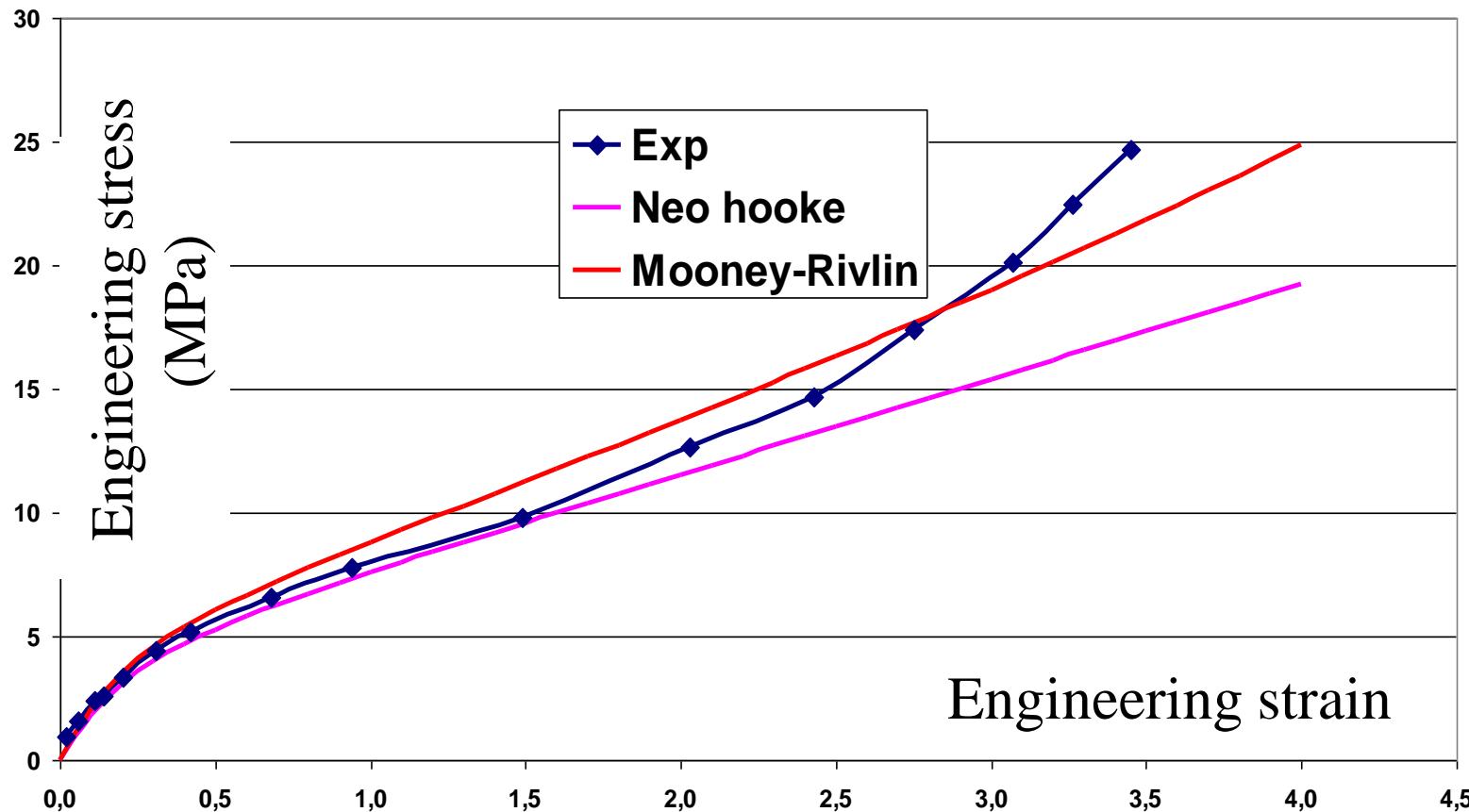
# Identification of parameters from all the data

## Prediction of the uniaxial tensile test



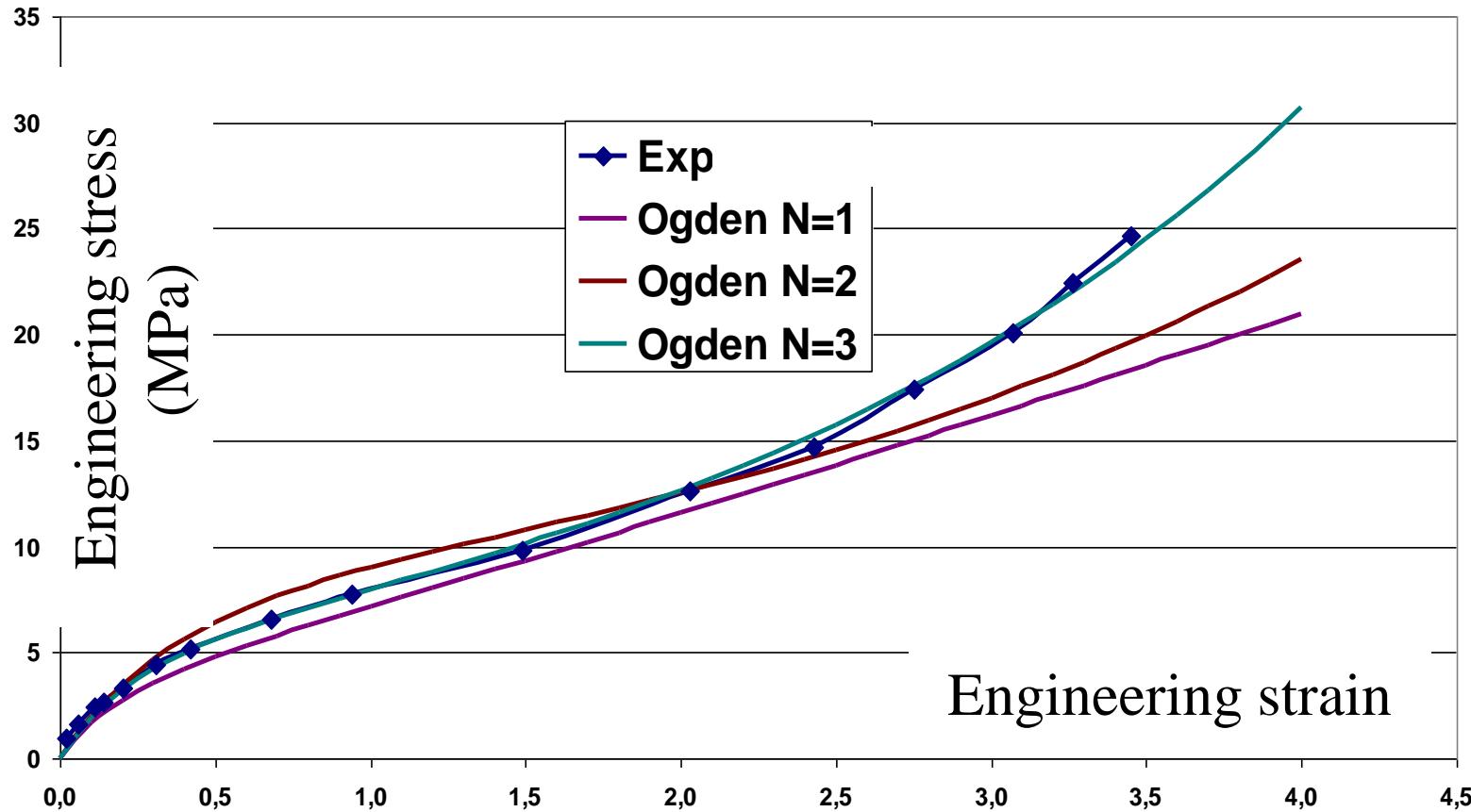
# Identification of parameters from all the data

## Prediction of the planar tensile test



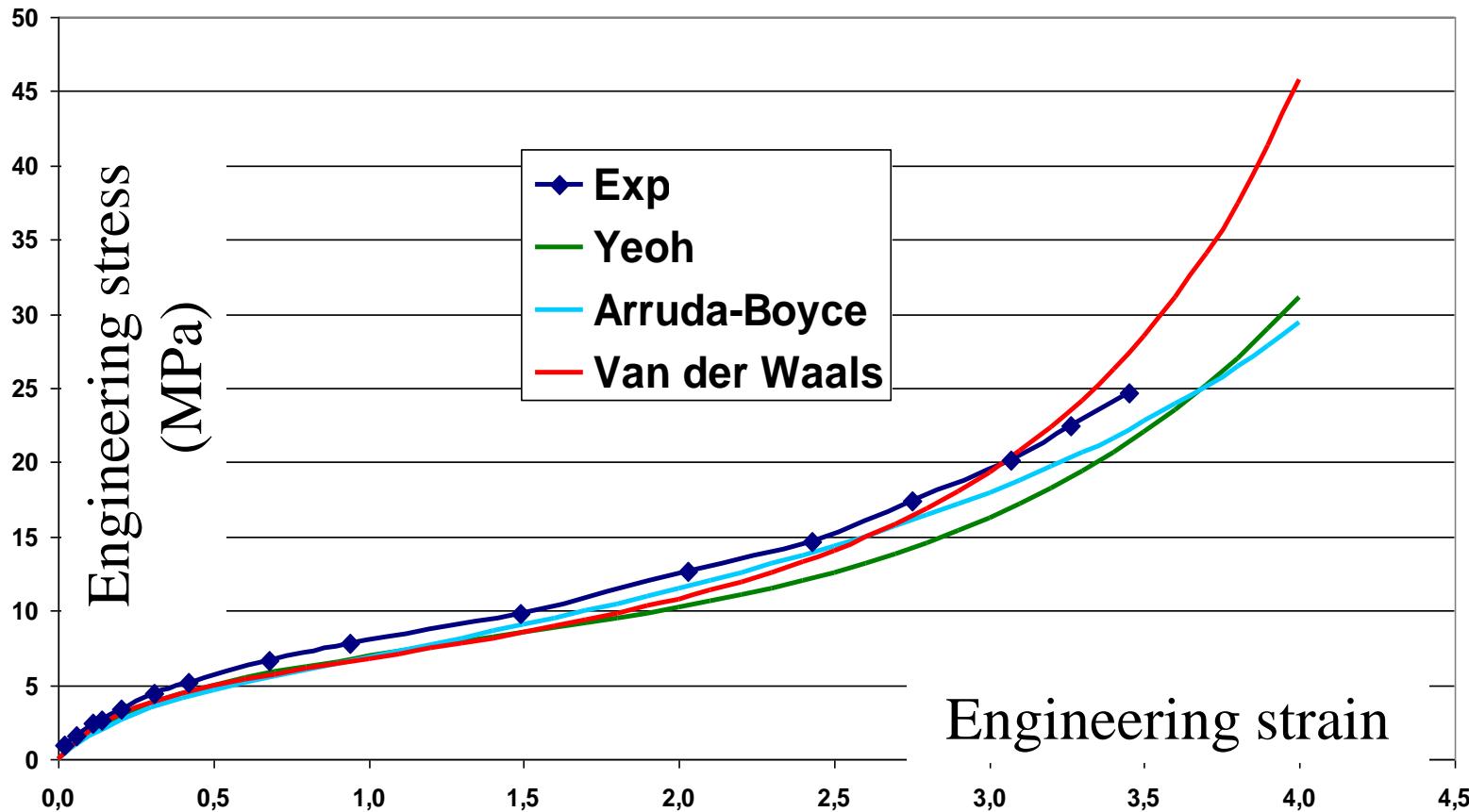
# Identification of parameters from all the data

