



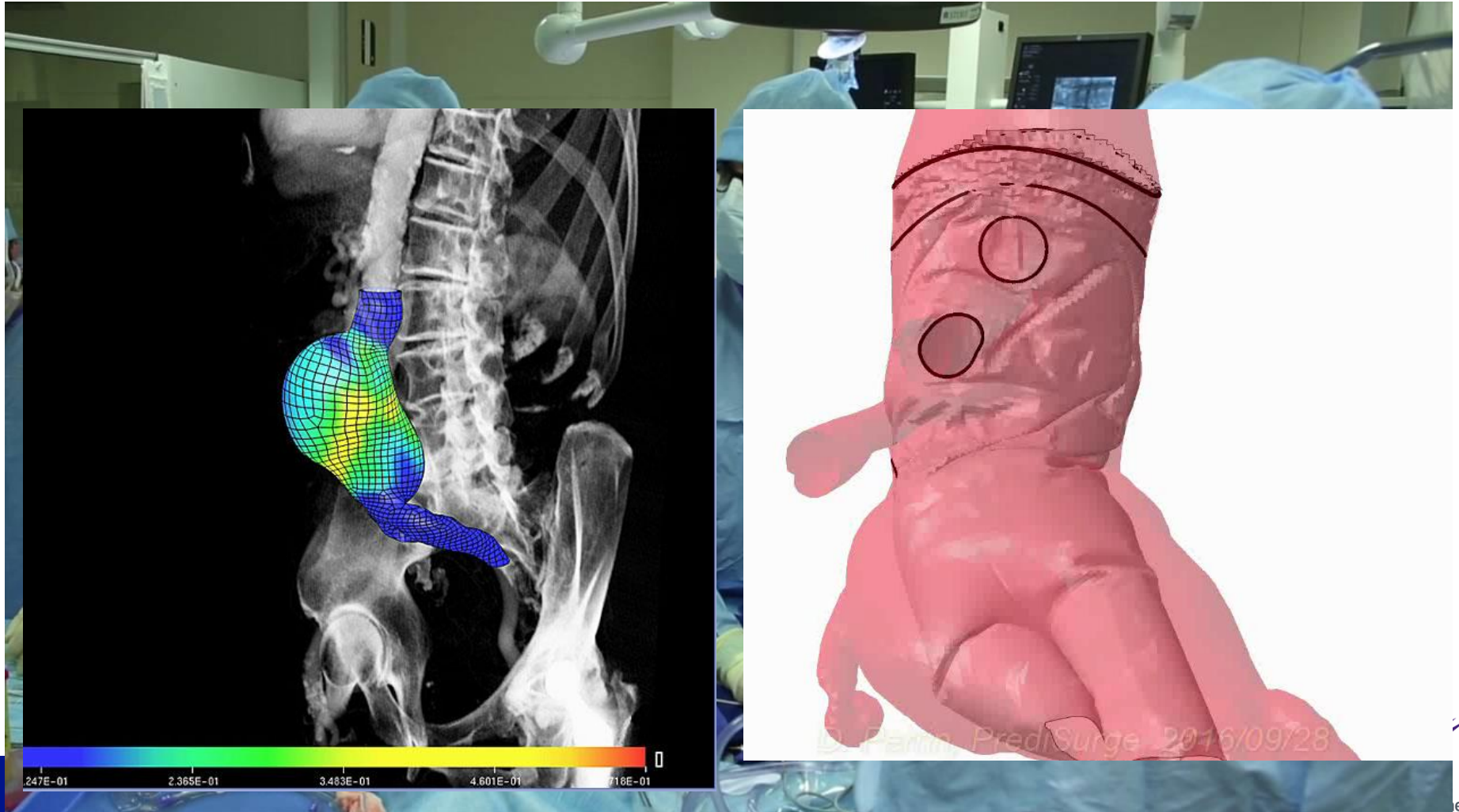
Mechanobiology of aortic aneurysms: novel approach using finite-element modeling and multimodality imaging



Prof. Stéphane AVRIL

Numerical simulation in the OR for vascular surgery?

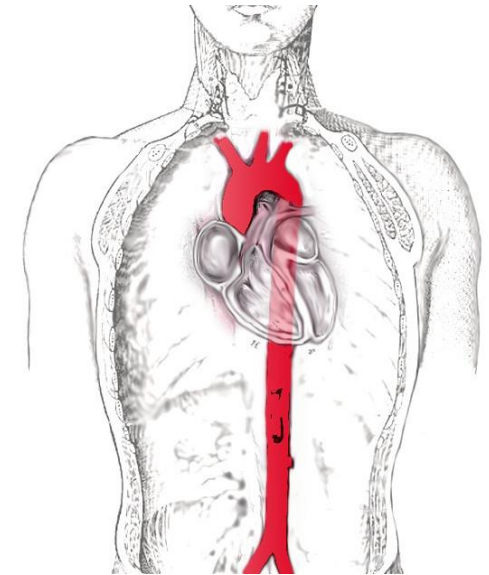
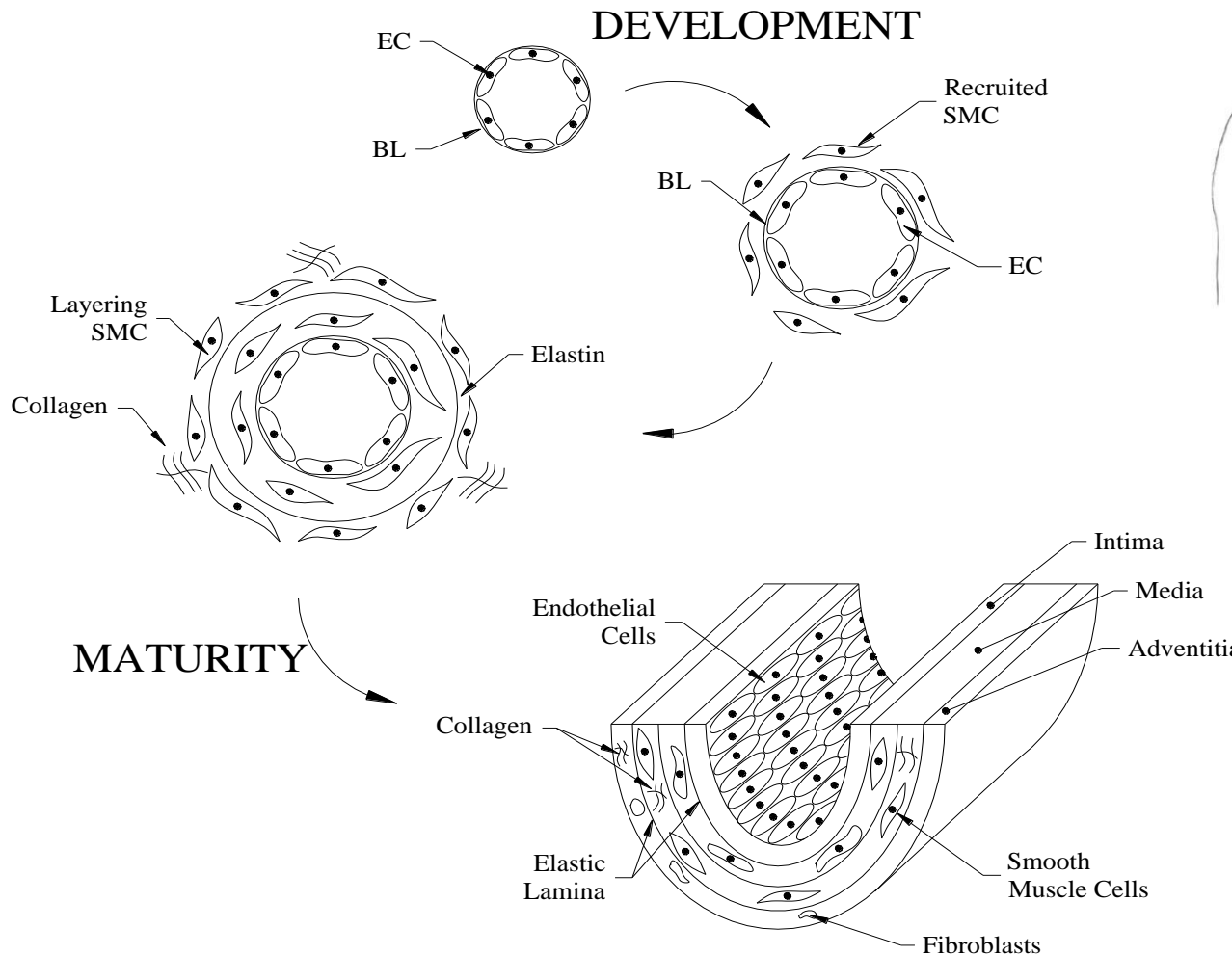
www.predisurge.com



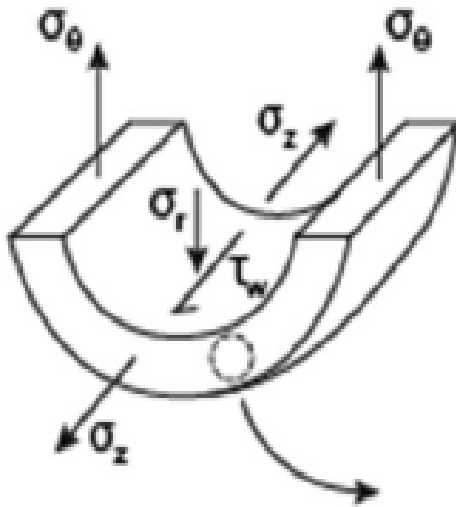


Basis of arterial biomechanics and mechanobiology

Schematic representation of aortic structure



Basics of aortic mechanics

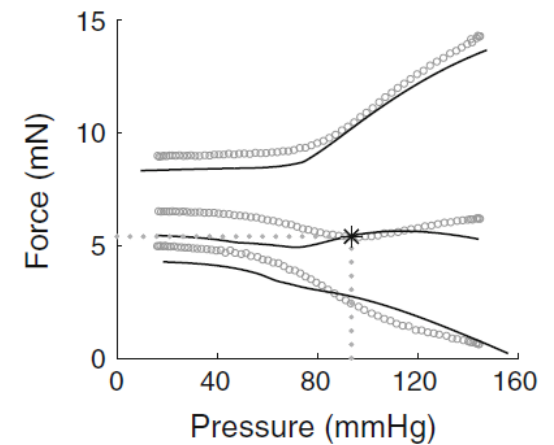
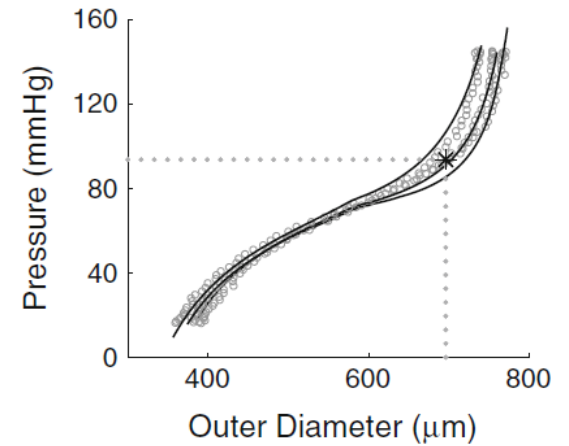
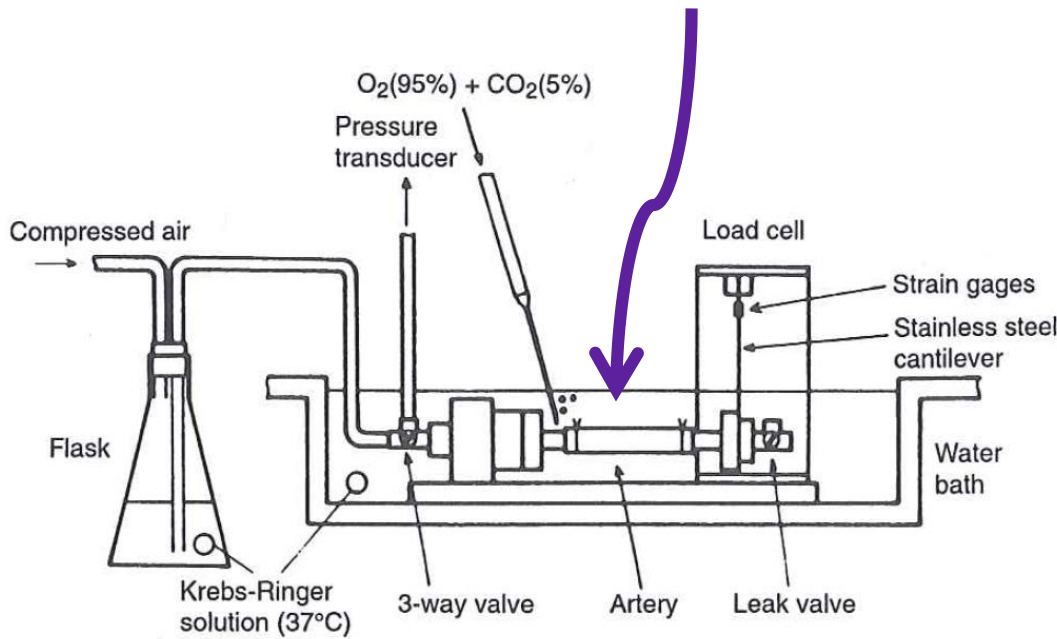


$$\tau_w = \frac{4\mu Q}{\pi a^3}, \quad \sigma_\theta = \frac{P a}{h}$$

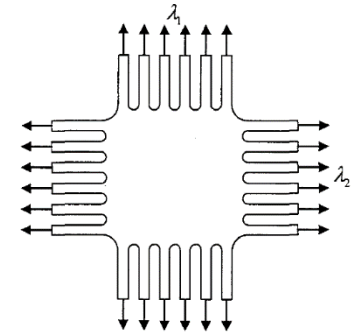
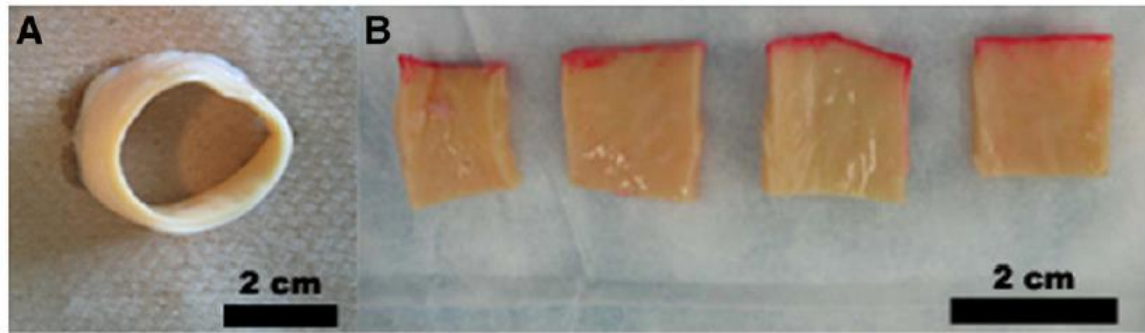
$$\sigma_z = \frac{f_z}{\pi (b^2 - a^2)} = \frac{f_z}{\pi h (2a - h)}$$

Humphrey JD (2002) *Cardiovascular Solid Mechanics: Cells, Tissues, and Organs*, Springer-Verlag, NY