## Prediction of the planar tensile test



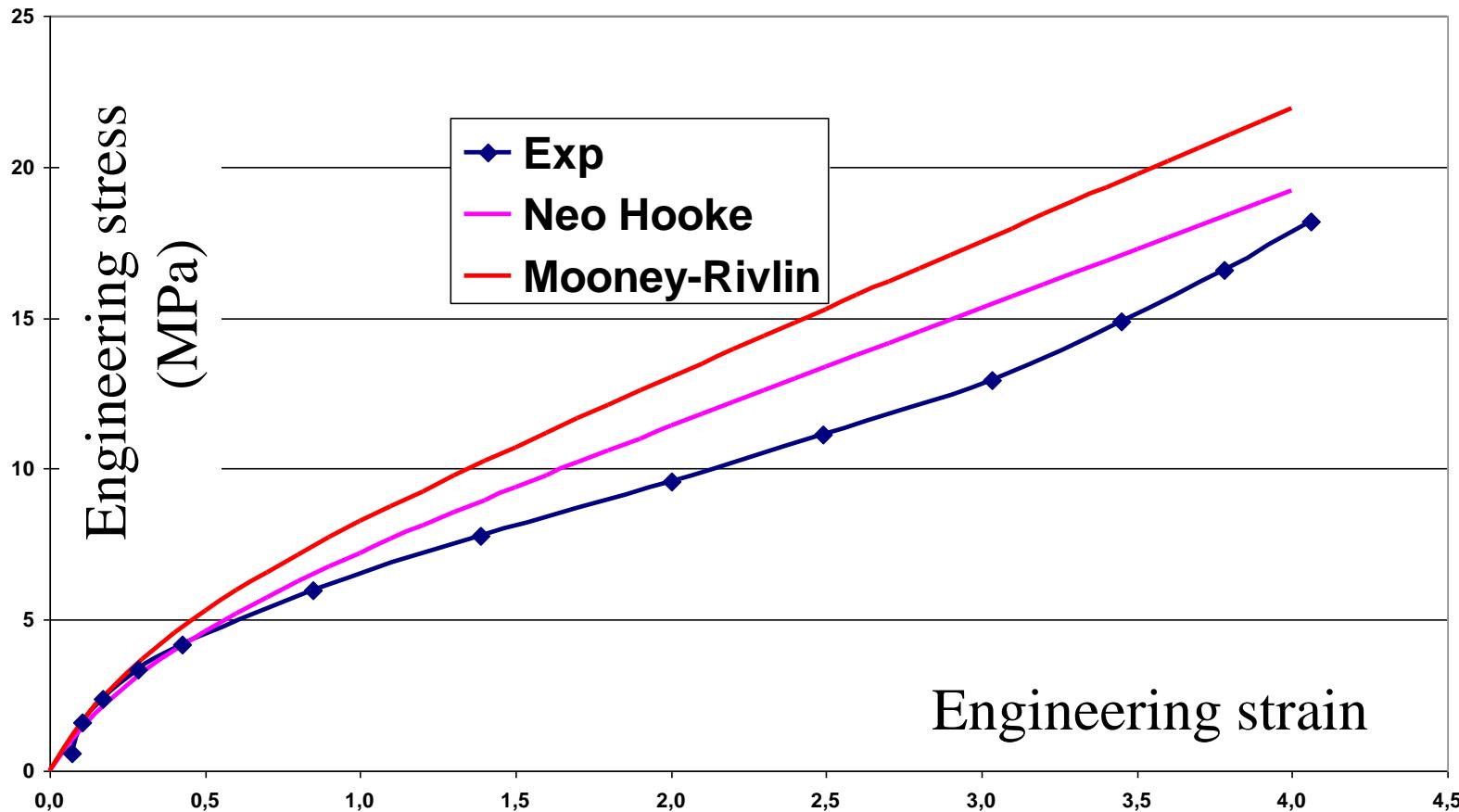
# Identification of parameters from all the data

## Prediction of the uniaxial tensile test



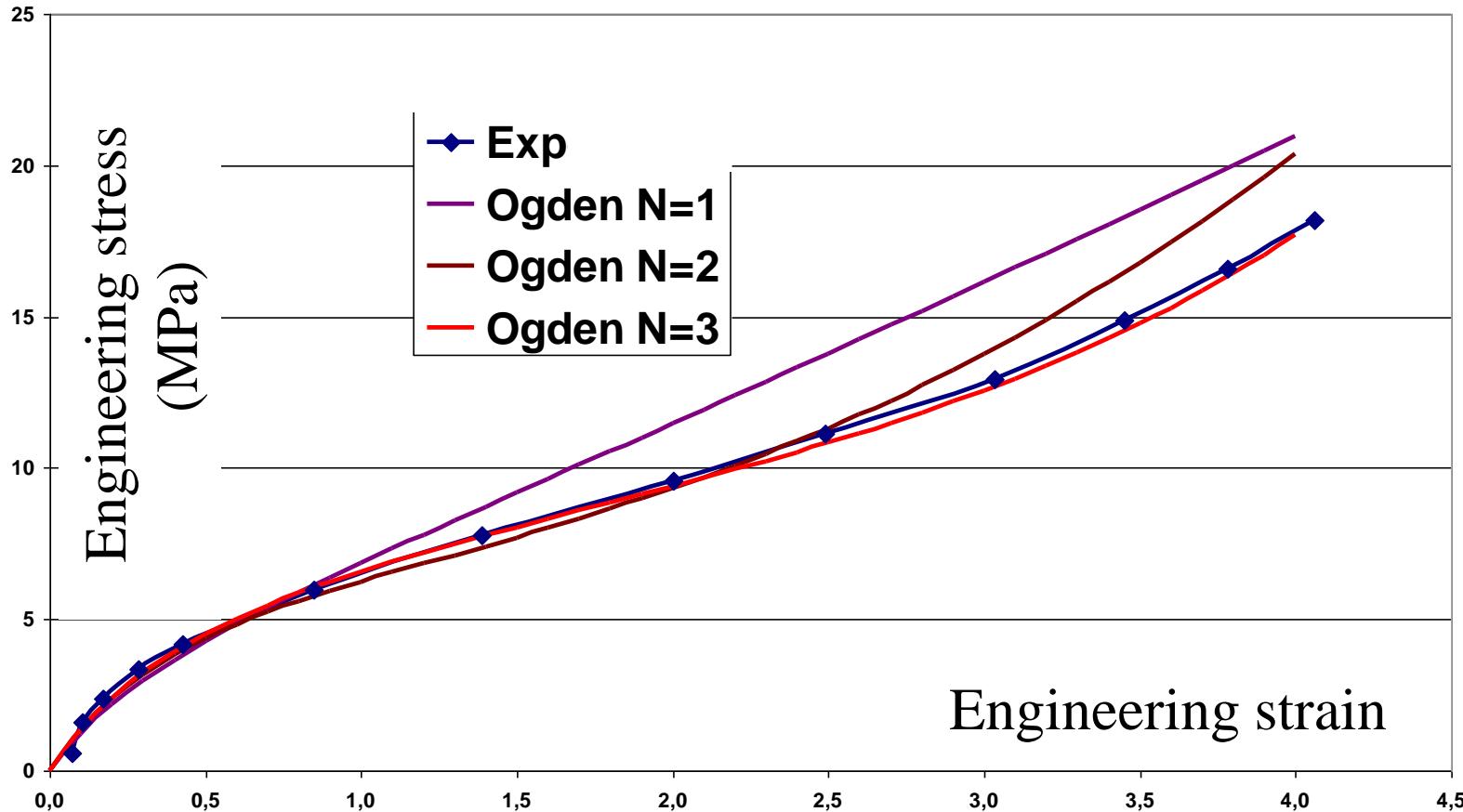
# Identification of parameters from all the data

## Prediction of the biaxial tensile test



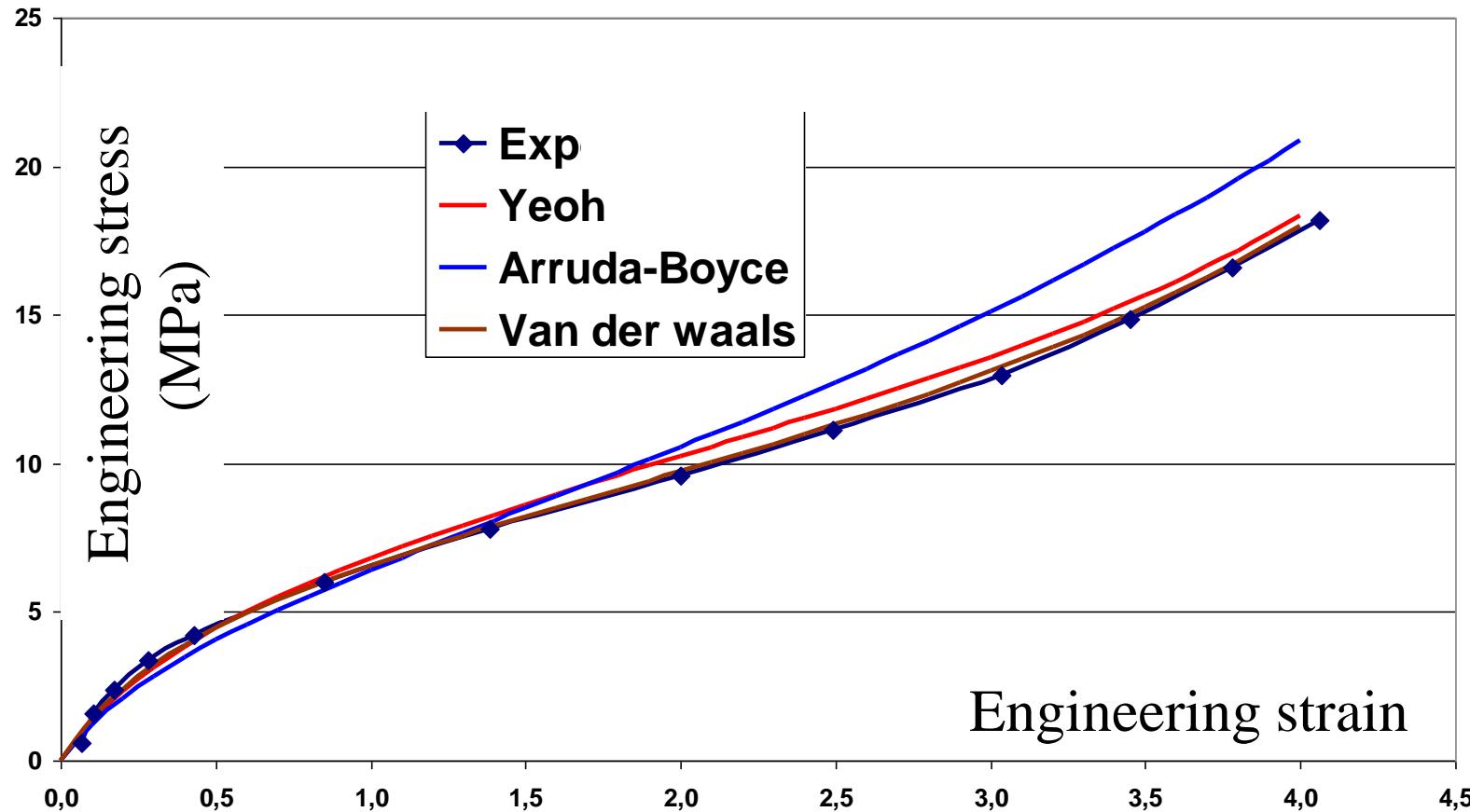
# Identification of parameters from all the data

## Prediction of the biaxial tensile test

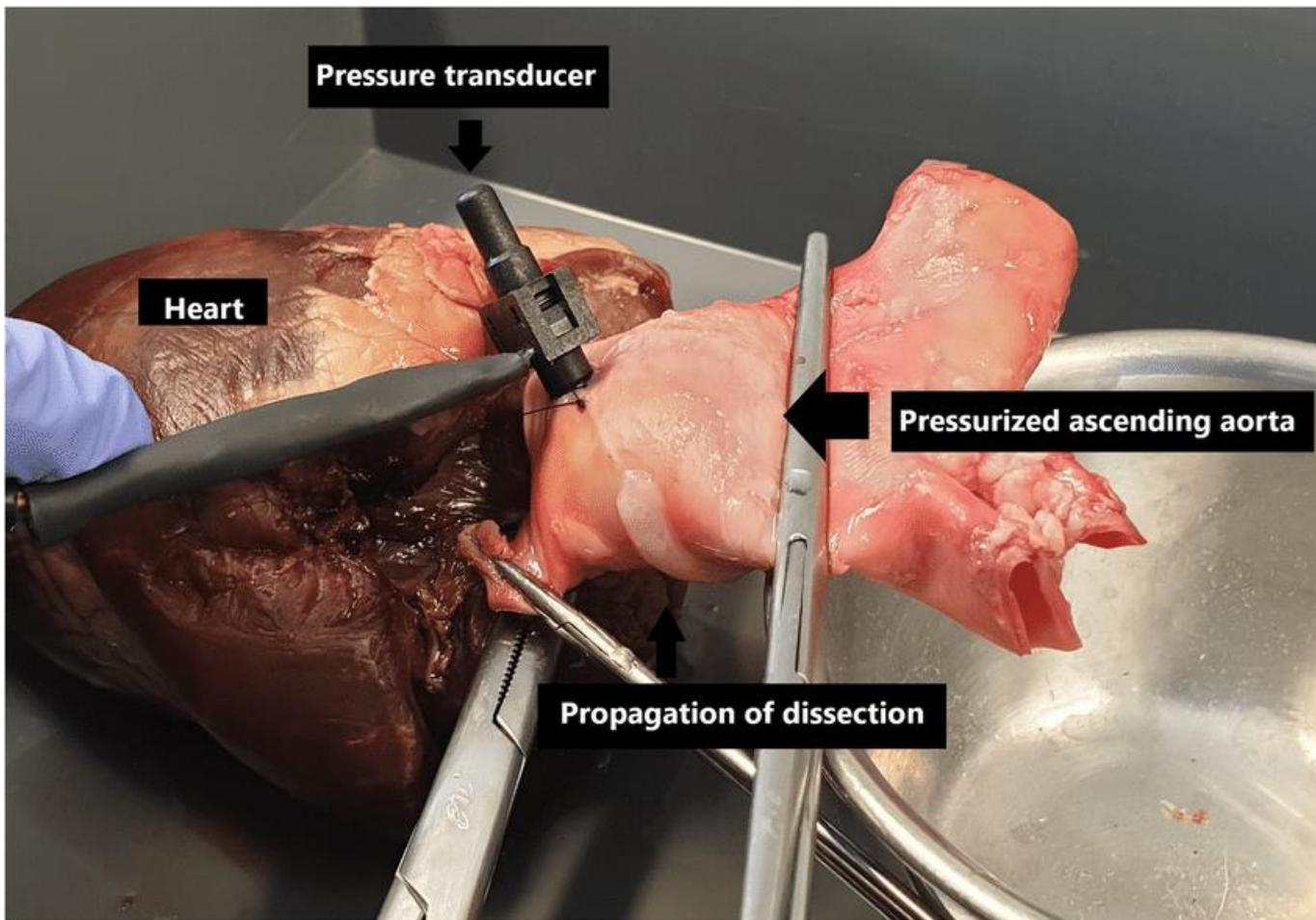


# Identification of parameters from all the data

## Prediction of the biaxial tensile test



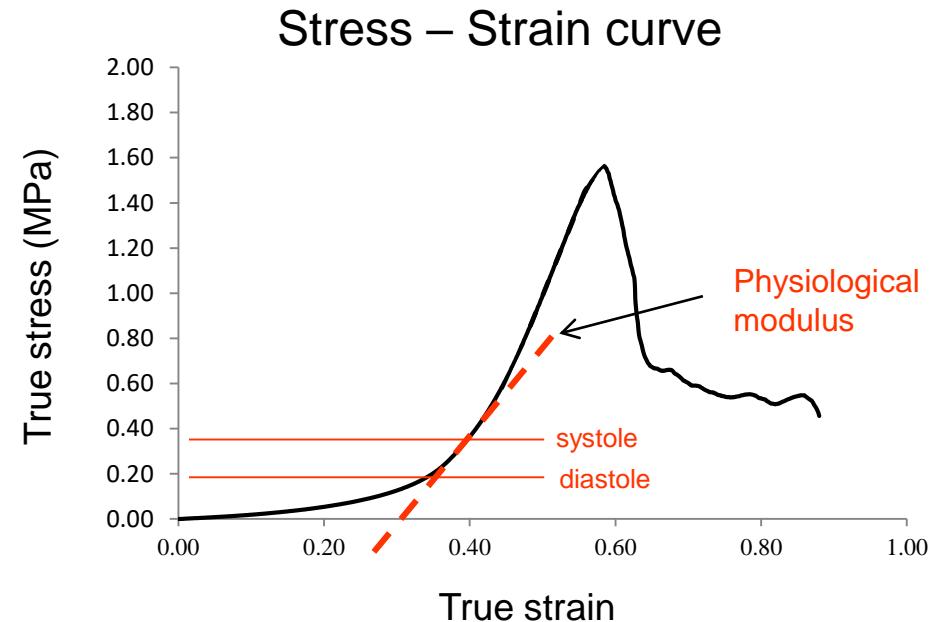
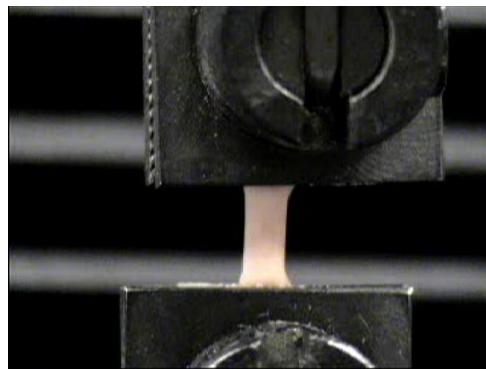
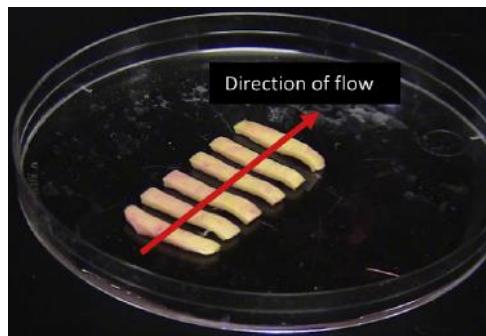
# Testing soft tissues: arteries



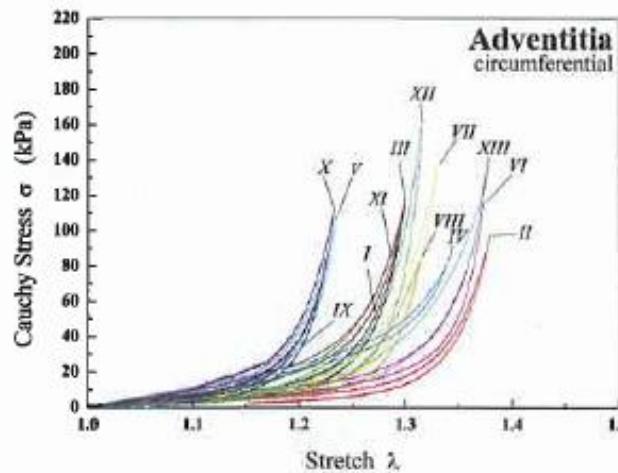
# Tensile test - uniaxial tension



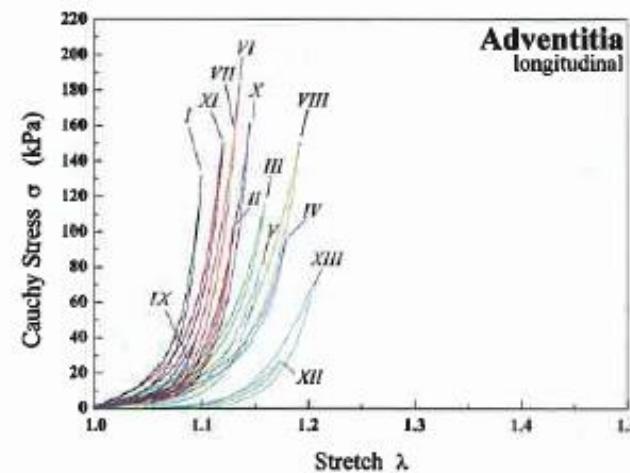
[Duprey, 2010]



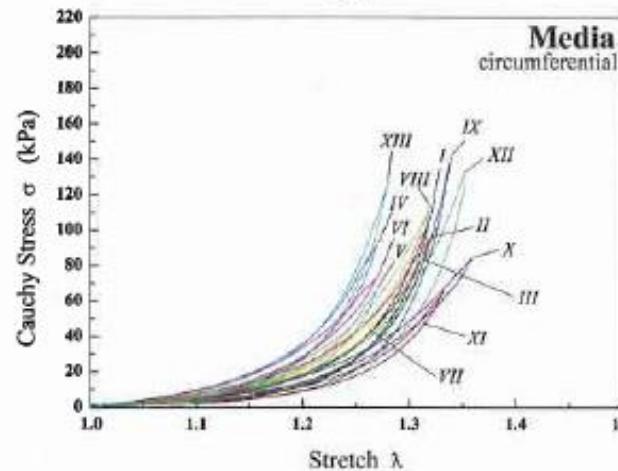
# Tensile test - uniaxial tension



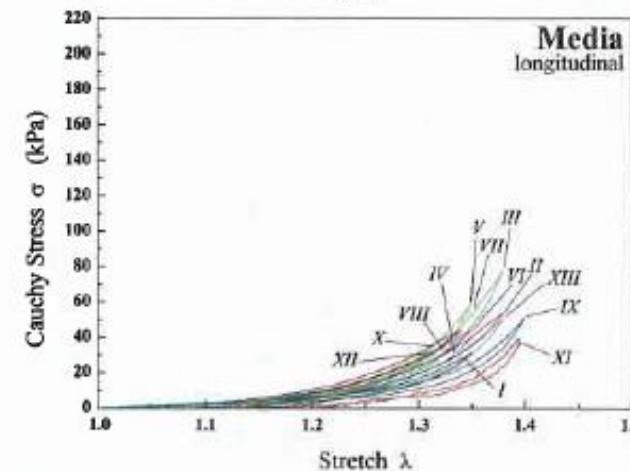
(a)



(b)