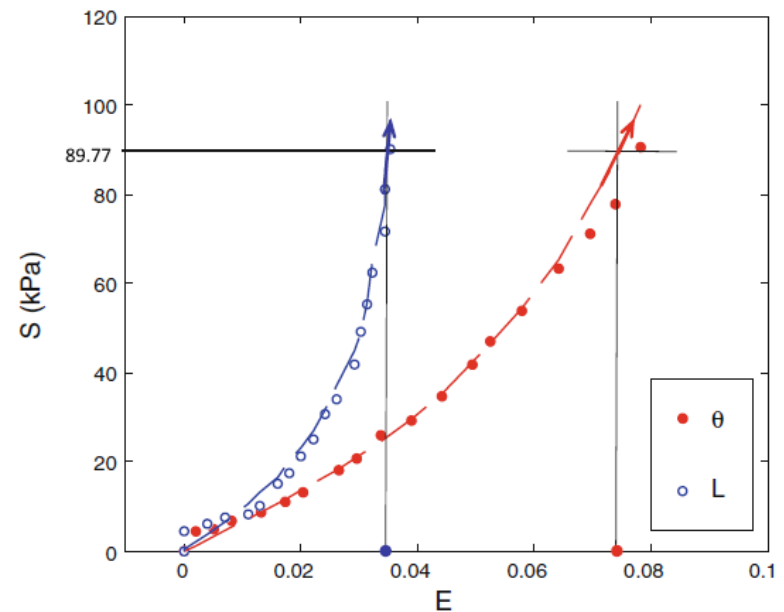
Functional biomechanical behavior

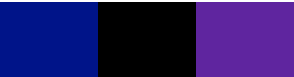


Material characterization and constitutive modeling



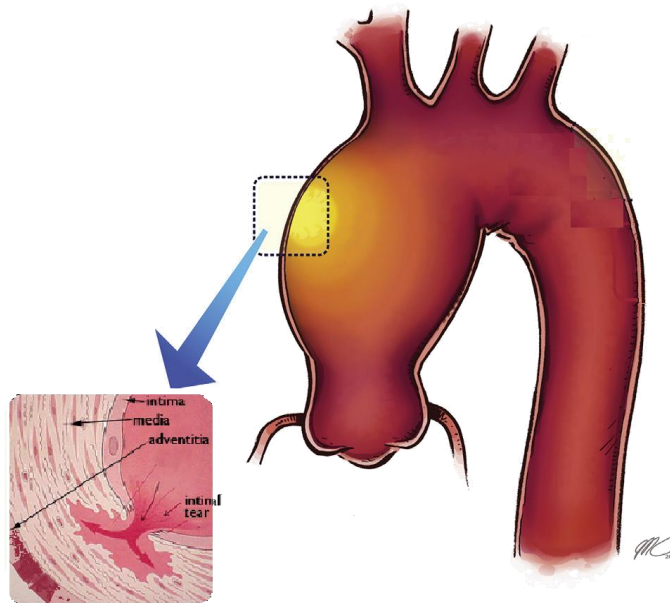
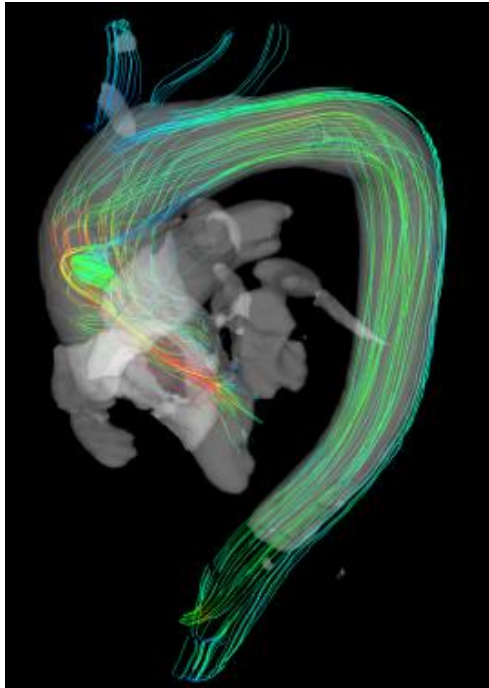
$$W = C_{10} (\bar{I}_1 - 3) + \frac{1}{D} \left(\frac{J^2 - 1}{2} - \ln J \right) + \frac{k_1}{2k_2} \sum_{\alpha=1}^N \left\{ \exp \left[k_2 \langle \bar{E}_\alpha \rangle^2 \right] - 1 \right\}$$





Prediction of aneurysm rupture using biomechanics and multimodal imaging

Prediction of risk of rupture and dissection



dissection

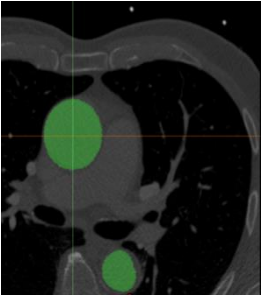


Context

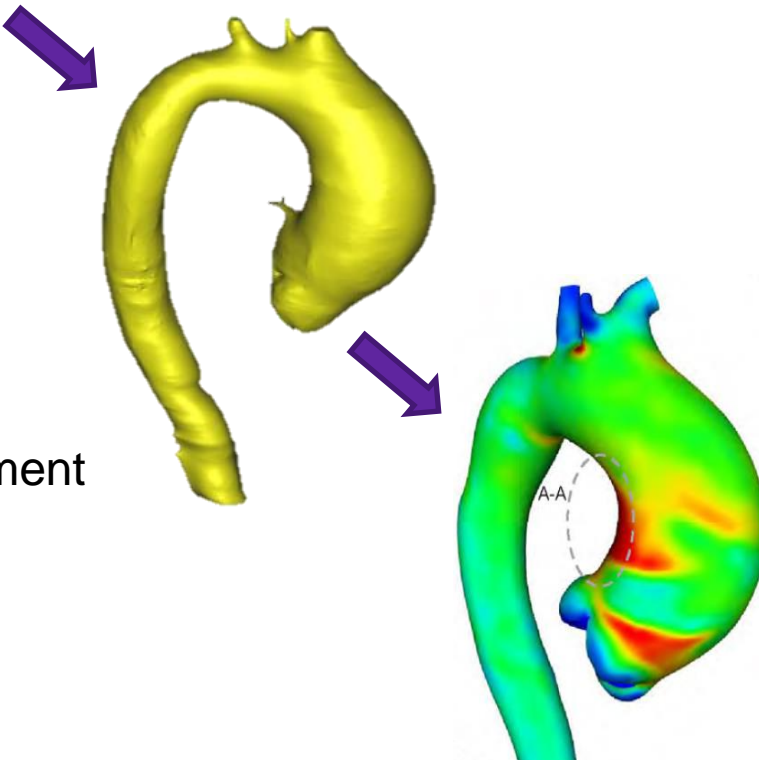
- **More and more aneurysms are detected at an early stage (incidence >8% for males >65 years old).**
- **An intervention is recommended if the aneurysm grows more >1cm/year or it is >5.5cm. This represents >90000 interventions per year in Europe and USA**
- **BUT:**
 - 25% aneurysms <5.5cm rupture : 15000 deaths**!
 - 60% of aneurysms >5.5 cm never experience rupture!
- **In summary: very high rate of inappropriate decisions and misprogramed surgical interventions!!**

** Pape et al, *Aortic Diameter ≥ 5.5 cm Is Not a Good Predictor of Type A Aortic Dissection Observations From the International Registry of Acute Aortic Dissection (IRAD)*, Circulation, 2007

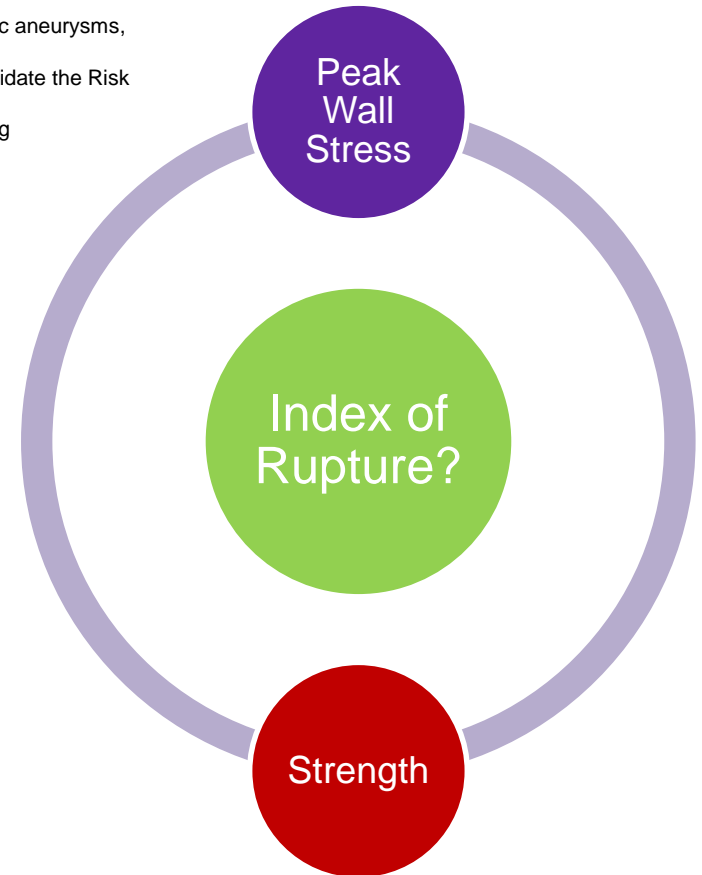
Challenges raised by rupture prediction



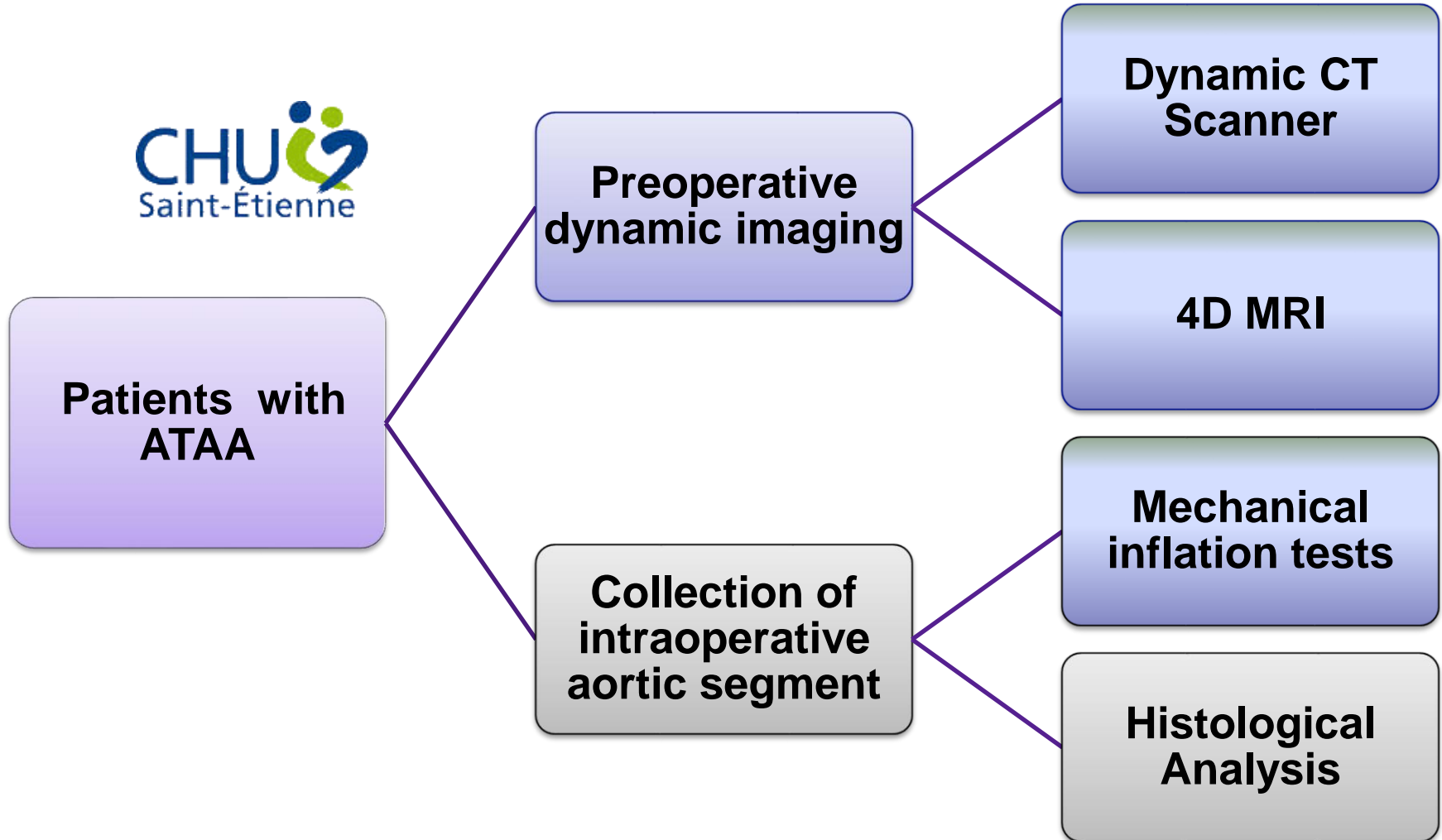
- O. Trabelsi, et al, Patient specific stress and rupture analysis of ascending thoracic aneurysms, J. Biomech. (2015).
- G. Martufi, et al, Is There a Role for Biomechanical Engineering in Helping to Elucidate the Risk Profile of the Thoracic Aorta?, Ann. Thorac. Surg. 101 (2016) 390–398.
- S. Pasta et al., Constitutive modeling of ascending thoracic aortic aneurysms using microstructural parameters, Med. Eng. Phys. 38 (2016) 121–130.