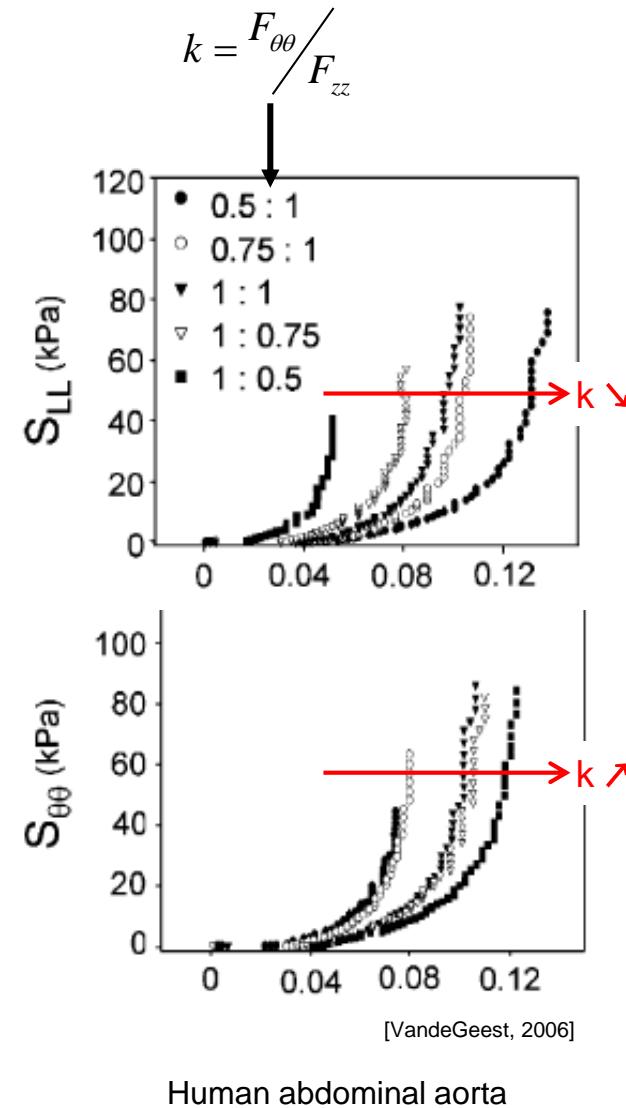
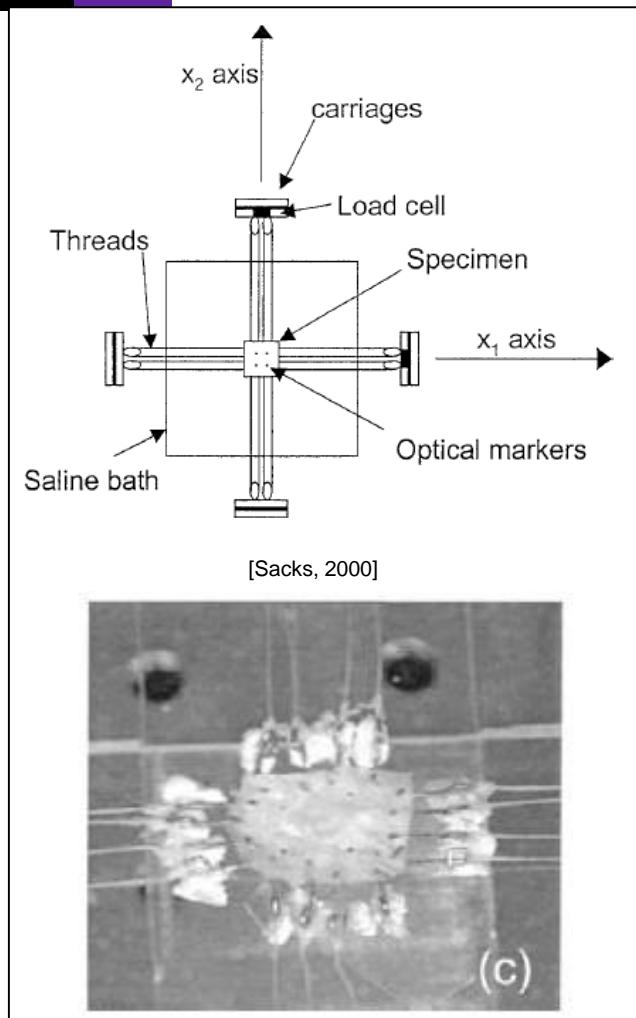
(c)



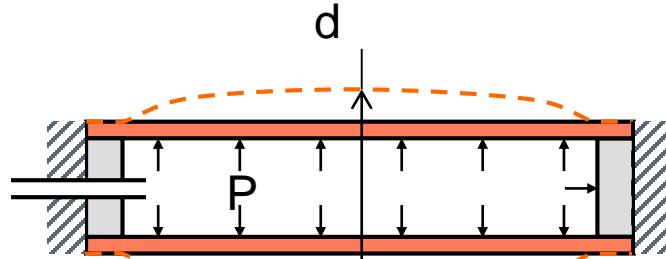
(d)

[Holzapfel, 2005]

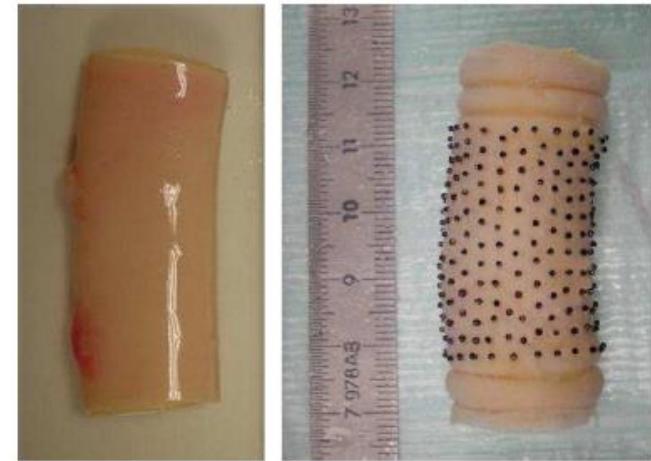
# Biaxial tension



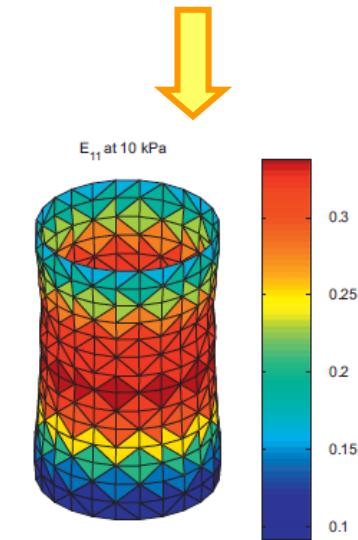
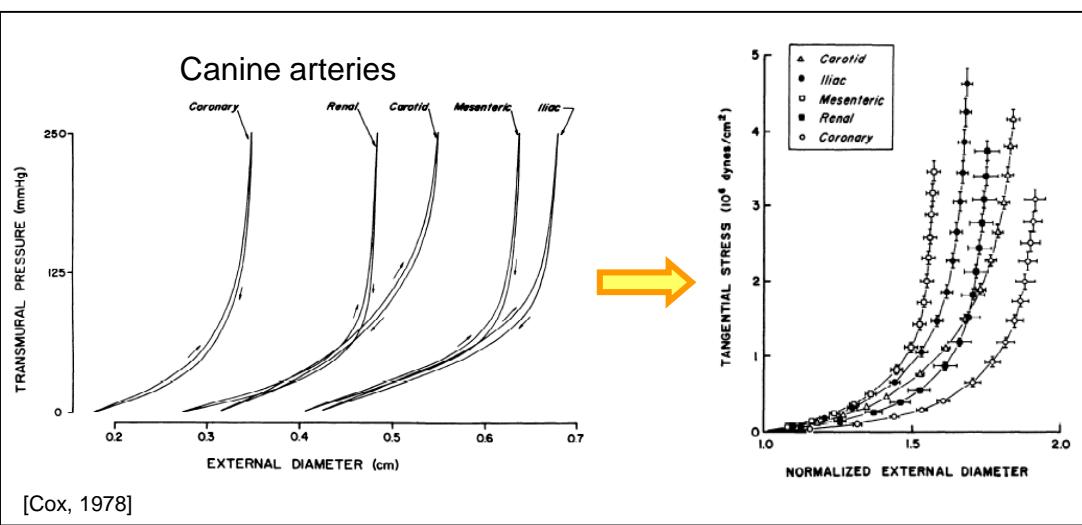
# Tension inflation



→  $P - d$  curve

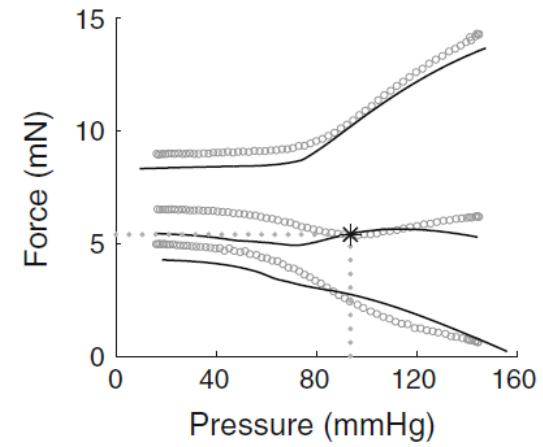
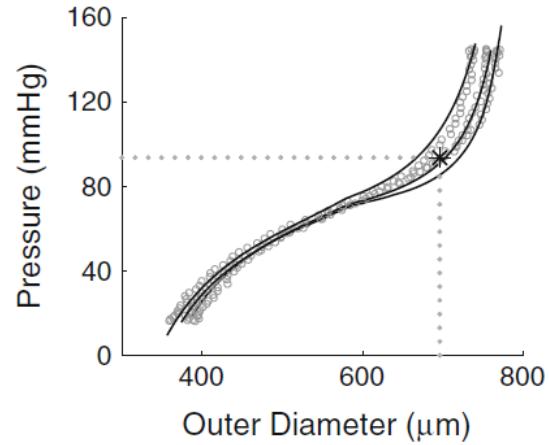
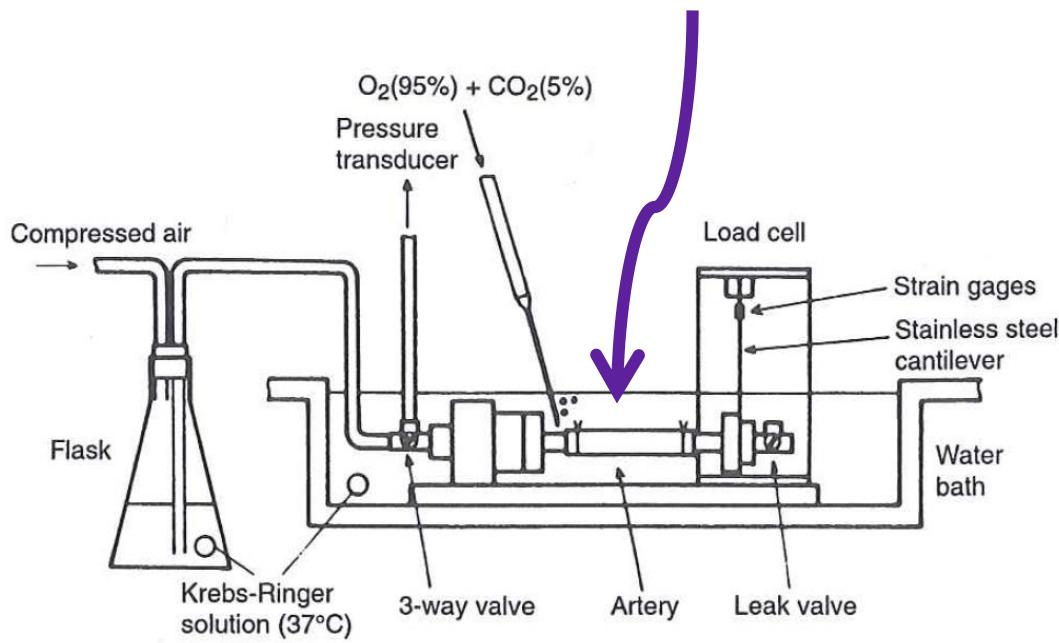


[Genovese, 2009][Avril, 2010](CIS)

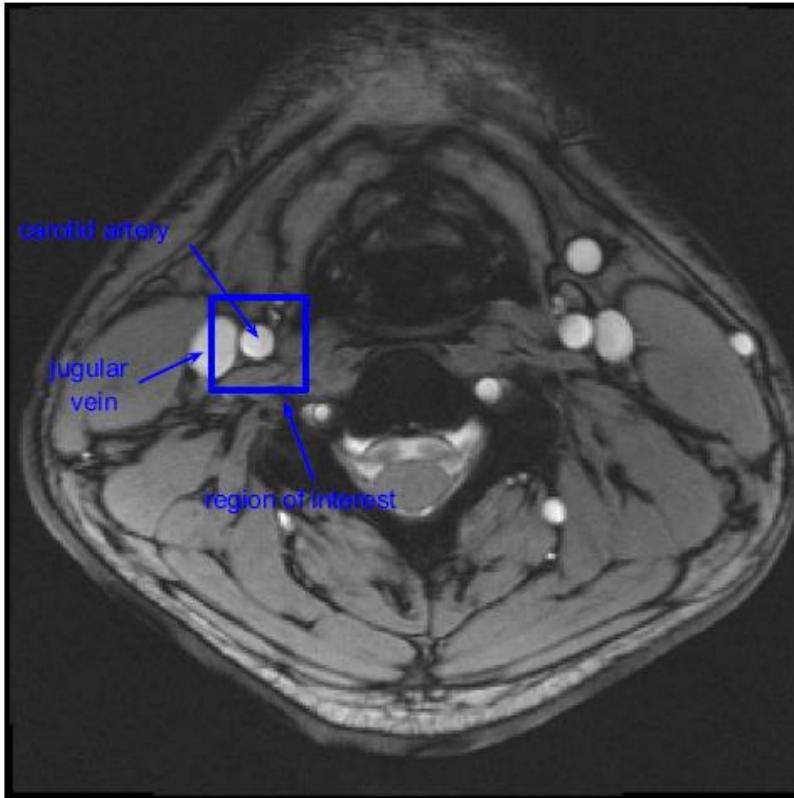


# Tension inflation =

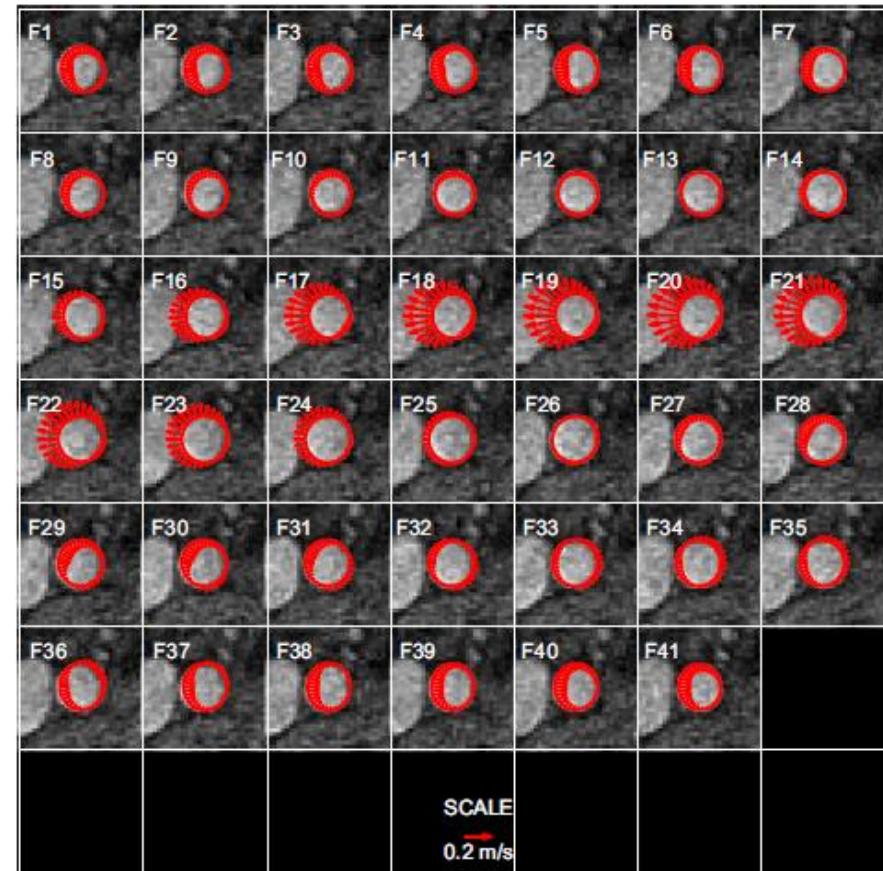
## Functional biomechanical behavior



# In vivo measurements

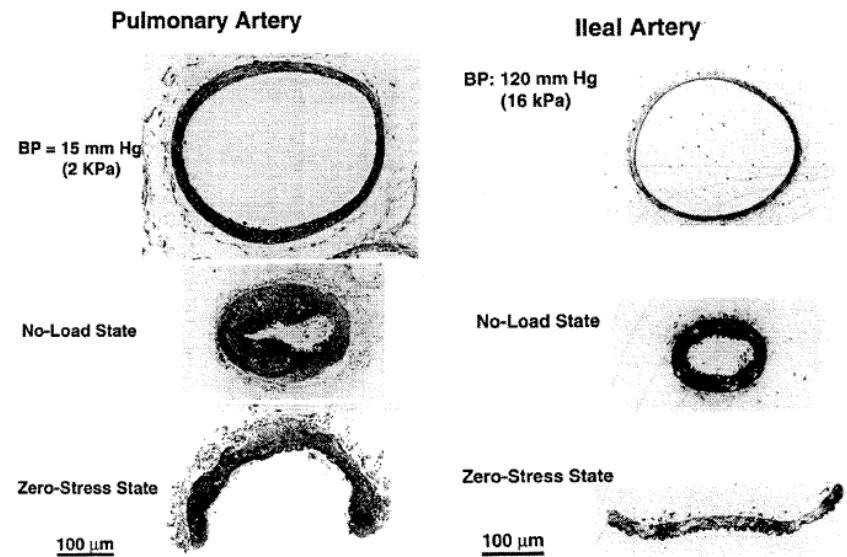
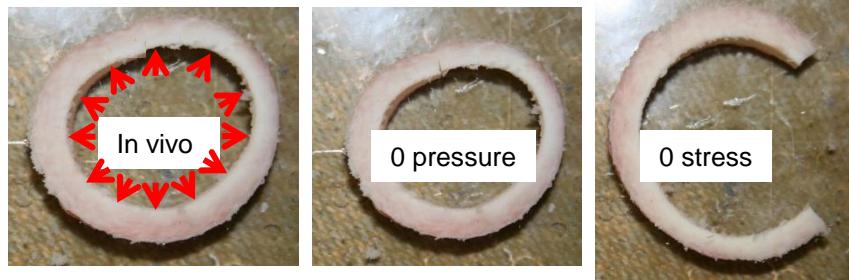


[Avril, 2010]



[Avril, 2011]

# Residual stresses



[Fung, 1993]

# Incompressibility

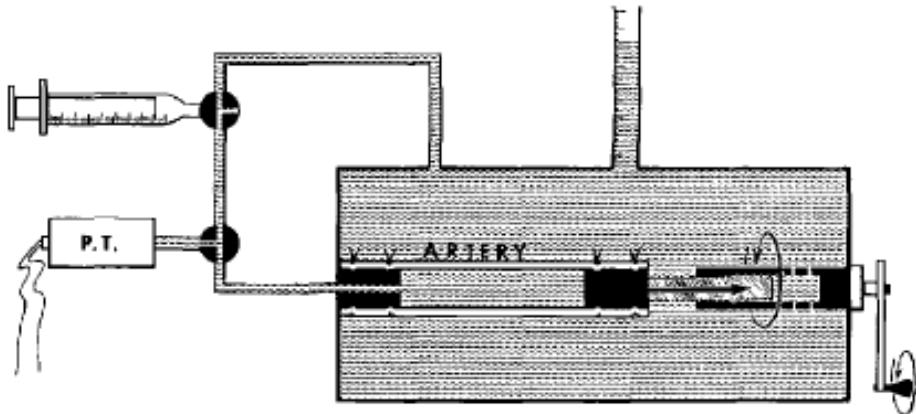


FIGURE 1

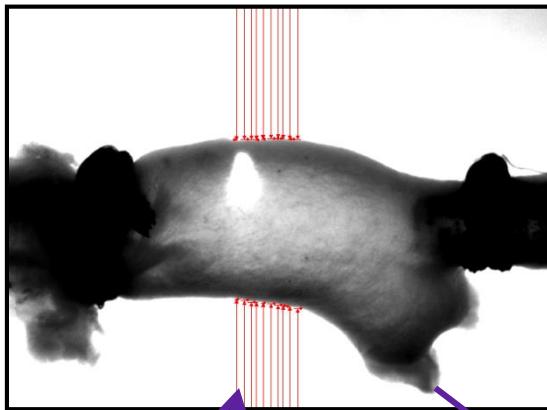
Diagram of experimental set-up. P.T. = pressure transducer. During an experiment the capillary tube shown at the top of the figure was directed horizontally so that changes in fluid level in the tube would not change the static pressure level. Note from the directional arrows that the end of the artery moves to the right without twisting as the crank is advanced.

[Carew, 1968]

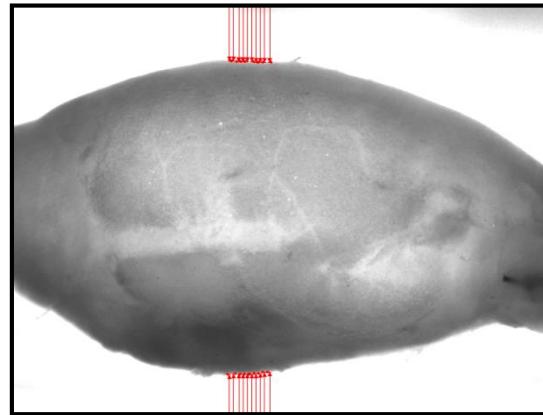
$$K = \frac{p_{tissu}}{\Delta V/V_0} = \frac{tr(\underline{\underline{\sigma}})/3}{\Delta V/V_0} \quad \gg \quad G = \frac{E}{2(1+\nu)}$$