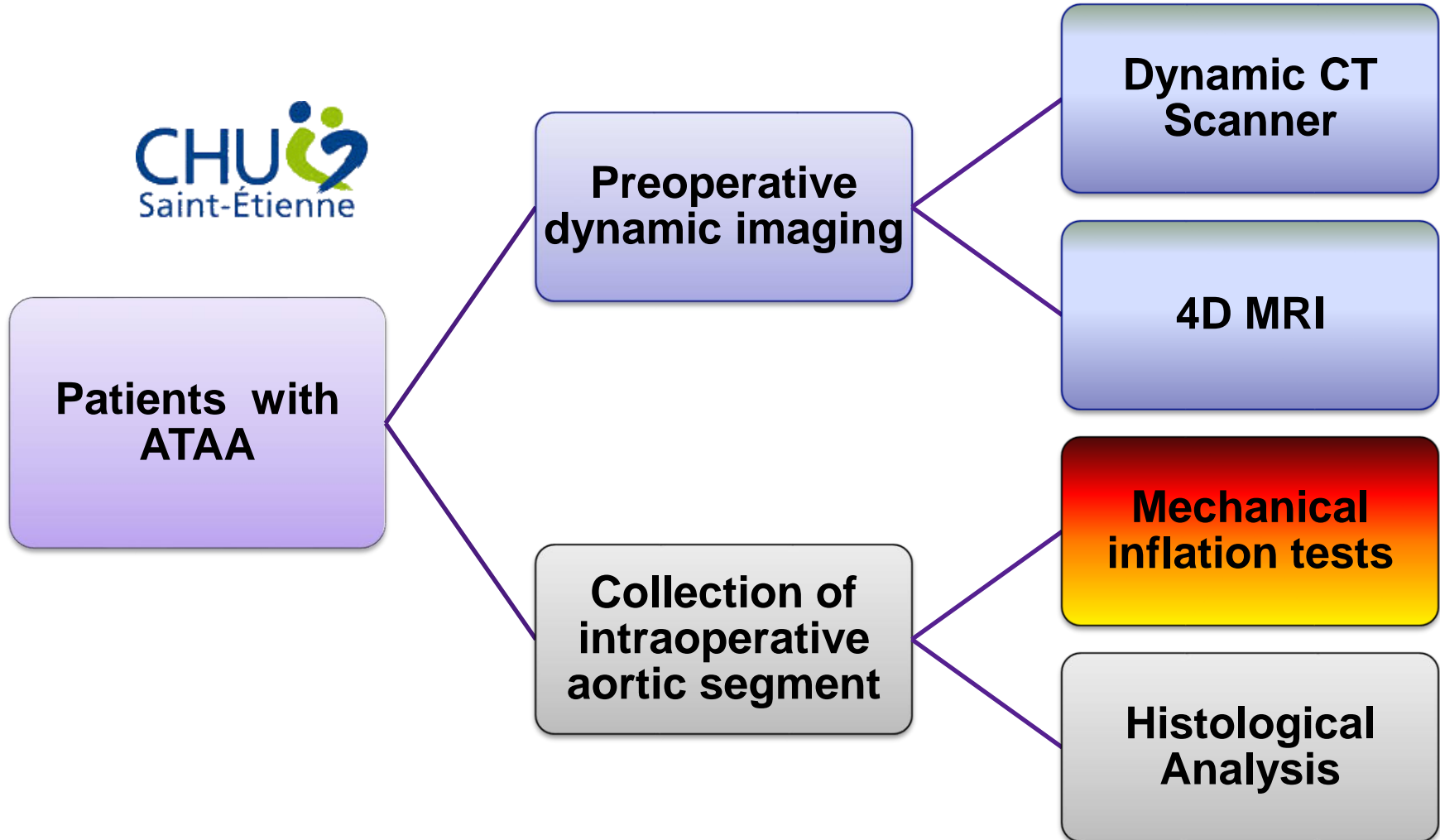
Finite-element modeling



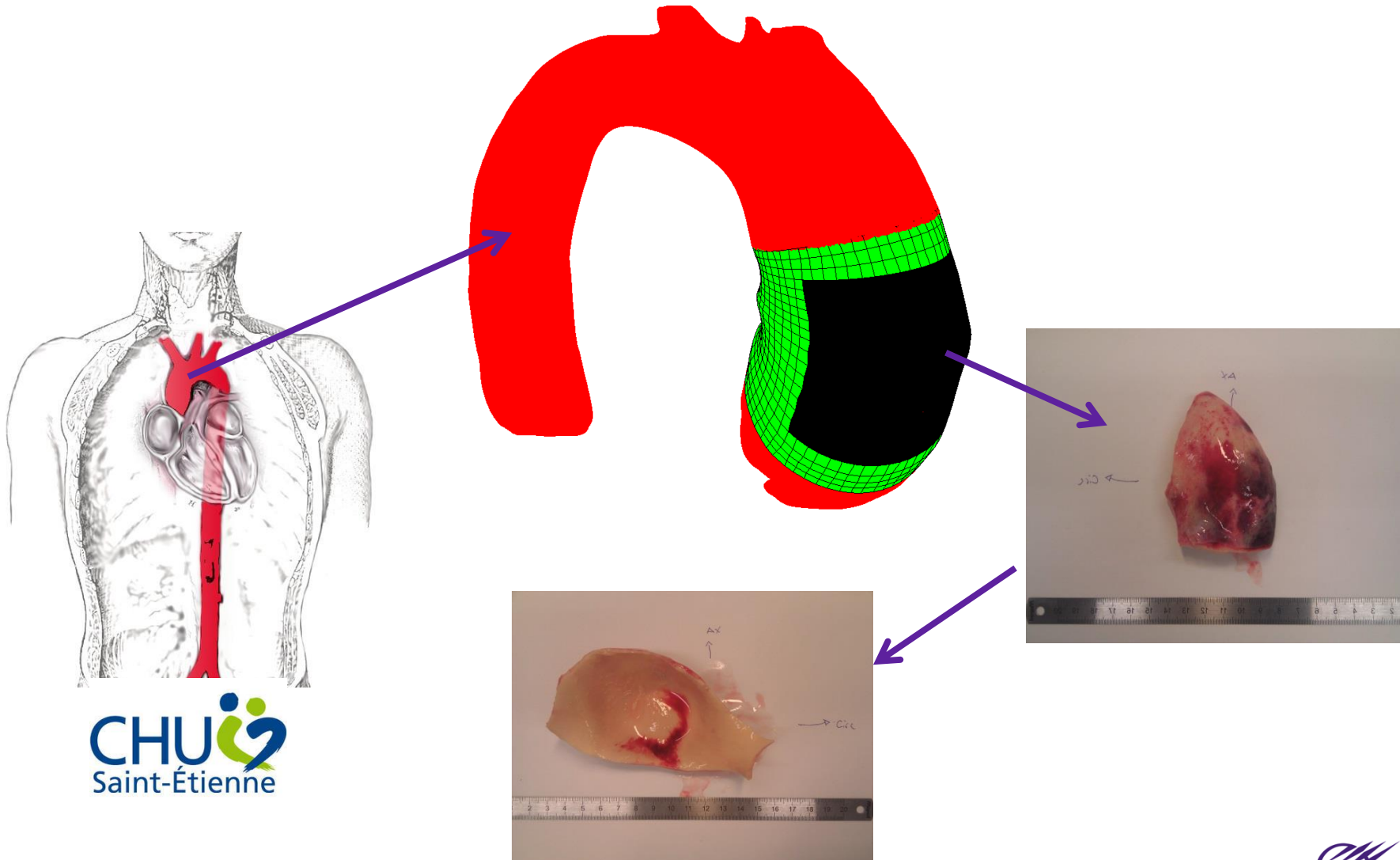
Methodology



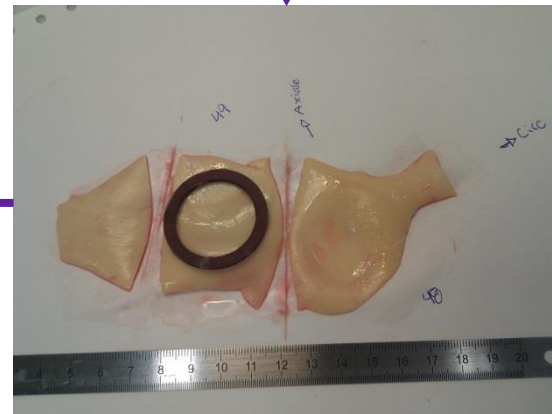
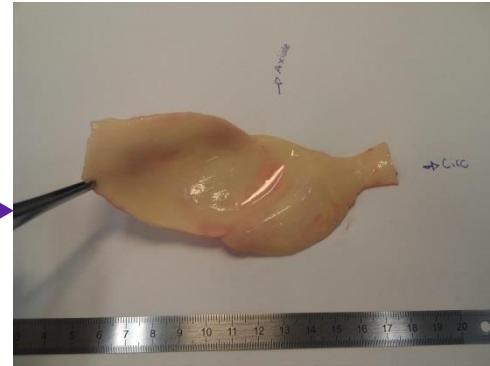
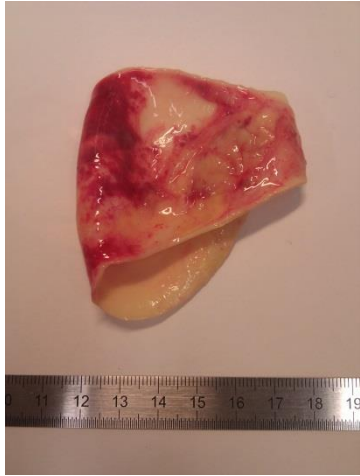
Methodology



Collection of the samples

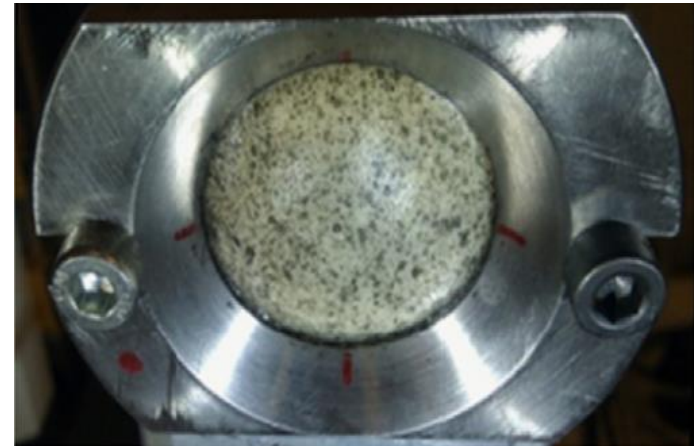
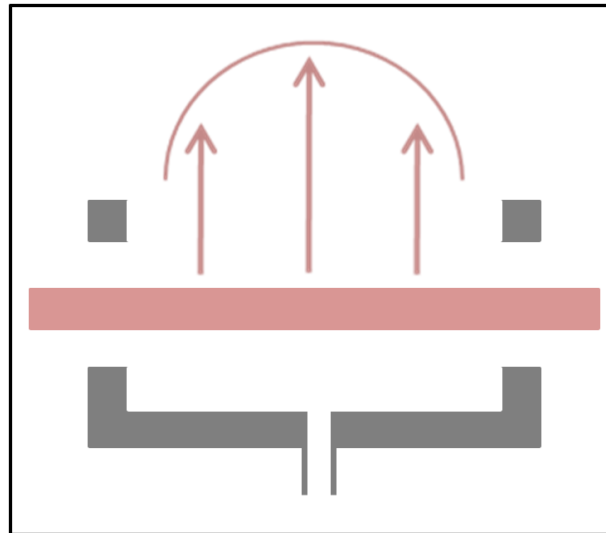


Preparation

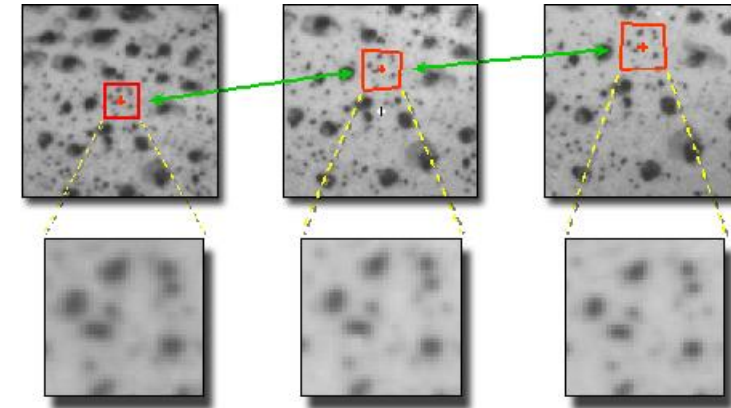


Bulge inflation test

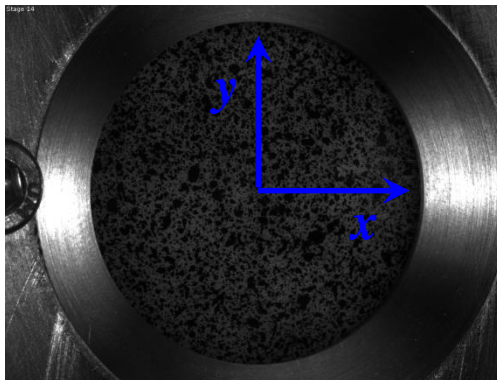
Romo et al. Journal of Biomechanics -2014.