# Advanced investigations

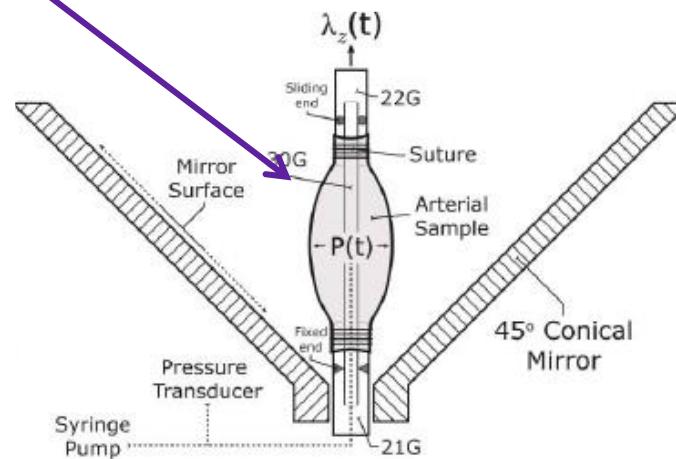
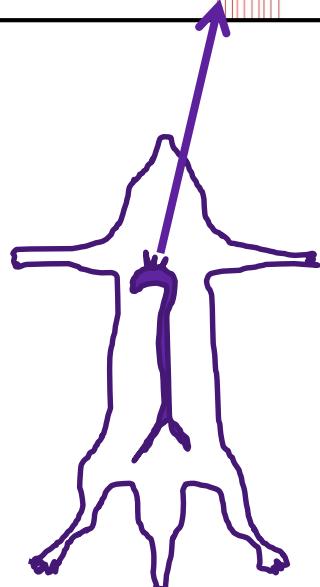
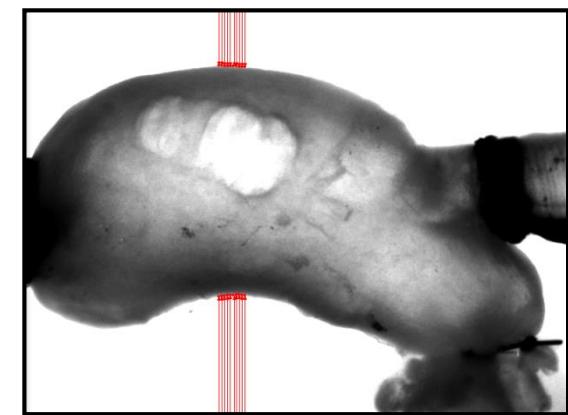
Control



Fibulin 4 SMC KO



Fibrillin 1  $mgR/mgR$



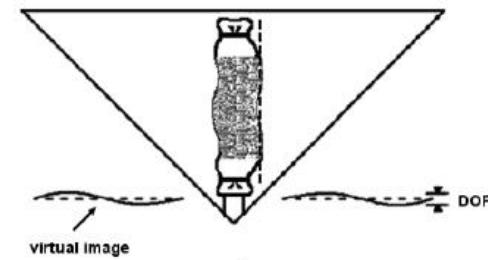
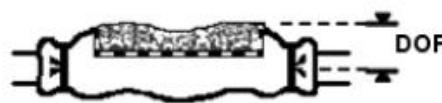
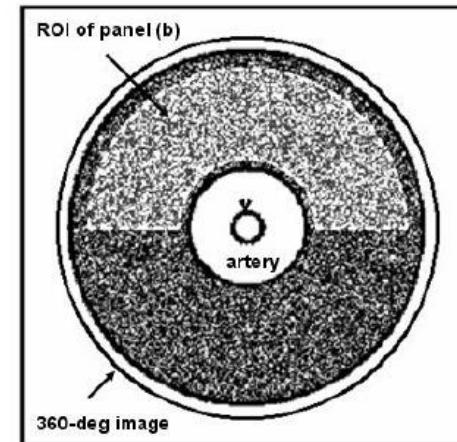
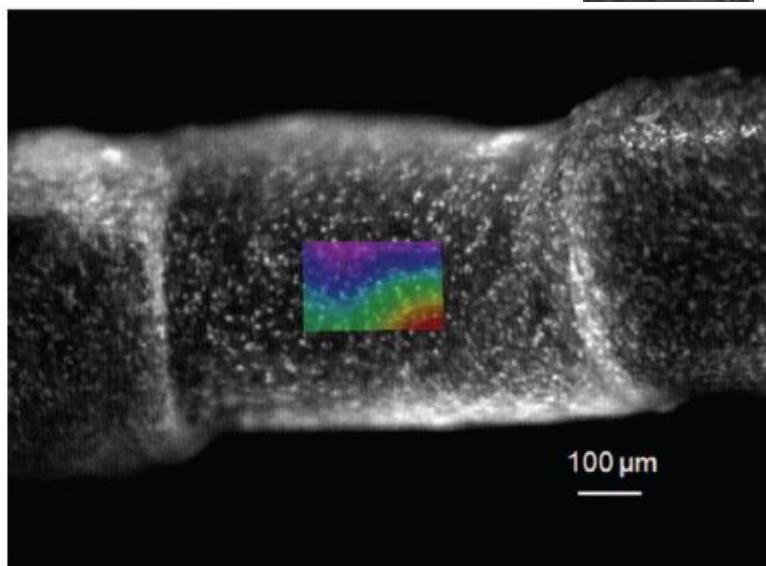
# MEASUREMENT OF THE RESPONSE USING DIGITAL IMAGE CORRELATION



classical



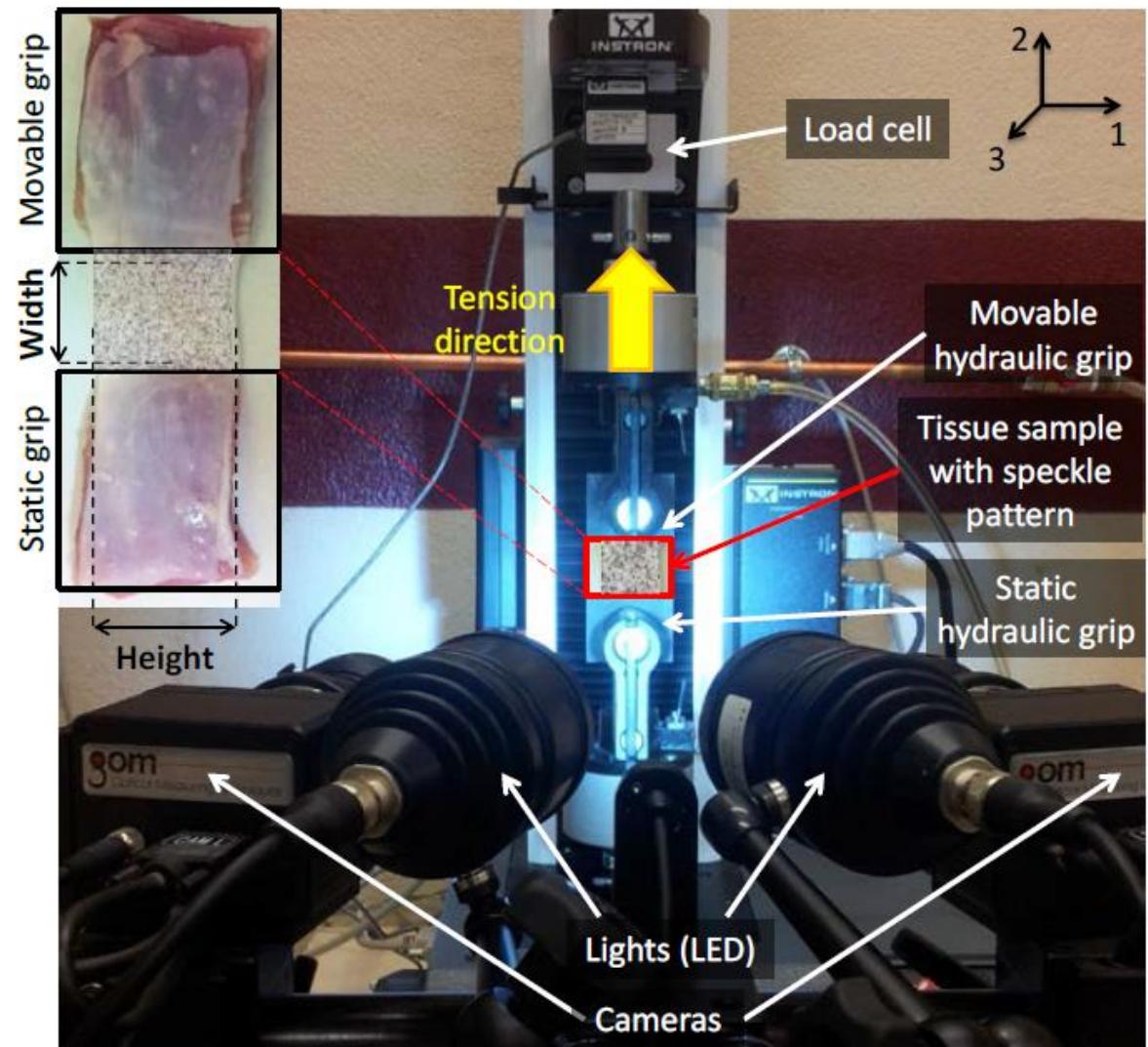
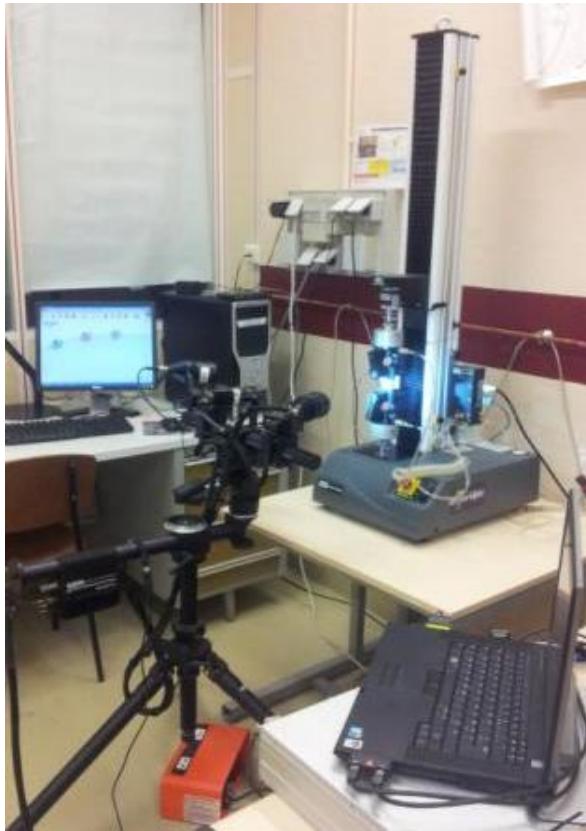
panoramic



Badel et al. CMBBE, **15**, p 37-48, 2012.

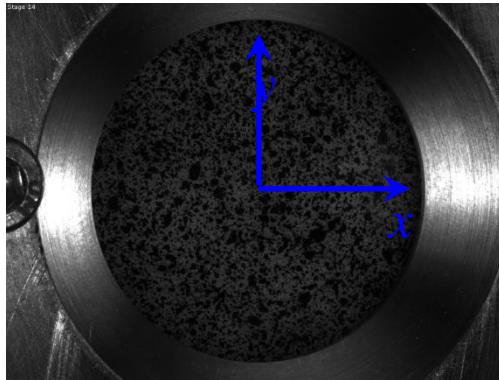
Genovese. Optics Lasers Eng, **47**, p 995-1008, 2009.