Full-field measurements using sDIC



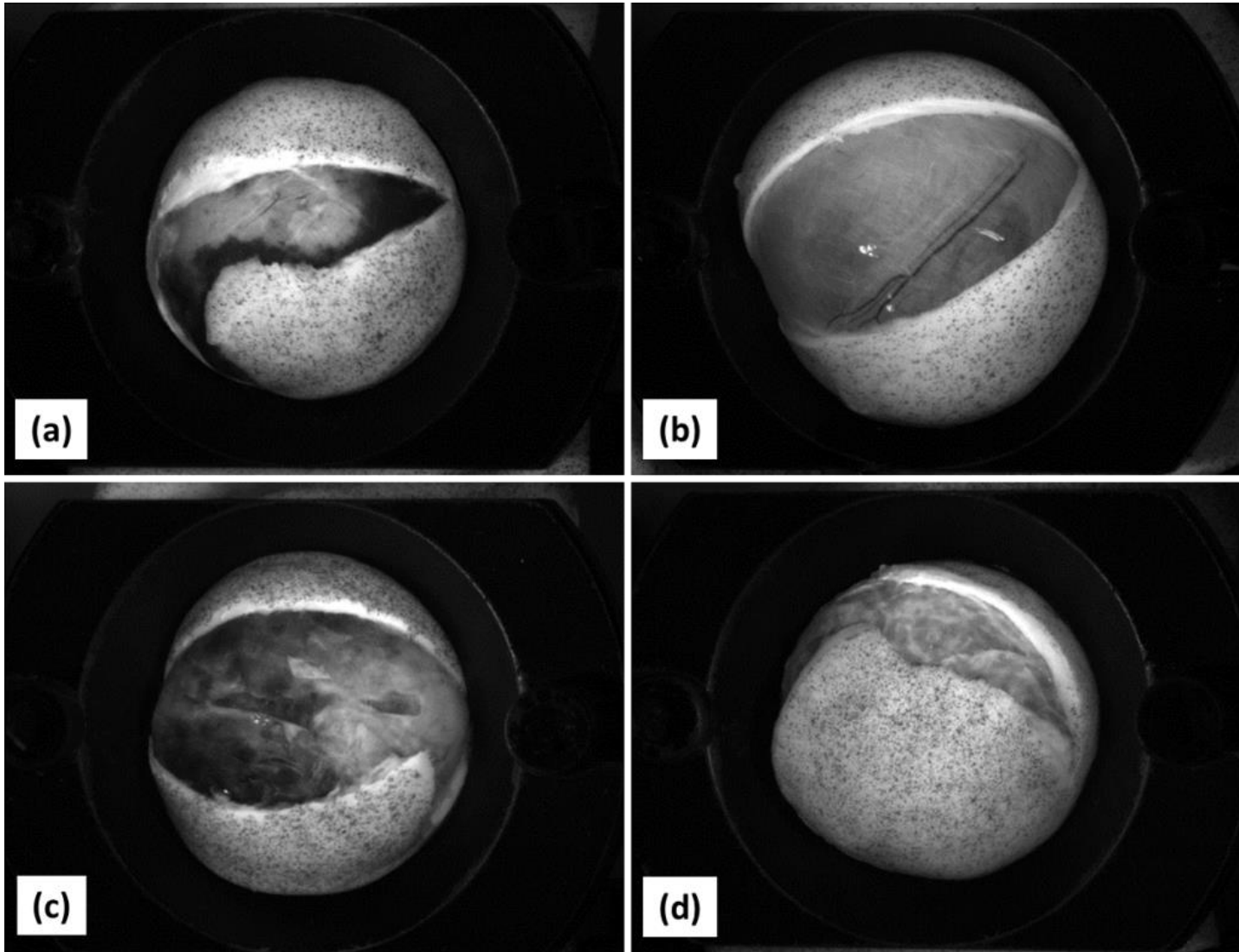
Undeformed



Deformed

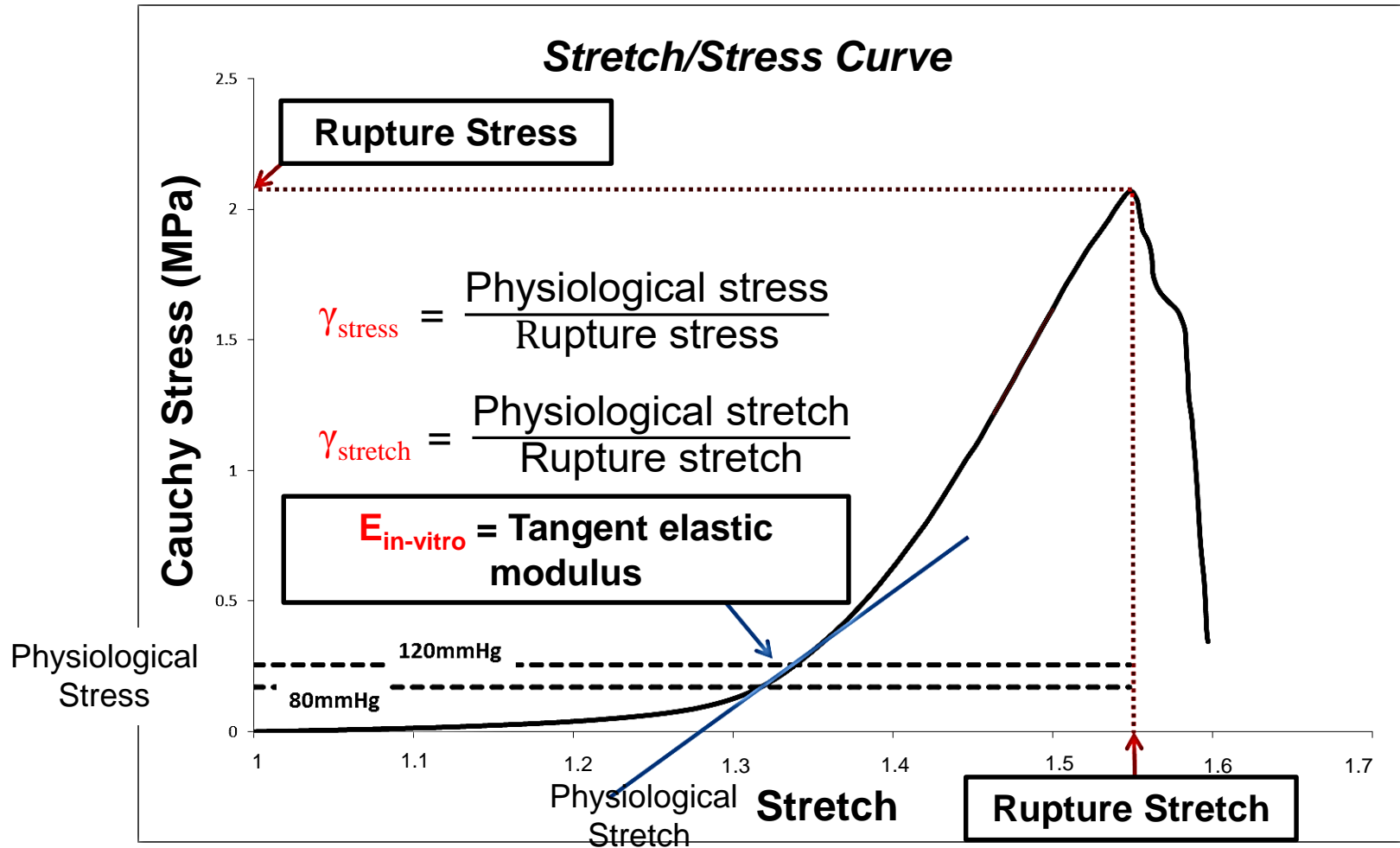


Rupture profiles

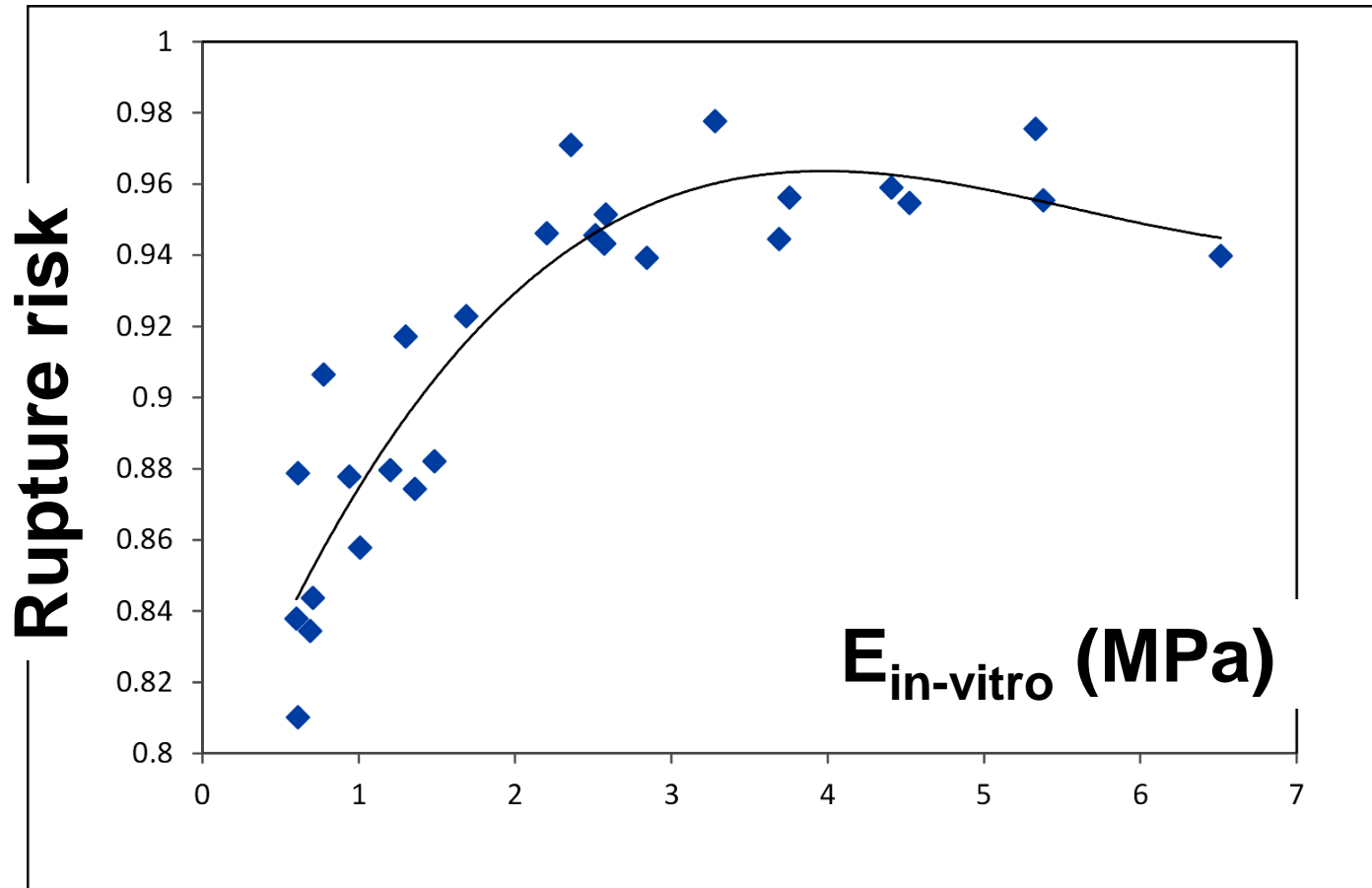


50% of aortas ruptured with an angle θ equal to 90°

Rupture risk estimation

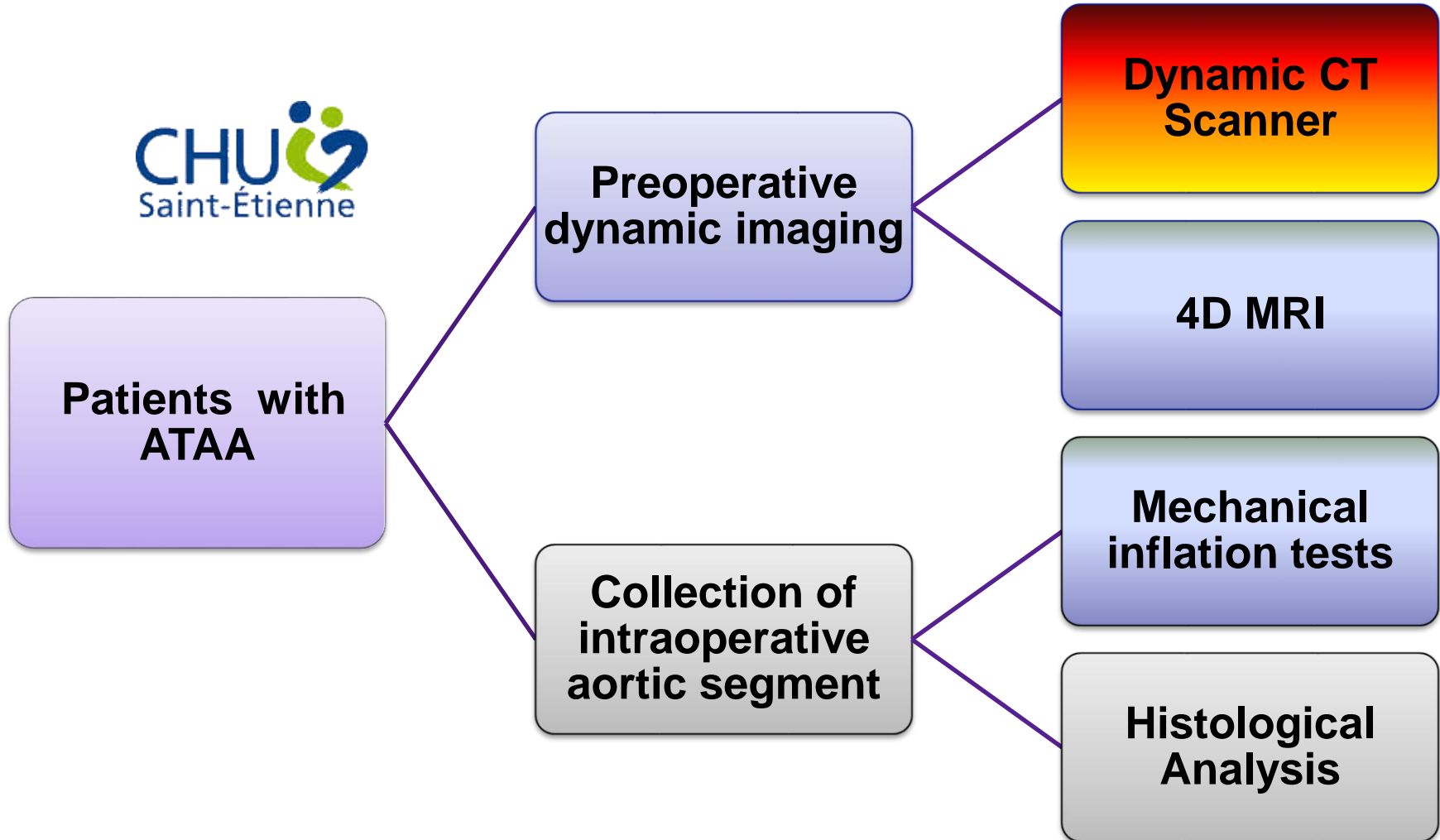


Correlation between the stretch-based rupture risk and the tangent elastic modulus



Duprey A, et al. Biaxial rupture properties of ascending thoracic aortic aneurysms. *Acta Biomaterialia* 2016.