# DIC tend to be used for all kind of soft tissues

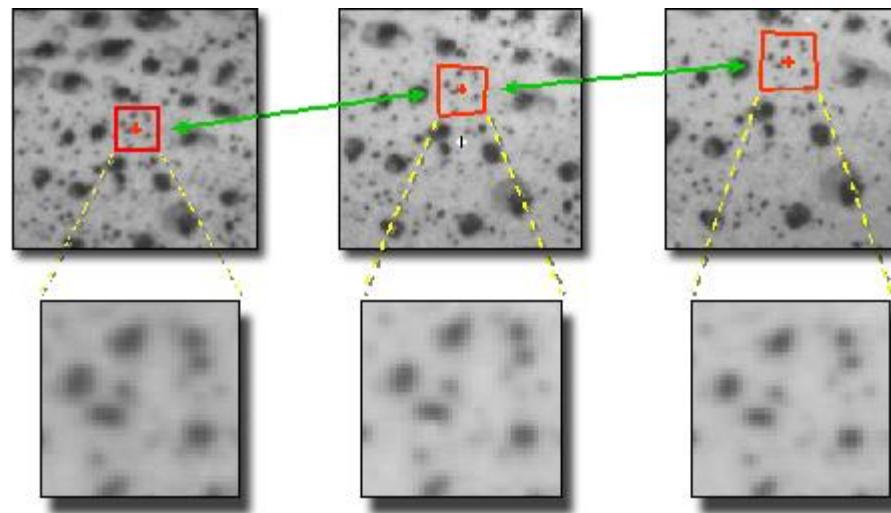
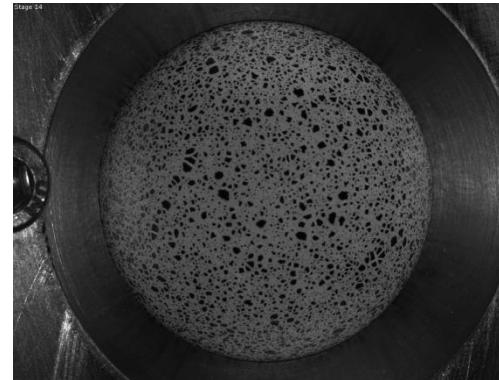


# Principle of DIC

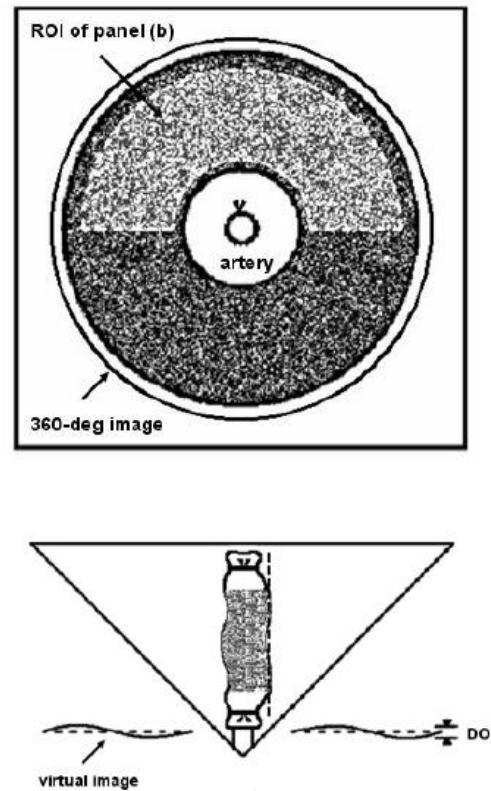
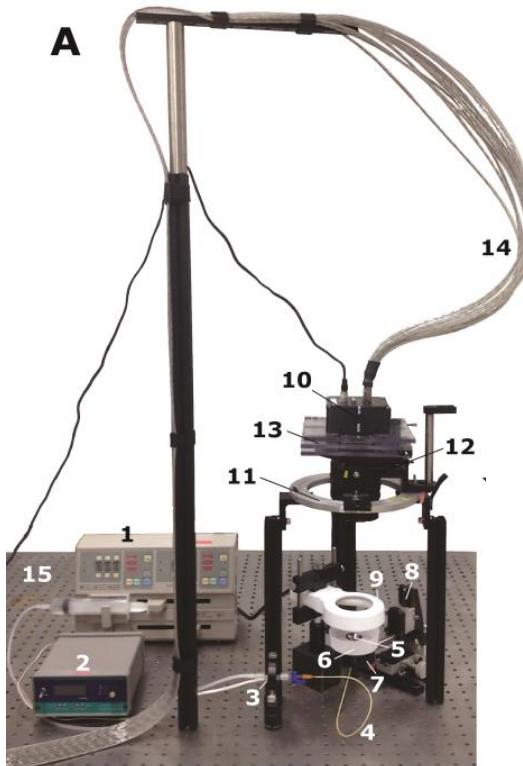
Undeformed



Deformed

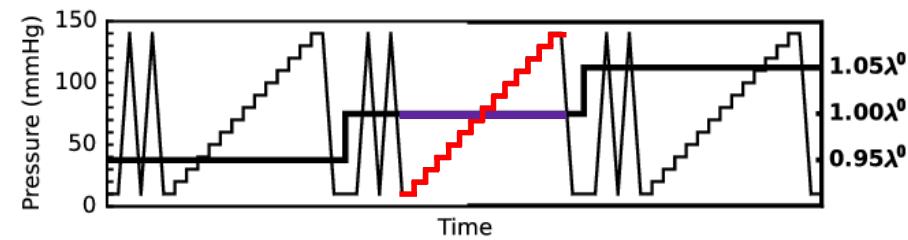
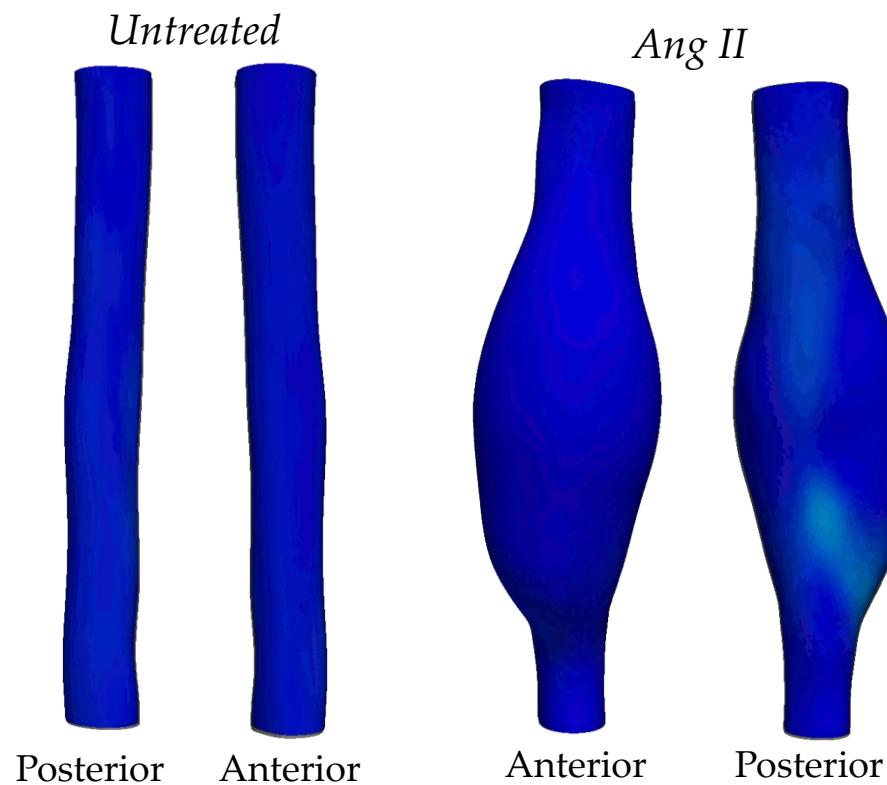