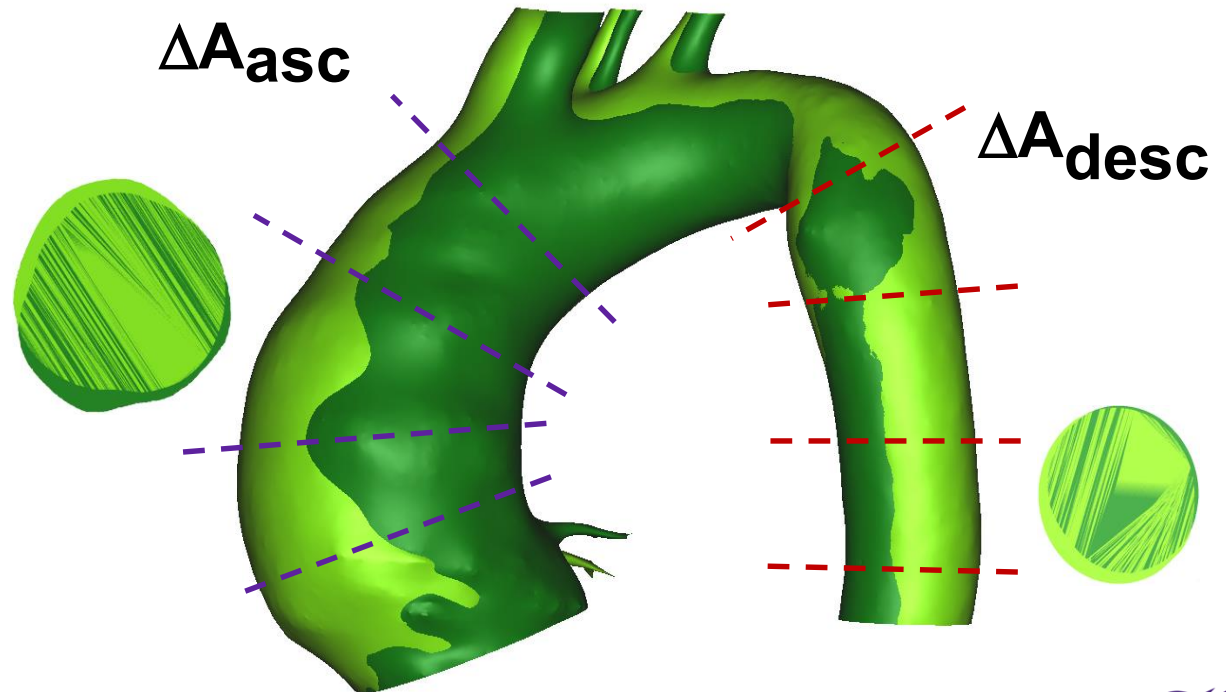
Methodology



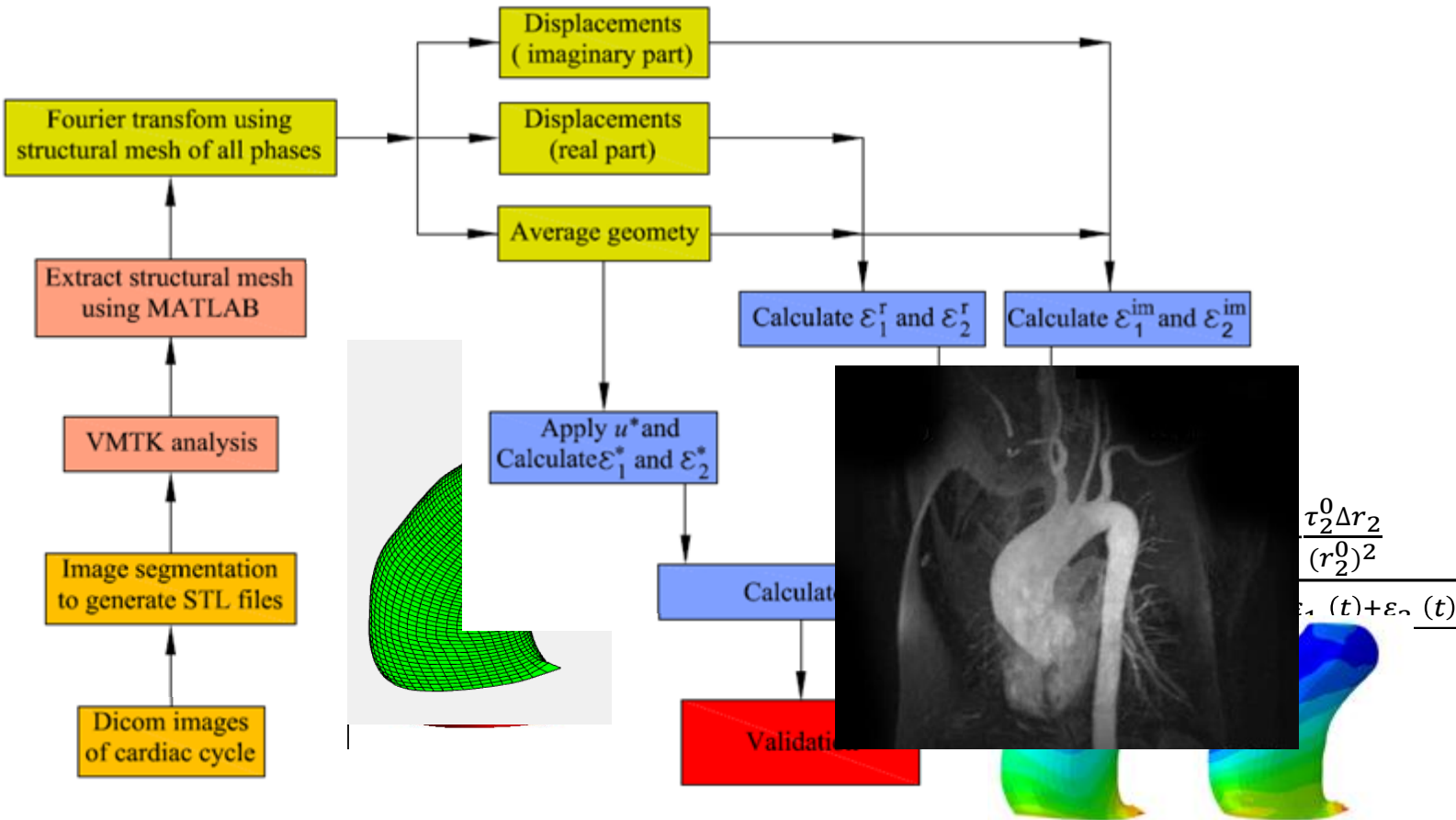
Measurement of aortic DISTENSIBILITY

■ *Aortic wall - 3D reconstruction from gated CT*

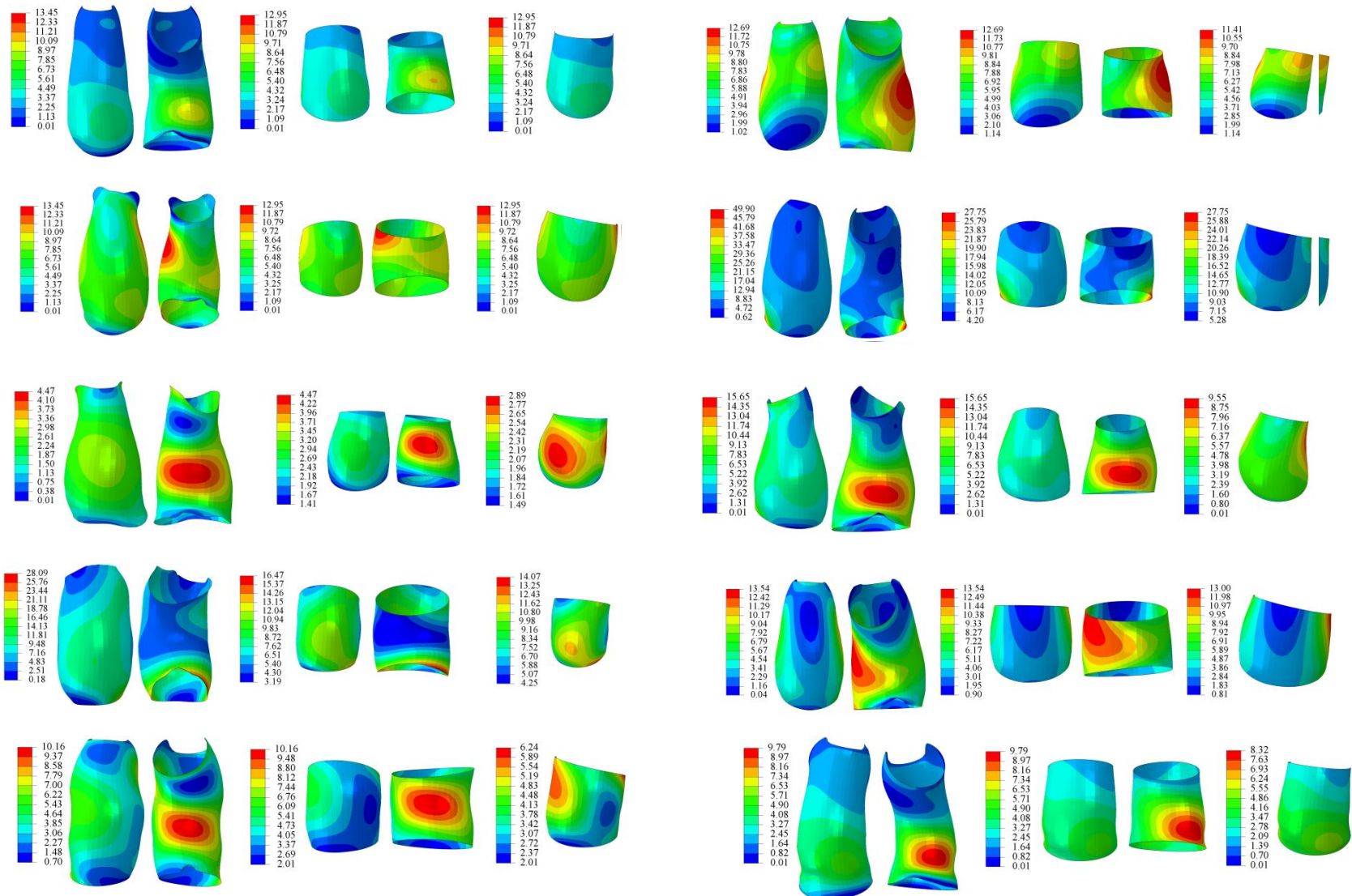
Dynamic preoperative scanners during cardiac cycle (~ 0.92 s) = 10 phases.
CT: (resolution 512x512, slice thickness of 0.5 mm)



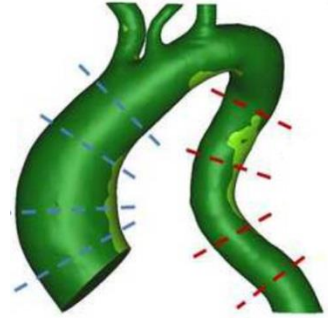
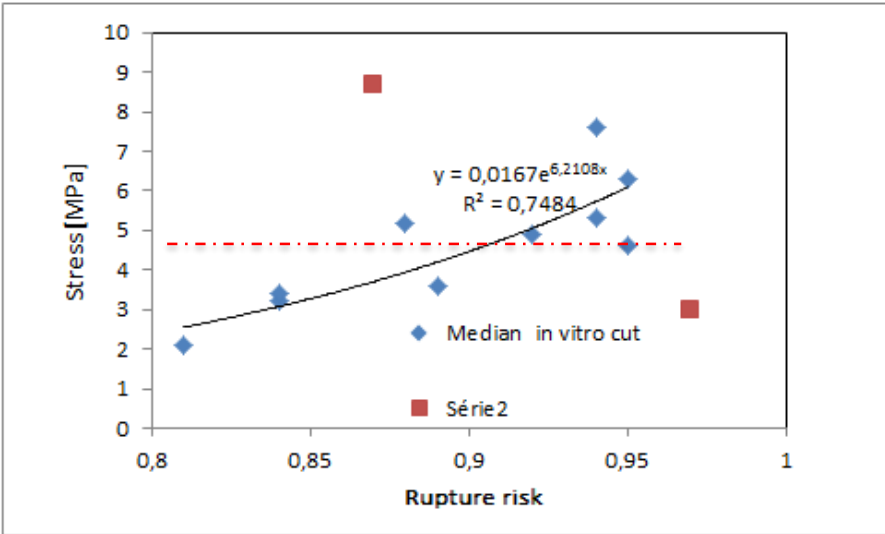
Methodology for non invasive reconstruction of in vivo stiffness distribution



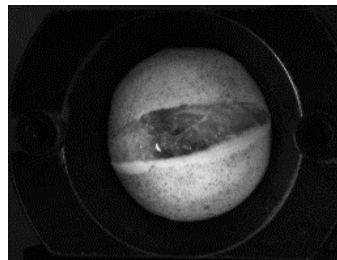
Stiffness distributions for 10 patients



Correlation between stretch and membrane stiffness

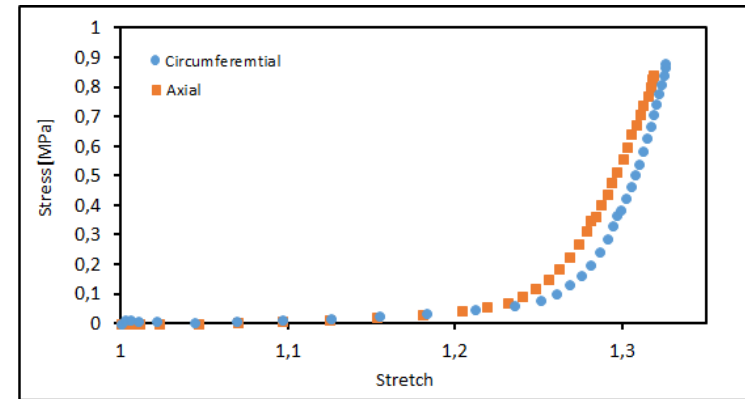
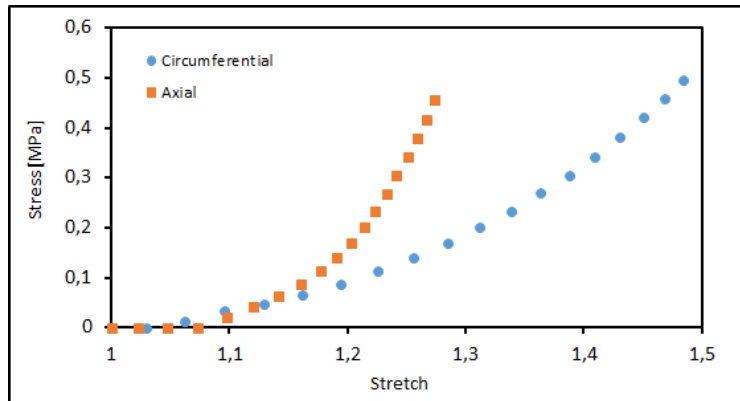
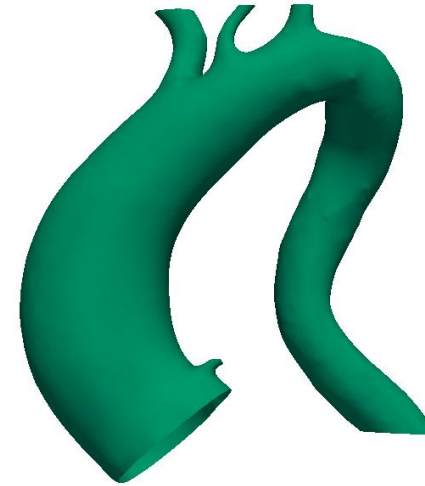


In vivo



In vitro

Two examples of soft and stiff ascending aorta



Summary

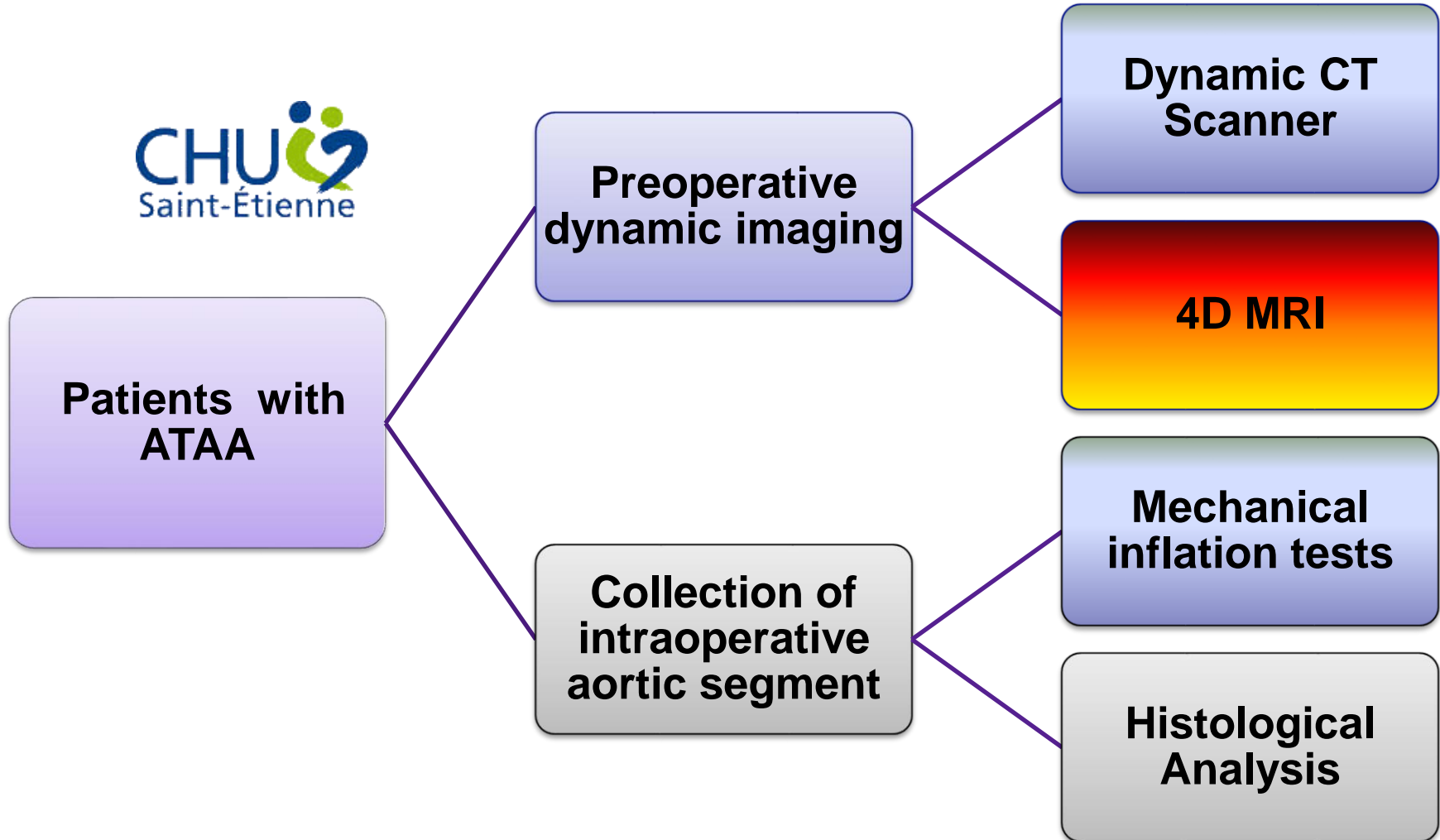
- 2 ways of defining rupture:
 - PWS – but unknown patient-specific strength
 - γ_{stretch} correlated with in vivo circumferential stiffness

Higher distensibility \Rightarrow less risk because the aneurysm can more easily withstand volume variation

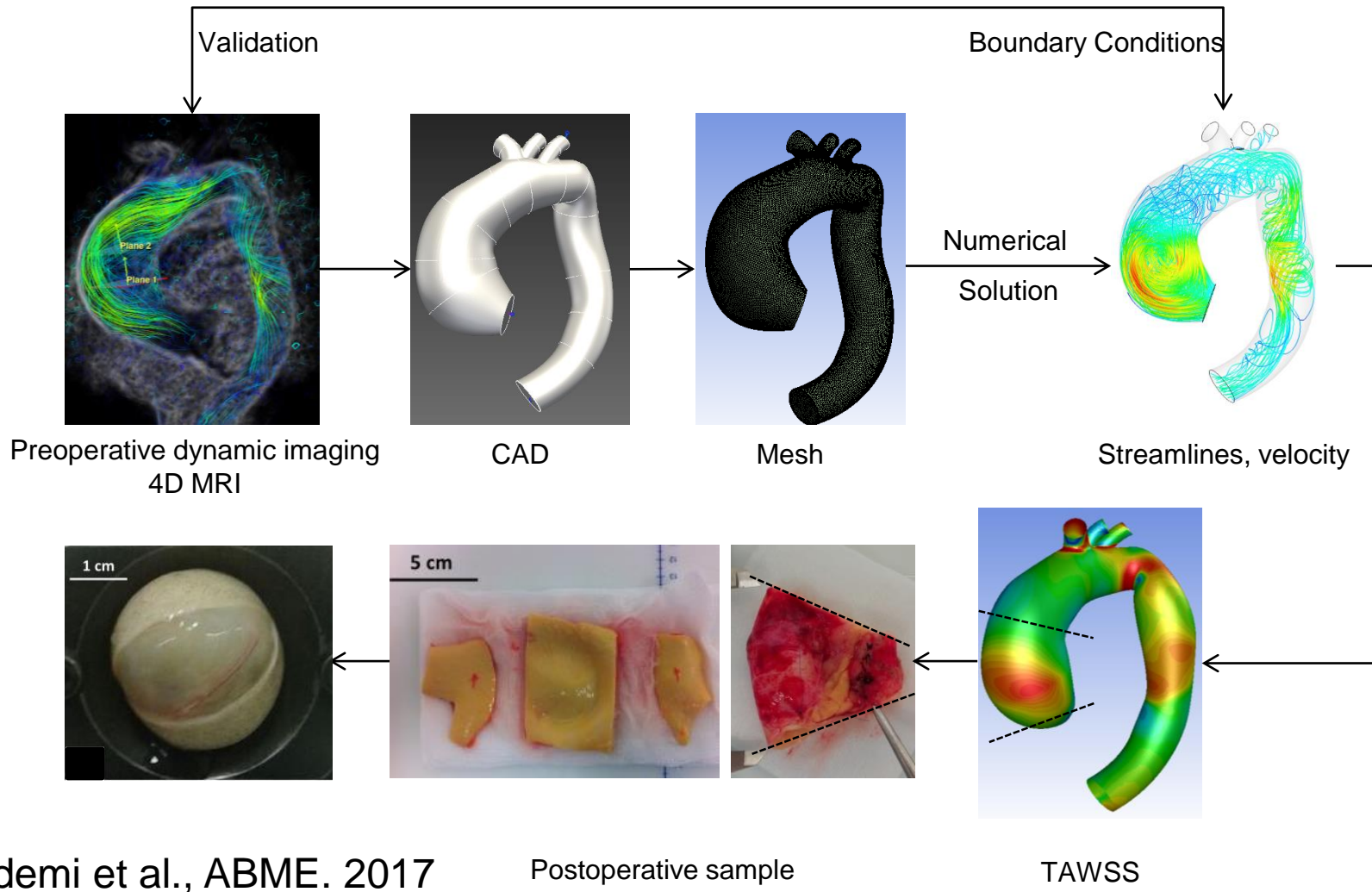


Martin et al., Acta Biomater. 2013, Duprey et al., Acta Biomater. 2016.

Methodology



Role of hemodynamics in rupture risk

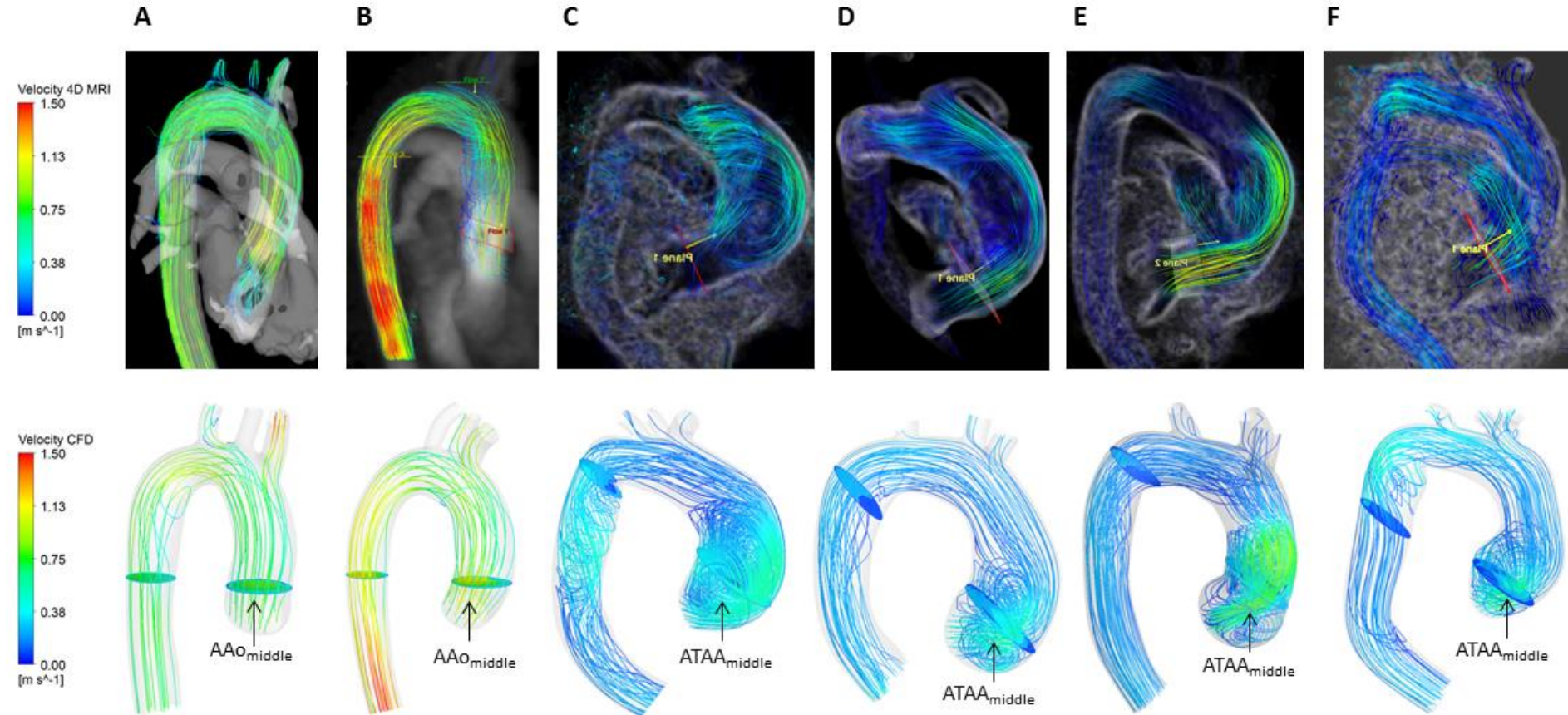


Condemi et al., ABME. 2017

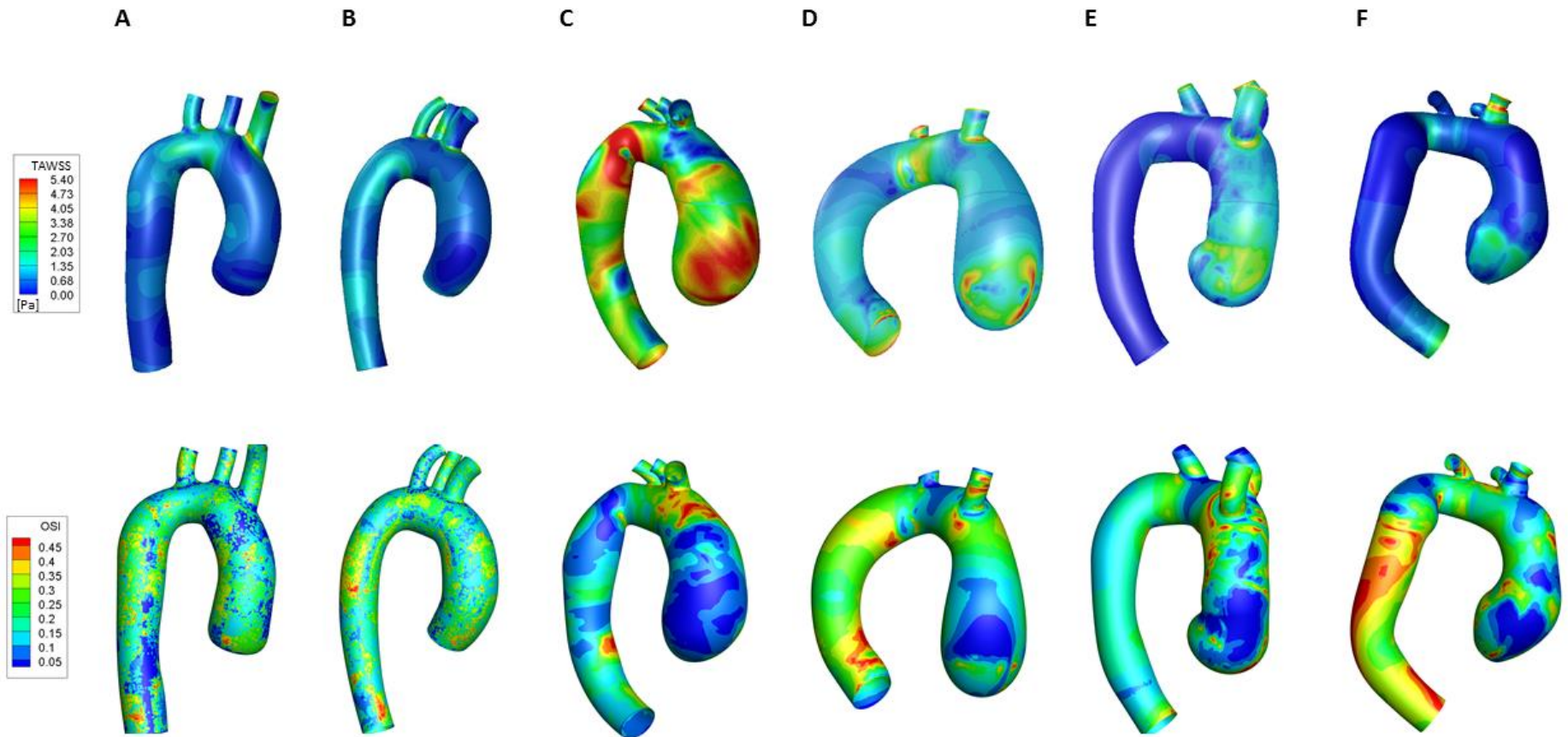
Postoperative sample

TAWSS

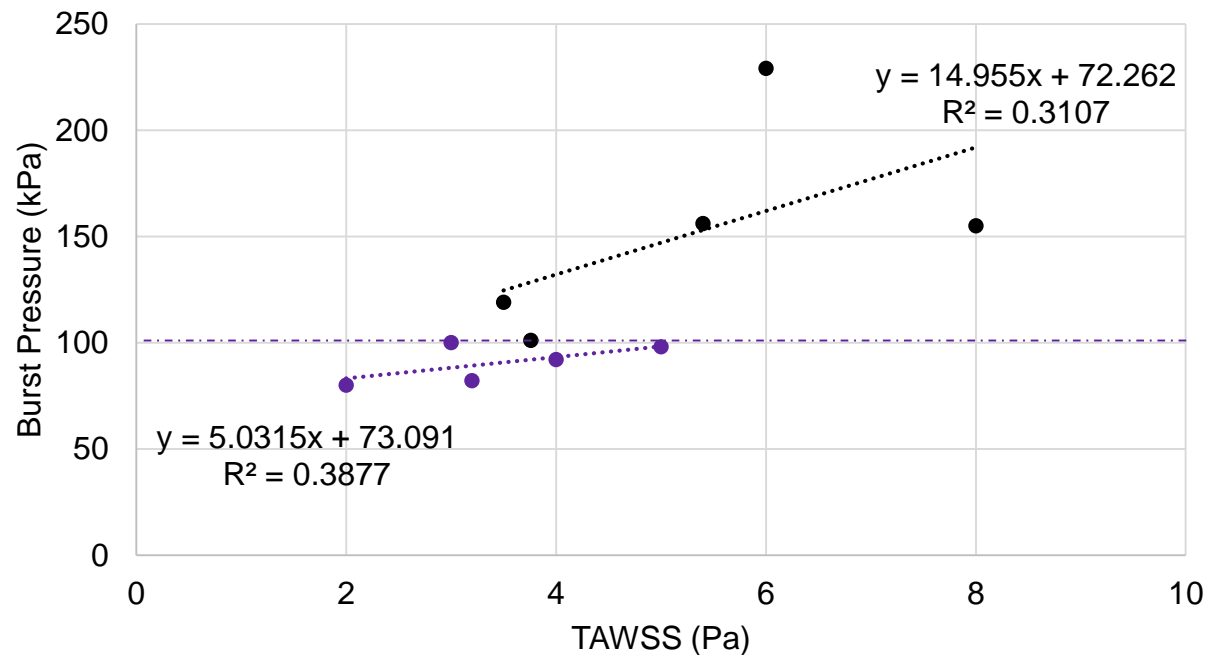
RESULTS- Flow_{eccentricity} calculated from the CFD studies against the 4D MRI results



RESULTS- OSI and TAWSS

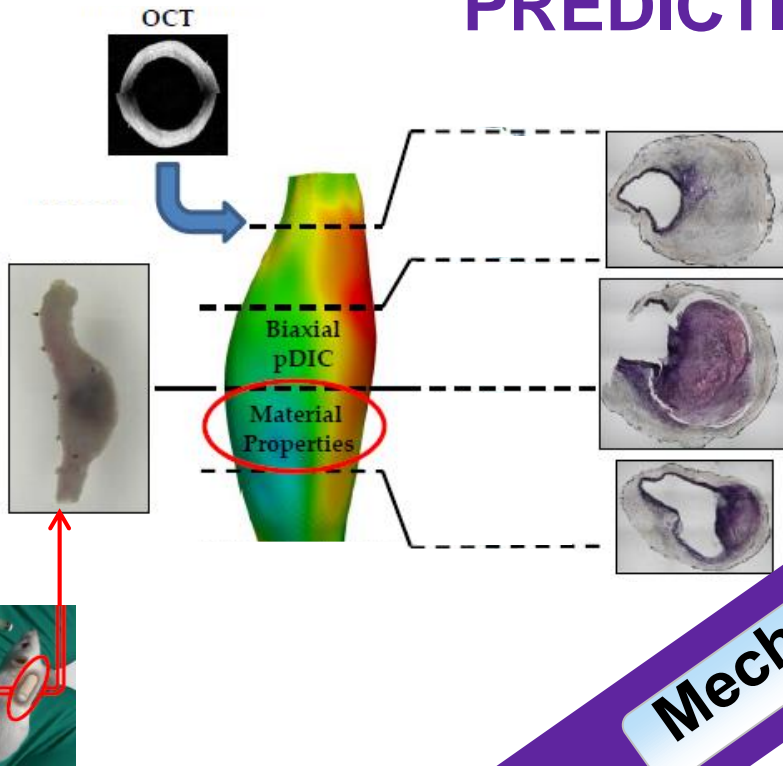


RESULTS- TAWSS versus wall properties



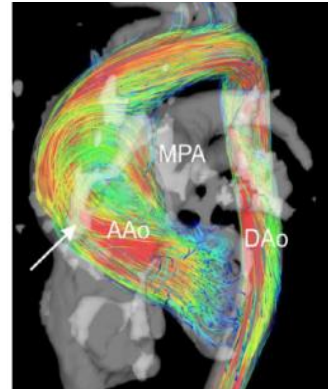
- Low Burst Pressure (kPa) vs. TAWSS (Pa)
- High Burst Pressure (kPa) vs. TAWSS (Pa)
- Linéaire (Low Burst Pressure (kPa) vs. TAWSS (Pa))
- Linéaire (High Burst Pressure (kPa) vs. TAWSS (Pa))