# The pDIC technique

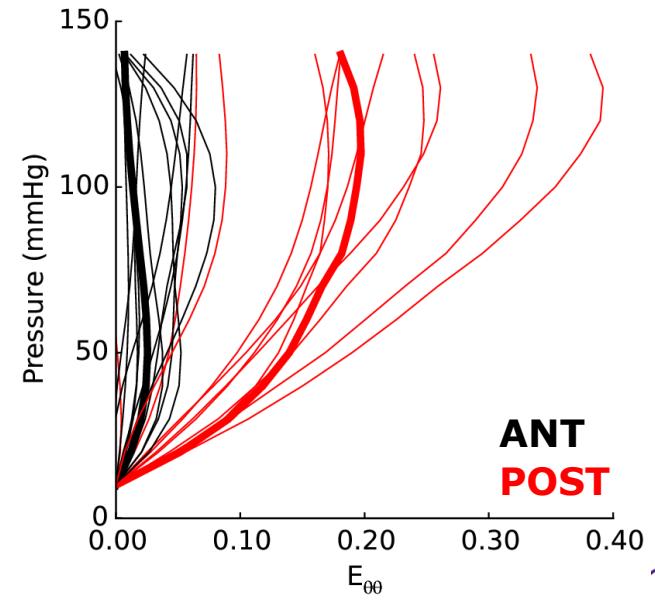


# Measurement of surface deformation fields using Panoramic Digital Image Correlation (pDIC)

## Suprarenal Abdominal Aorta (SAA)



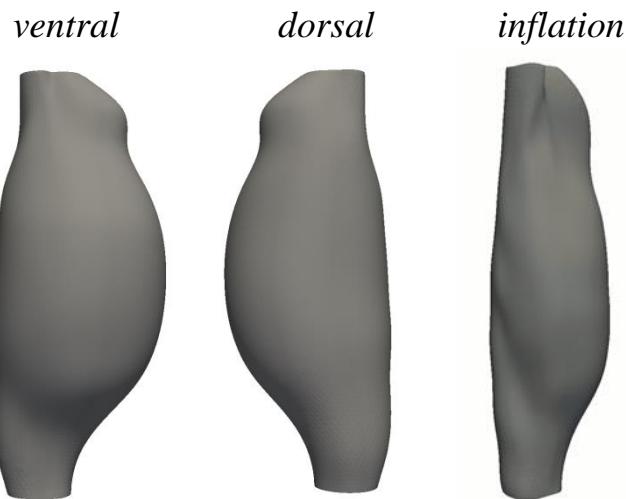
## Circumferential Green Strain



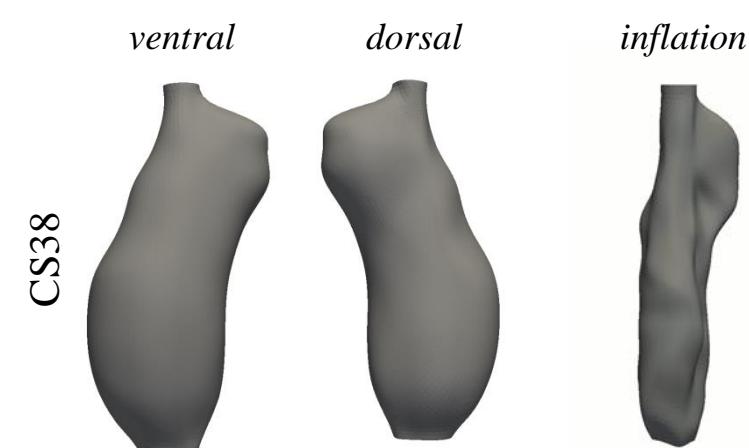
# pDIC measurements



Fibulin 4 SMC KO

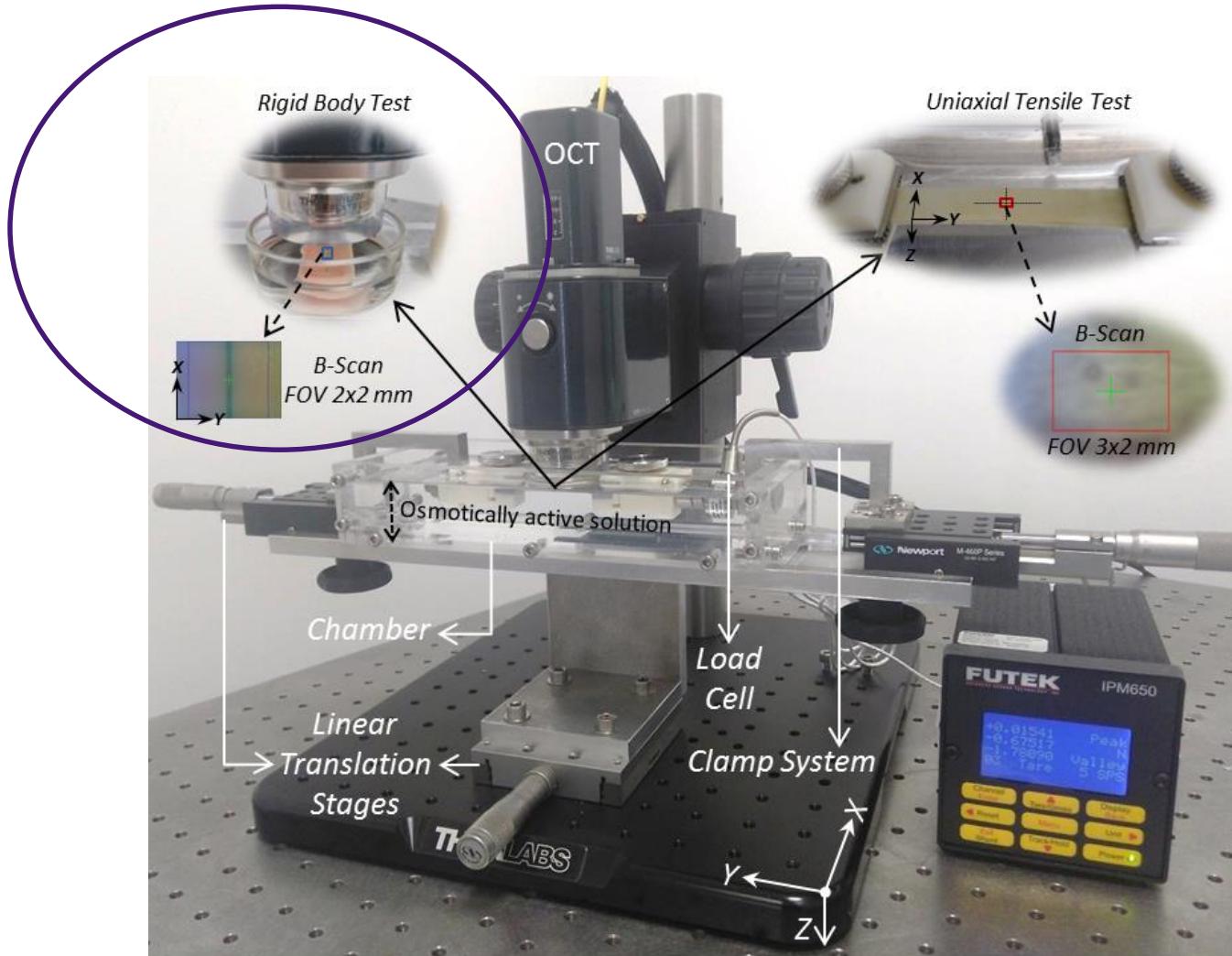


Fibrillin 1  $mgR/mgR$

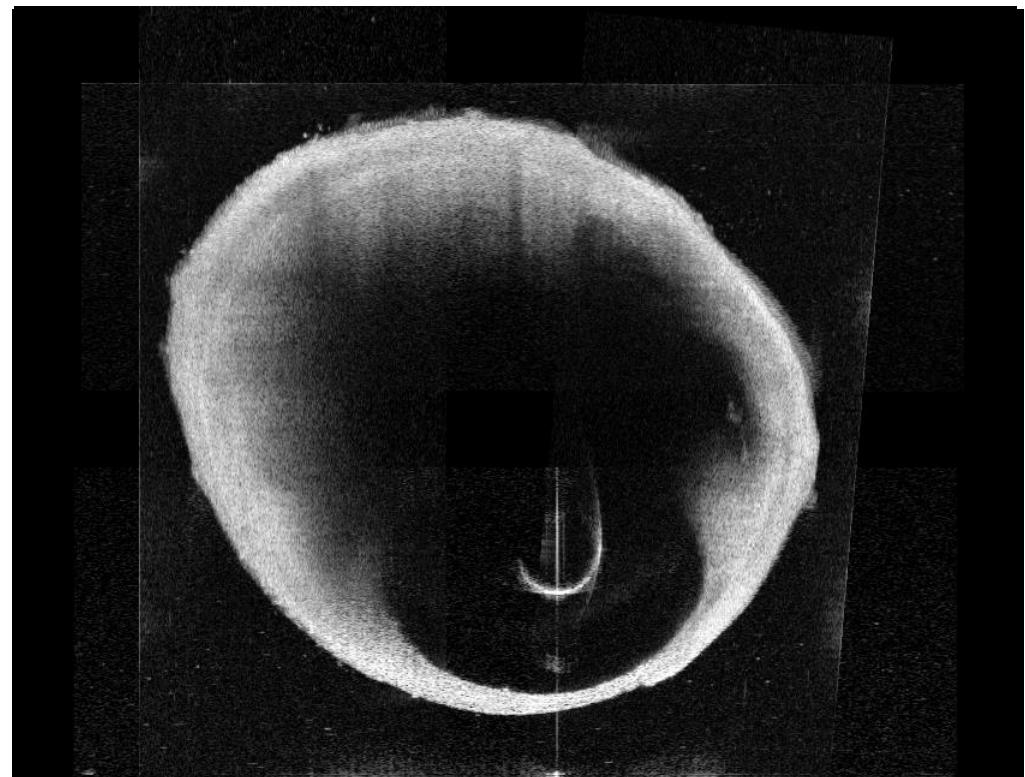
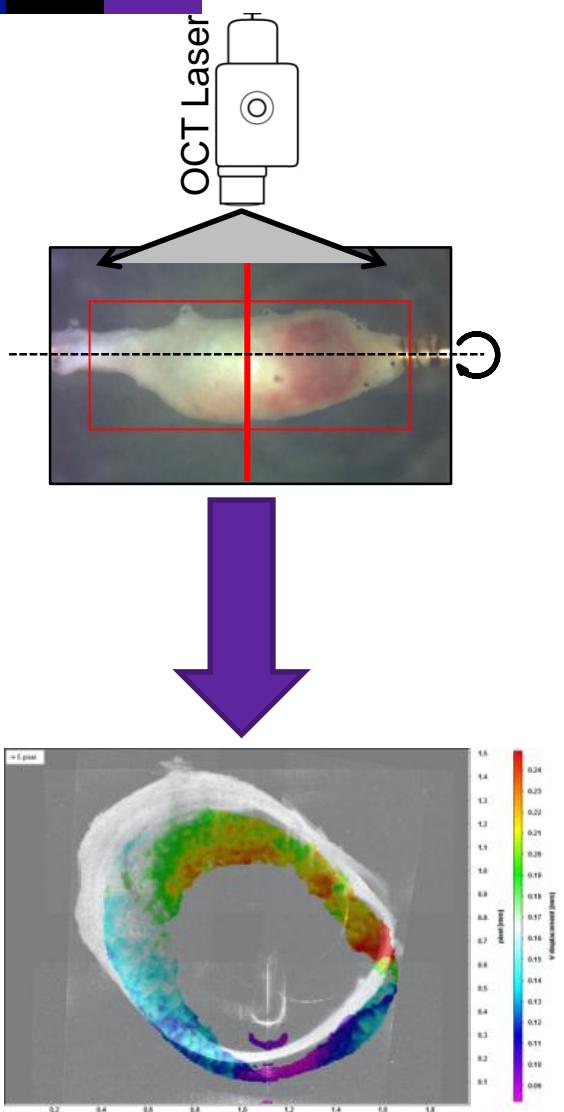




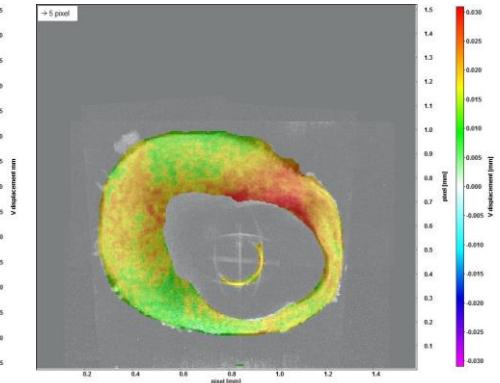
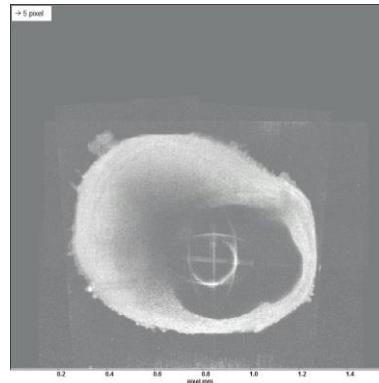
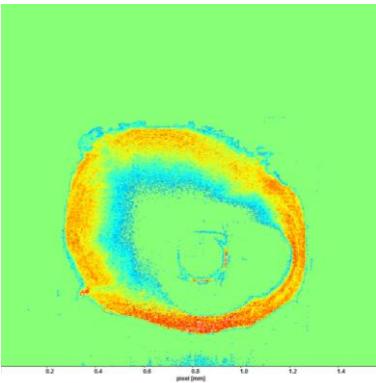
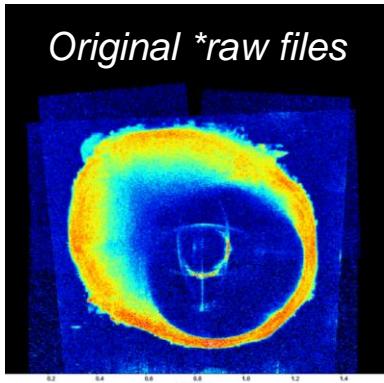
# OCT-DVC applied to arterial mechanics



# Measurement of bulk deformation fields by Digital Volume Correlation on OCT images



# Image Processing Methodology – Inflation Test



Title: REF

Width: 667 pixels

Height: 640 pixels

Depth: 100 pixels

Voxel size: 1x1x1 pixel<sup>3</sup> (2.38um)

} *Original  
Image Parameters*

Pressures: 20, 40, 60, 80, 100, 120, 140

Lambda ( $\lambda$ ) 1 – 2 – 3

- **Algorithmic Mask – Threshold: 48**
- **Correlation window size [voxel]: 24 (8x8x8)**
- **Overlap : 75%**
- **Passes : 10**
- **Required valid voxel per window: 44%**

Correlation window sizes (setup up to six steps):

Size [voxel]	Overlap	Peak search	Volume	Passes
Step 1 24	0 : 1:1	8 : radius [voxel]	8x8x8 : binning	2 : passes
Step 2 20	0 : 1:1	4 : radius [voxel]	4x4x4 : binning	2 : passes
Step 3 16	0 : 1:1	2 : radius [voxel]	2x2x2 : binning	2 : passes
Step 4 12	0 : 1:1	1 : radius [voxel]	no : binning	2 : passes
Step 5 10	0 : 1:1	1 : radius [voxel]	no : binning	2 : passes
Step 6 8	0 : 1:1	75 : radius [voxel]	no : binning	10 : passes

Intensity threshold for compression: 0 counts  
(only GPU; 0 counts => lossless)

Required valid voxel per window: 45 %

Algorithmic mask with operation pipeline:

local StdDev	over N pixel , N=	3
sliding maximum	filter length N pixel , N=	4
<b>below threshold</b>	set to 0, enter lower limit	48
erosion	erode mask N times, N=	95
above threshold	set to 0, enter upper limit	3
erosion	erode mask N times, N=	105
above threshold	set to 0, enter upper limit	1
eliminate 0 pixel	set to l=1 (recommended l)	