TOWARDS ATAA GROWTH PREDICTIONS



Clinical applications

Mechanobiology



Development of mechanobiological models



European Research Council
Established by the European Commission





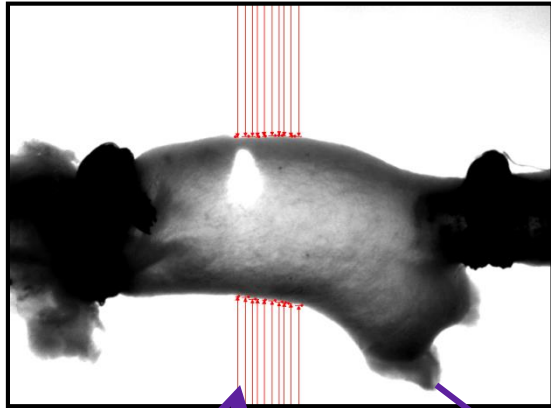
Understanding aneurysm growth using mechanobiology and multimodal imaging

Altered mechanics induce biological responses, including gene expression, protein activation and cell phenotype

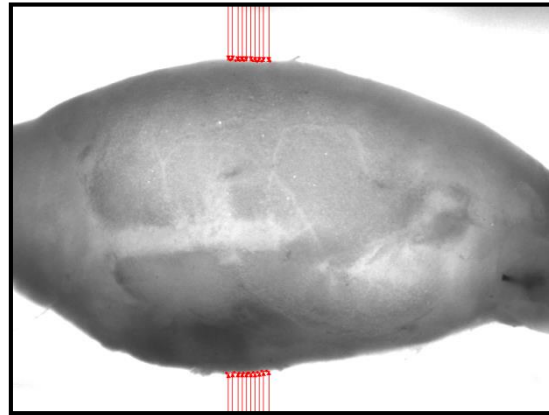


Study Design

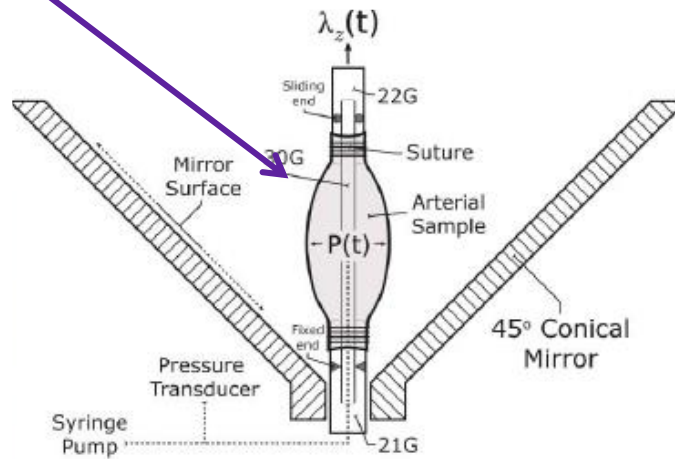
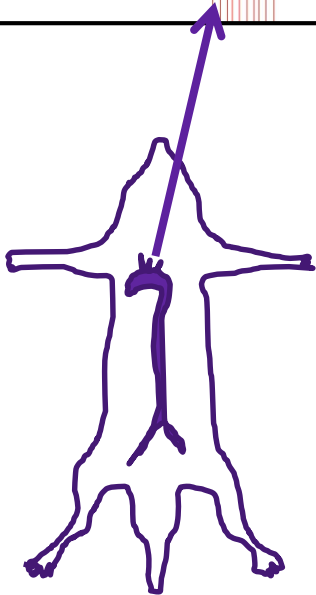
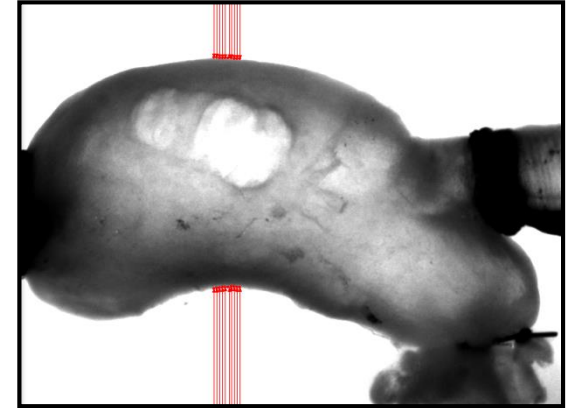
Control



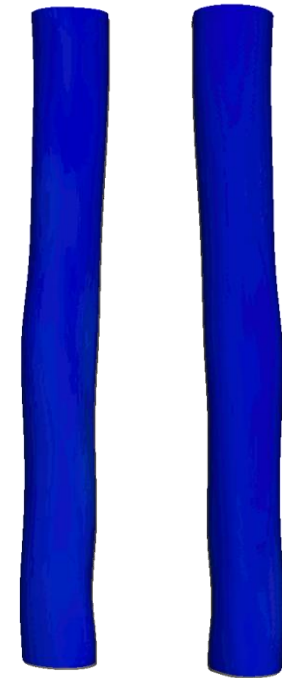
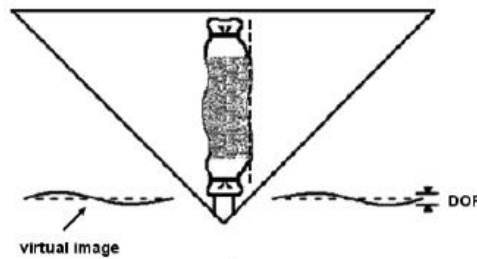
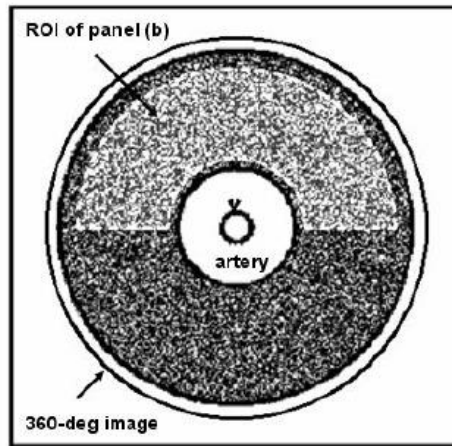
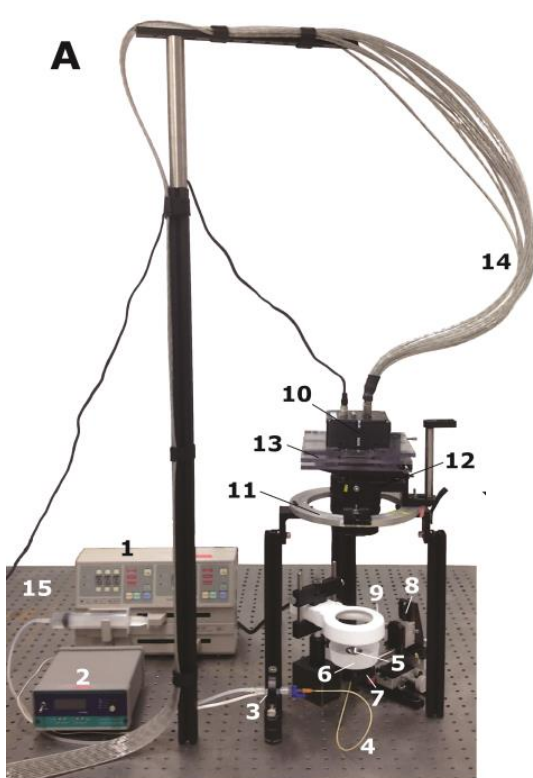
Fibulin 4 SMC KO



Fibrillin 1 *mgR/mgR*



The pDIC technique



pDIC measurements

Fibulin 4 SMC KO

Fibrillin 1 *mgR/mgR*

ventral

dorsal

inflation

ventral

dorsal

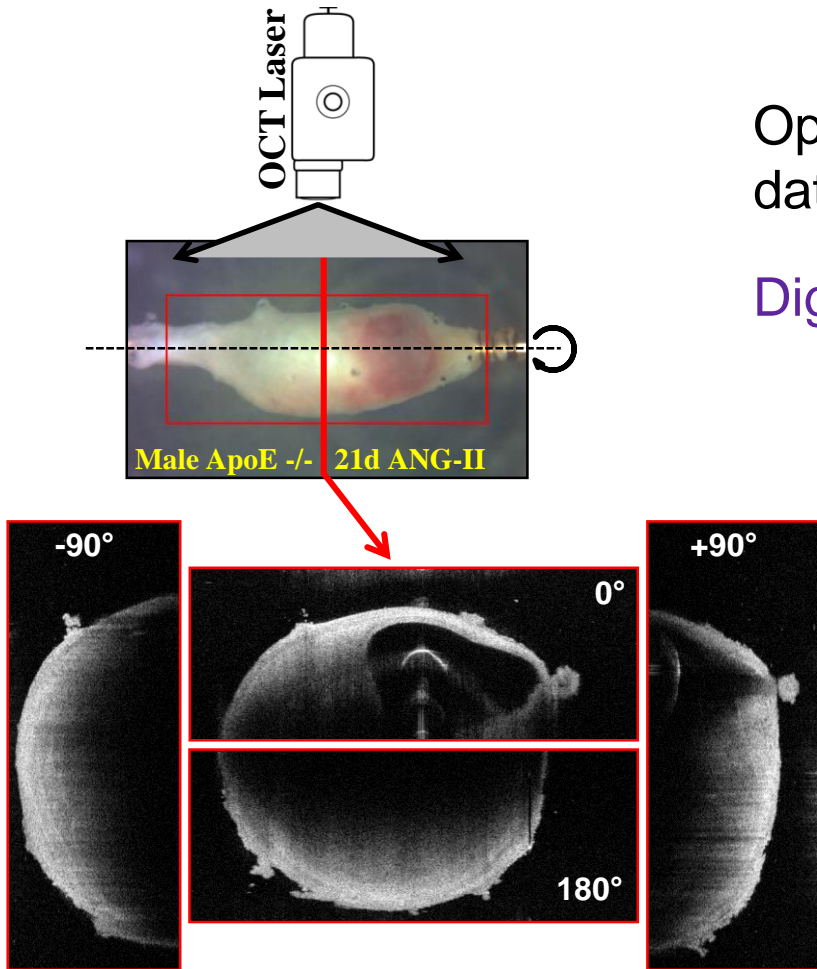
inflation

6852

CS38

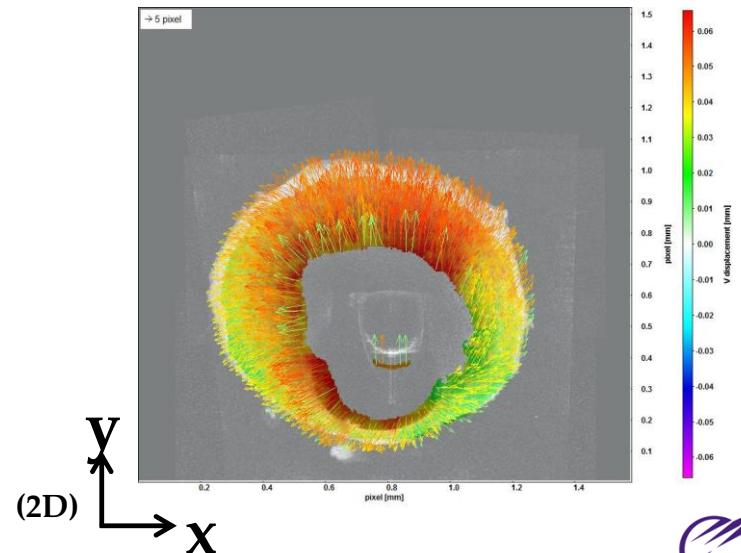


Bulk strain measurement and identification



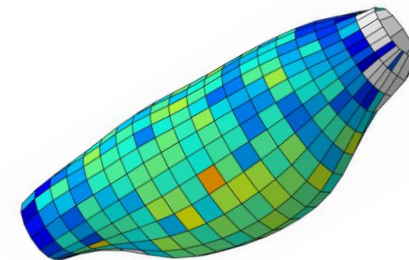
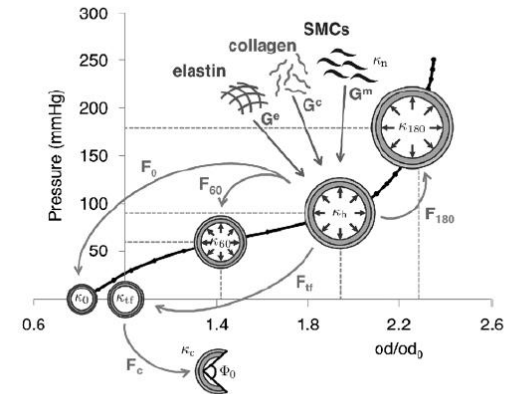
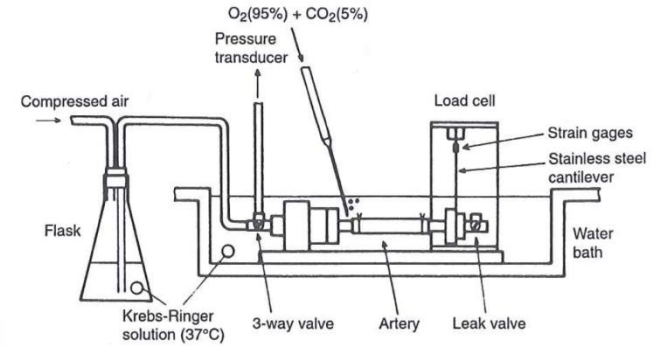
Optical Coherence Tomography (OCT) data are available from the experiments

Digital volume correlation

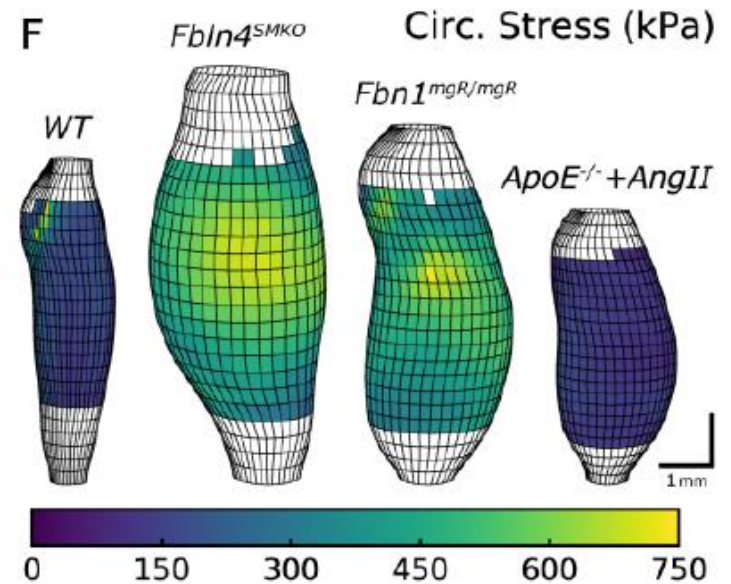
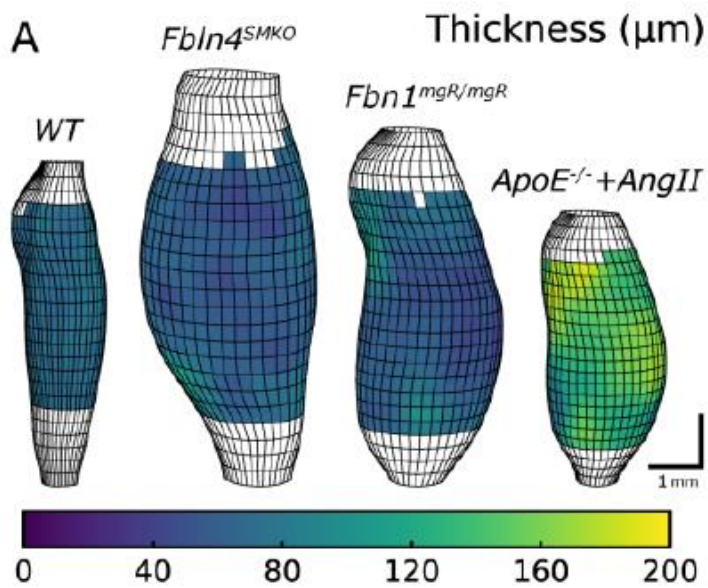


APPROACH

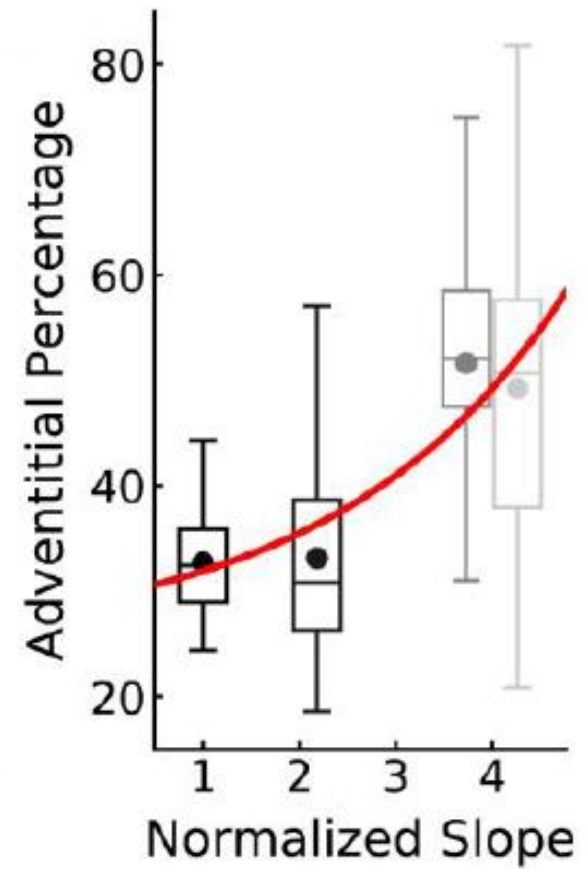
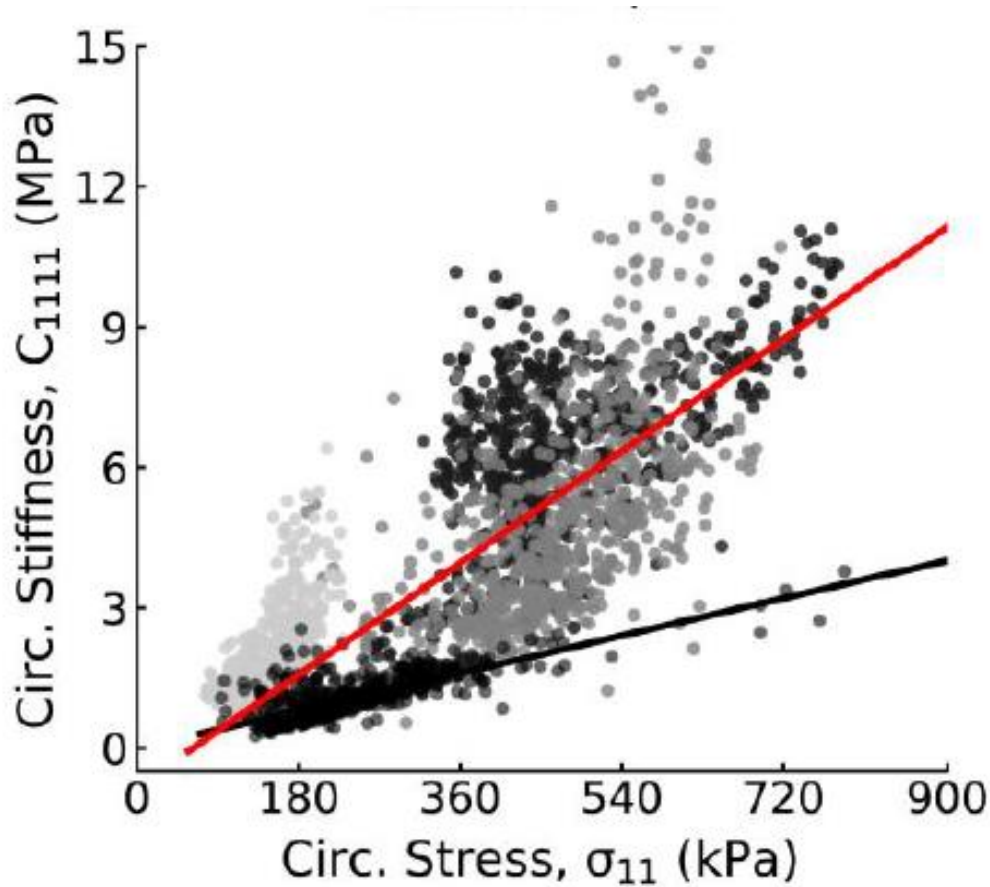
1. Experiments
2. Material model
3. Inverse method



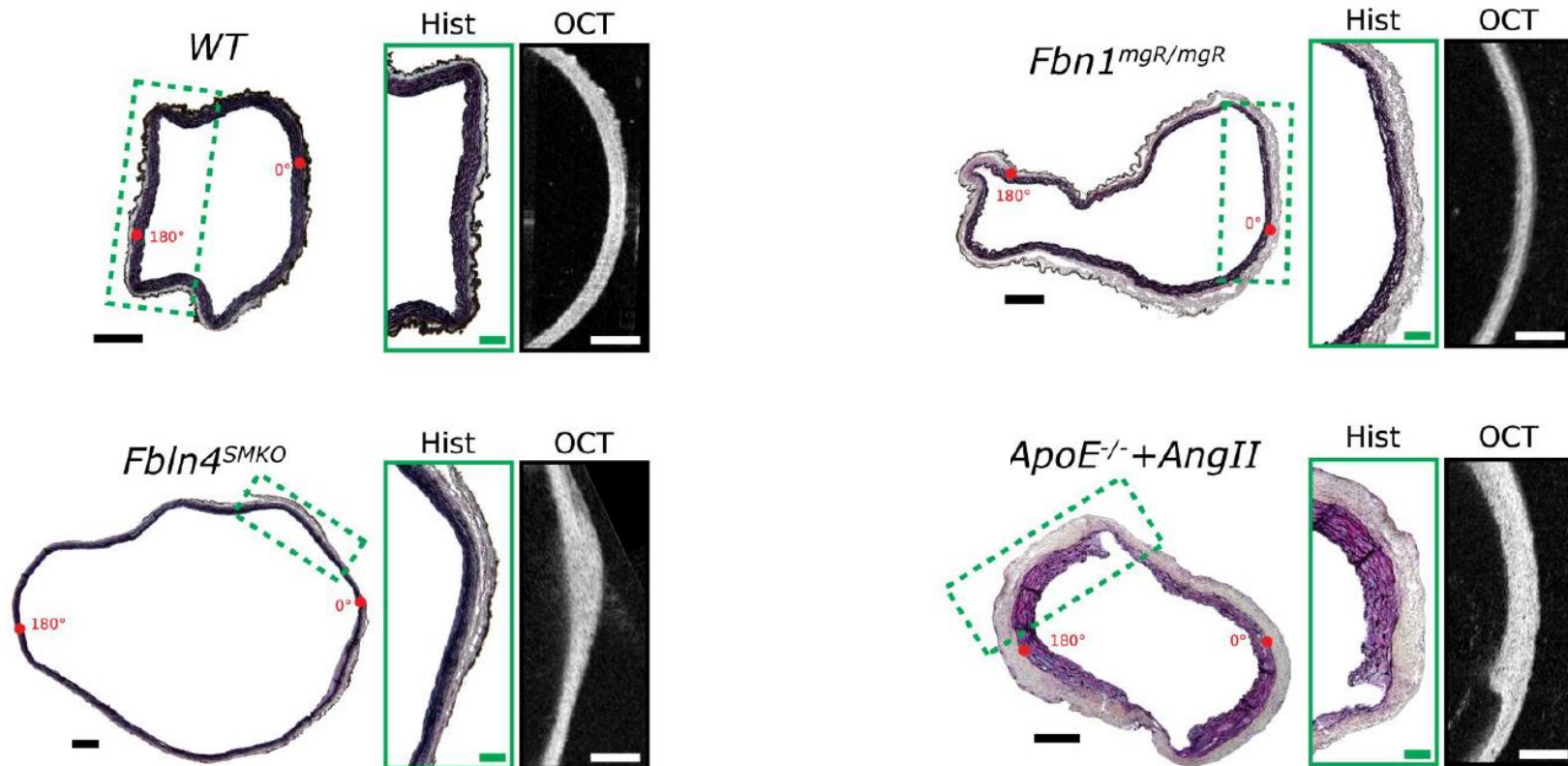
Full-Field Material Parameter Estimation vs thickness distribution



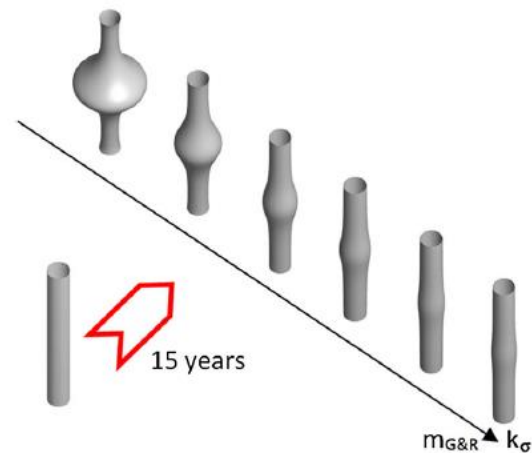
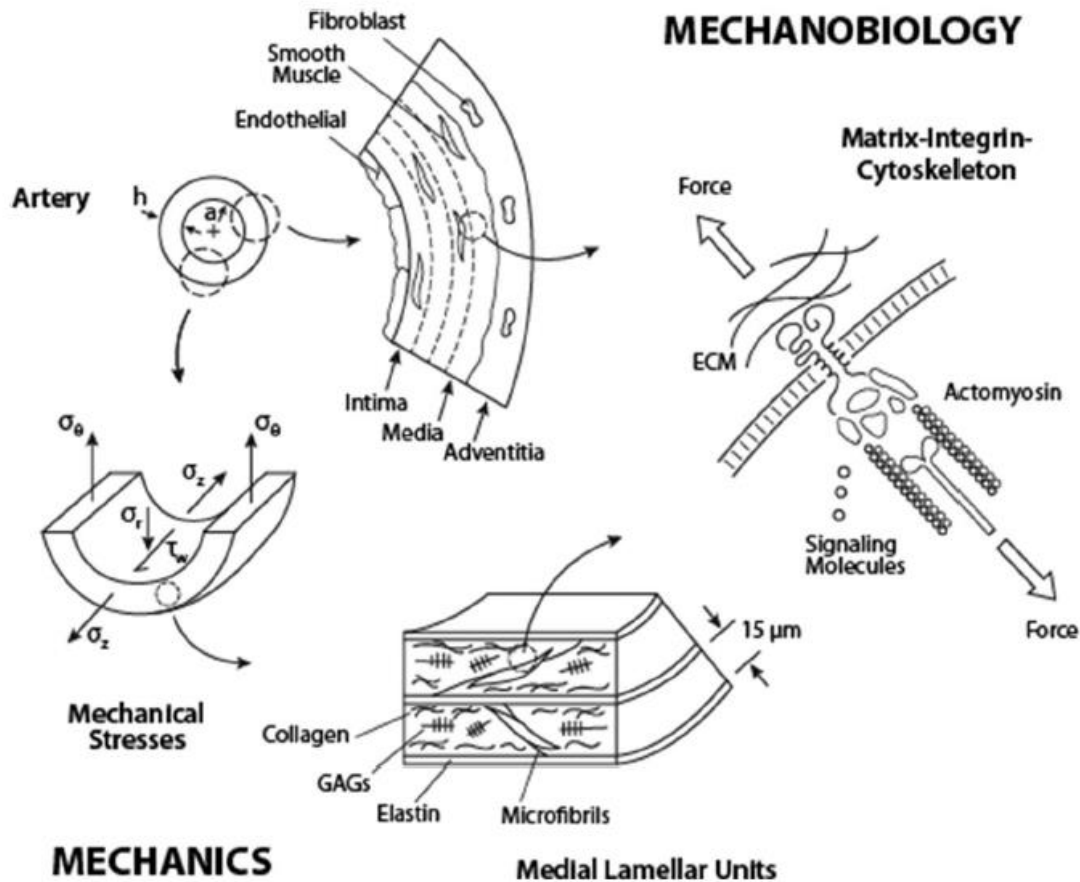
Full-Field Material Parameter Estimation vs local stress



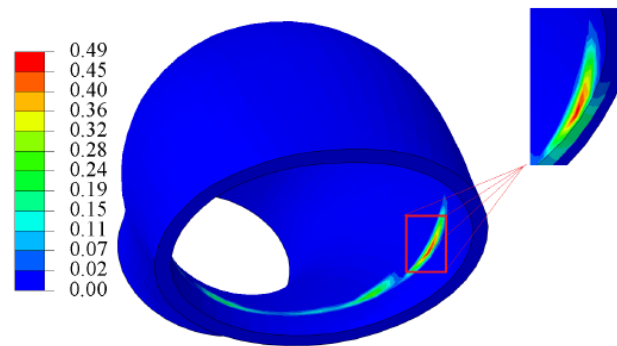
Correlation with tissue μ structure



Predictions of vascular adaptation and disease development

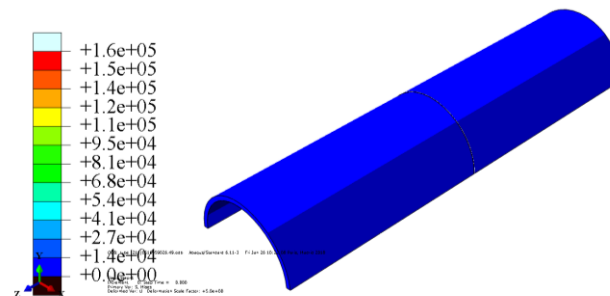


Cyron et al, BMMB, 2016, Mousavi et al, IJNMBE, 2018



Vision

- Our vision is that the evolution of the strength and of the wall stress of the aorta during the growth of an aneurysm can be predicted on a patient-specific basis by a **computational model**.
- On the basis of an MRI examination, our computational model, accessible by surgeons as an interactive intuitive user interface, would permit to predict when an aortic aneurysm is going to reach a critical size or a critical rupture risk.



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